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(54) **ABLATION APPARATUS AND SYSTEM TO LIMIT NERVE CONDUCTION**

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Publication Classification

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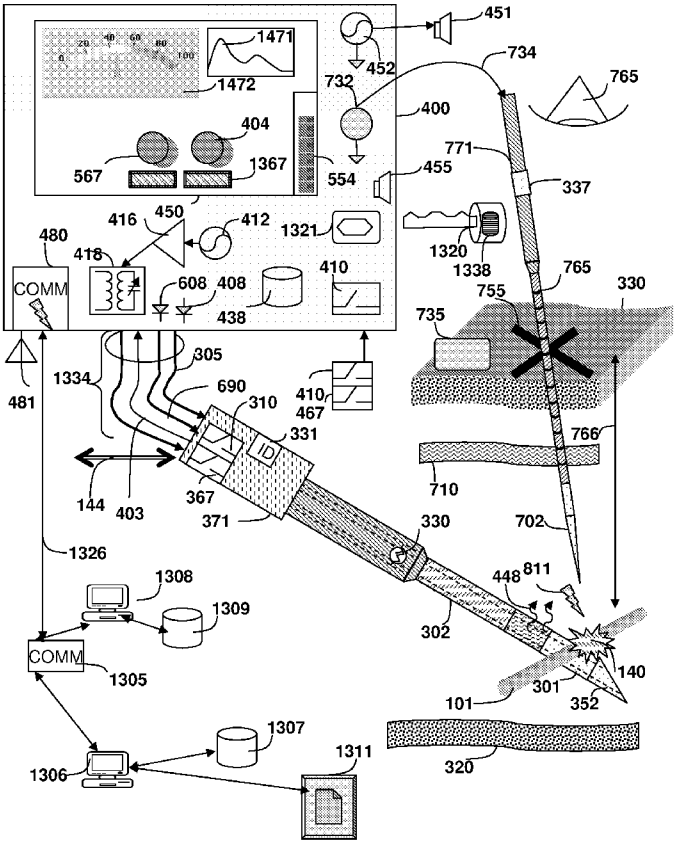
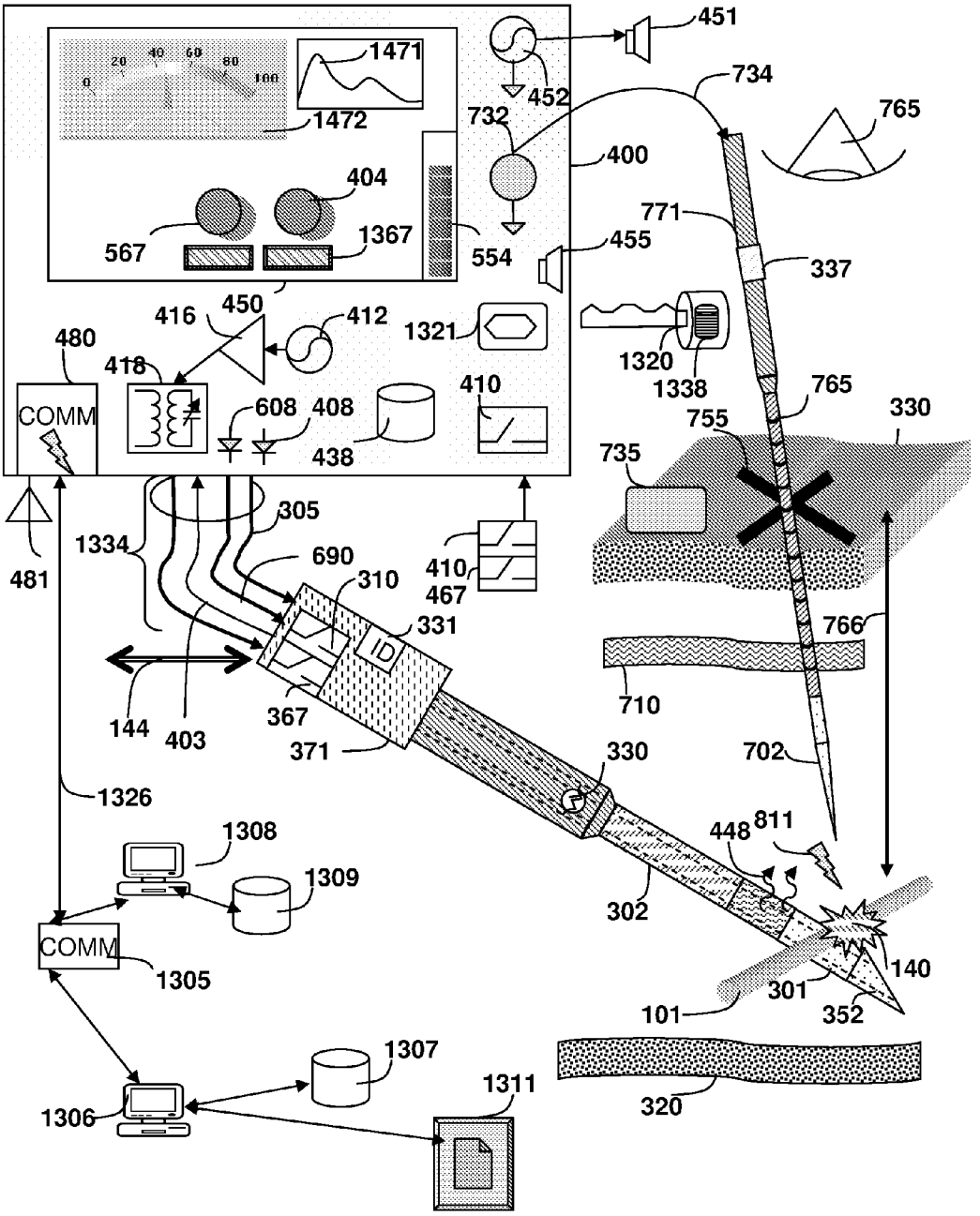
A61B 18/04 (2006.01)
A61B 5/05 (2006.01)

(52) **U.S. Cl.** **606/41**; 600/554

(57) **ABSTRACT**

An electrosurgical probe including a probe body which defines a longitudinal probe axis. The electrosurgical probe also includes a first and second conductive electrode, each disposed along the probe axis. The surface area of the first conductive electrode is greater of the surface area of the second conductive electrode. The ratio of the surface area of the first conductive electrode to the surface area of the second conductive electrode may be adjustable. Another aspect of the present invention is an electrosurgical probe having a probe body which defines a single longitudinal probe axis. The electrosurgical probe of this aspect of the invention further includes more than two electrodes operatively disposed at separate and distinct positions along the axis of the probe body. The electrodes may be selectively connected to one of or a combination of a stimulation energy source, an ablation energy source or a ground for either energy source. Another aspect of the present invention is a method of placing an electrosurgical probe such as described above for specific ablation procedures.

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734
765
452
732
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1471
1472
404
567
1367
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455
771
337
450
416
412
1321
480
418
1320
1338
765
330
COMM
608
408
410
438
755
735
305
1334
690
310
410
467
481
331
ID
766
710
144
403
367
371
330
702
1326
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811
302
COMM
1305
140
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352
101
1307
1311
1306
320

FIG. 1

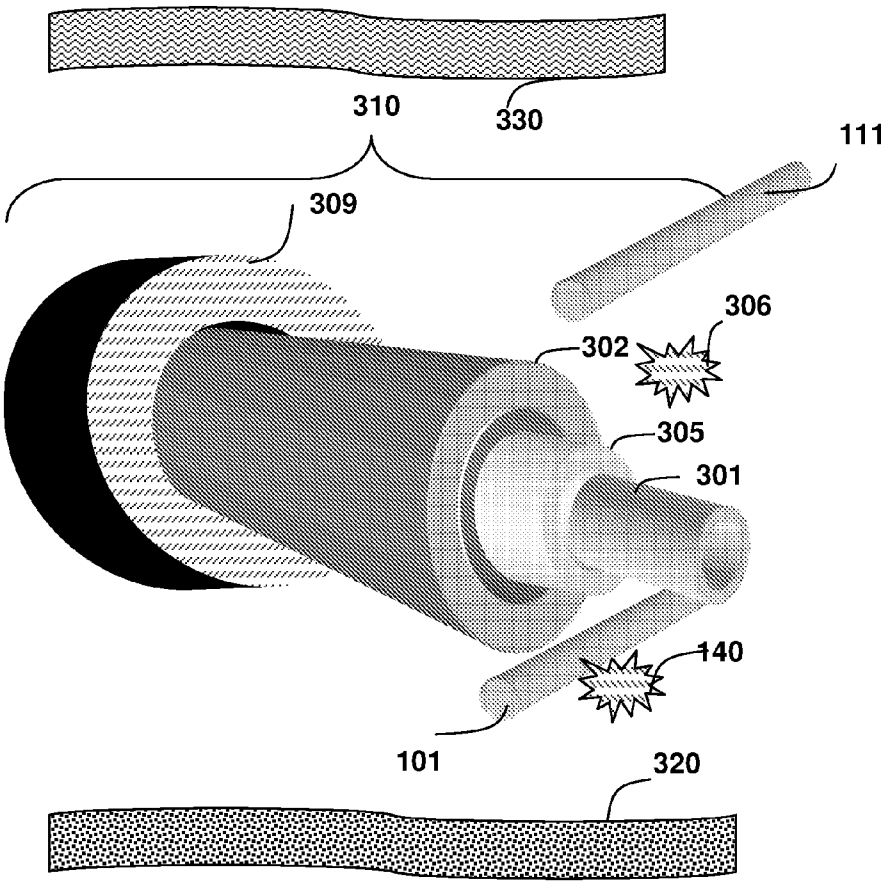


FIG. 2

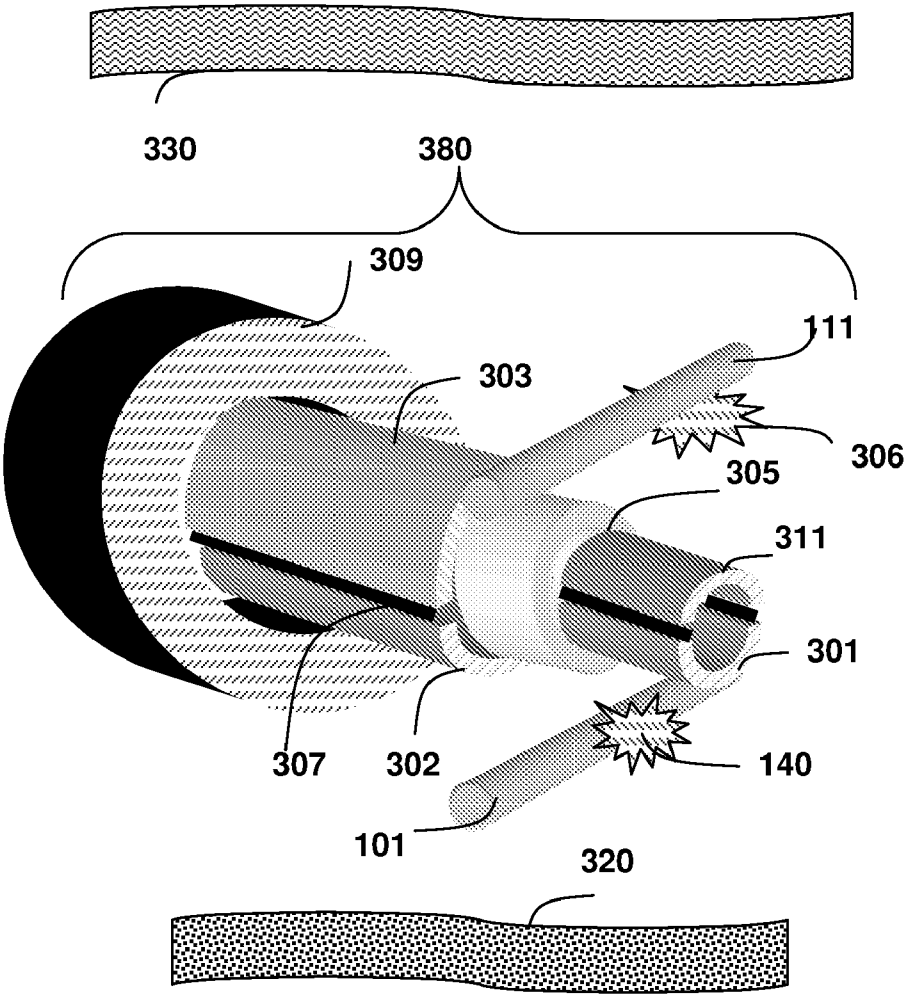


Fig. 2A

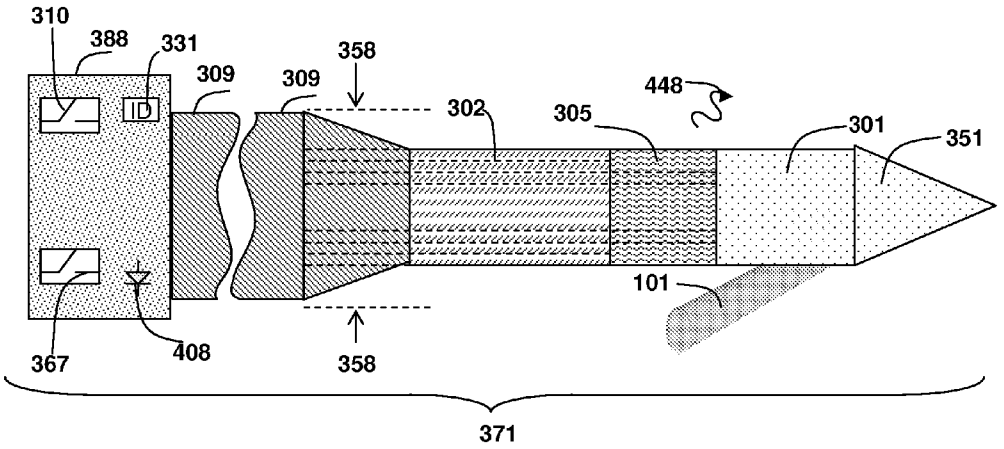

310
388
331
309
309
358
302
305
448
301
351
ID
101
367
408
358
371

FIG. 3A

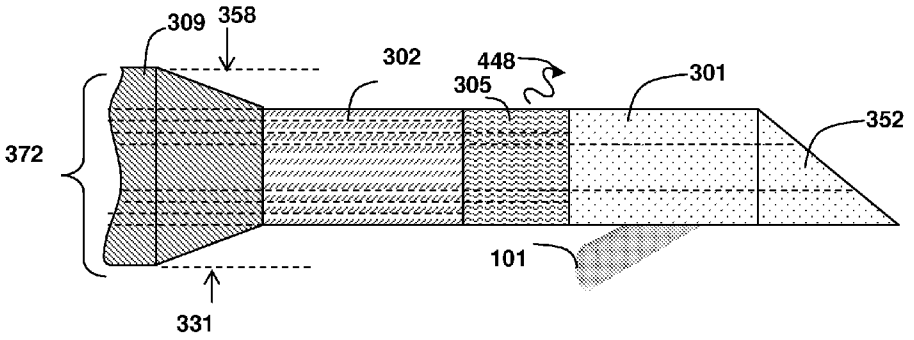
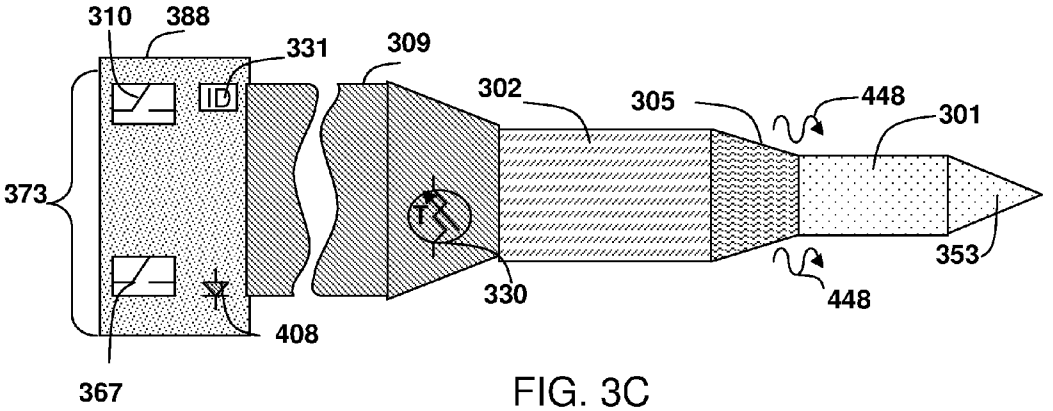

309
358
302
448
305
301
352
372
101
331

FIG. 3B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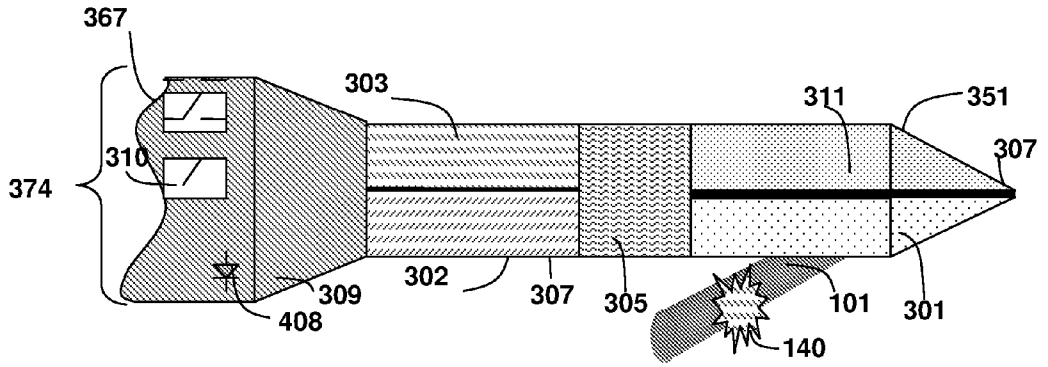
388
331
309
302
305
448
301
373
ID
353
330
448
408
367

FIG. 3C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303
311
351
307
310
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309
302
307
305
101
301
408
140

FIG. 3D

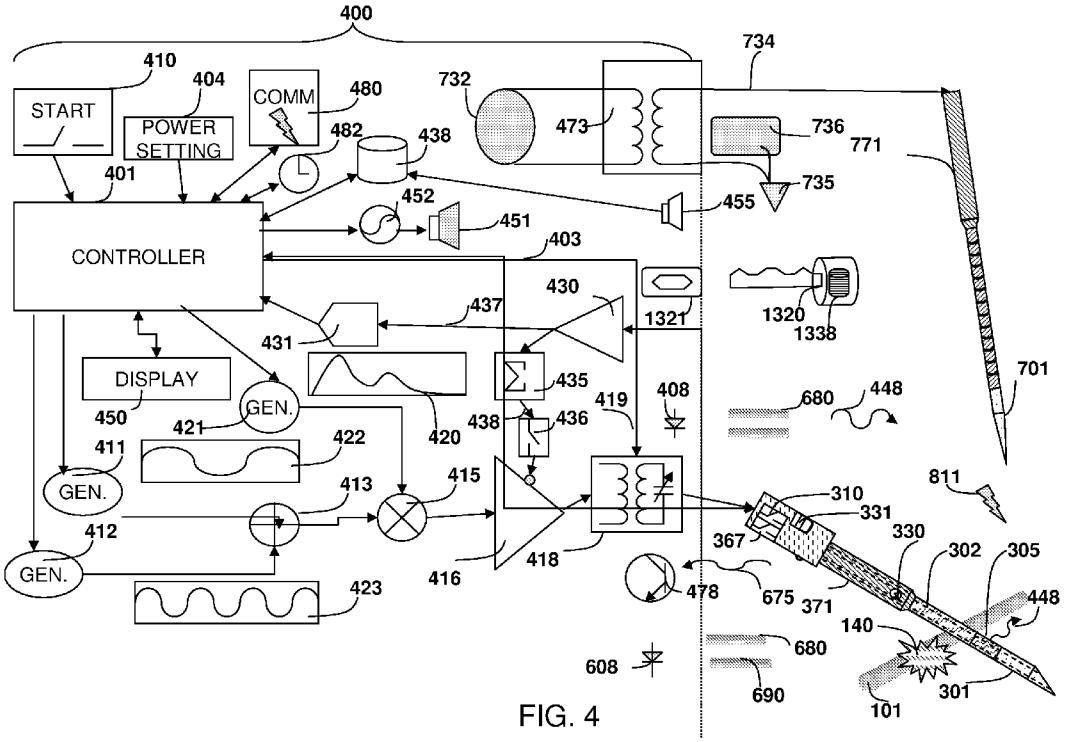

400
410
START
404
POWER SETTING
COMM
480
482
438
732
473
734
736
771
735
455
452
451
403
401
CONTROLLER
430
437
431
1321
1320
1338
701
DISPLAY
450
GEN.
421
422
420
435
436
438
419
408
680
448
411
GEN.
413
415
412
GEN.
423
416
418
310
331
330
367
302
305
811
448
478
675
371
140
680
608
690
301
101

FIG. 4

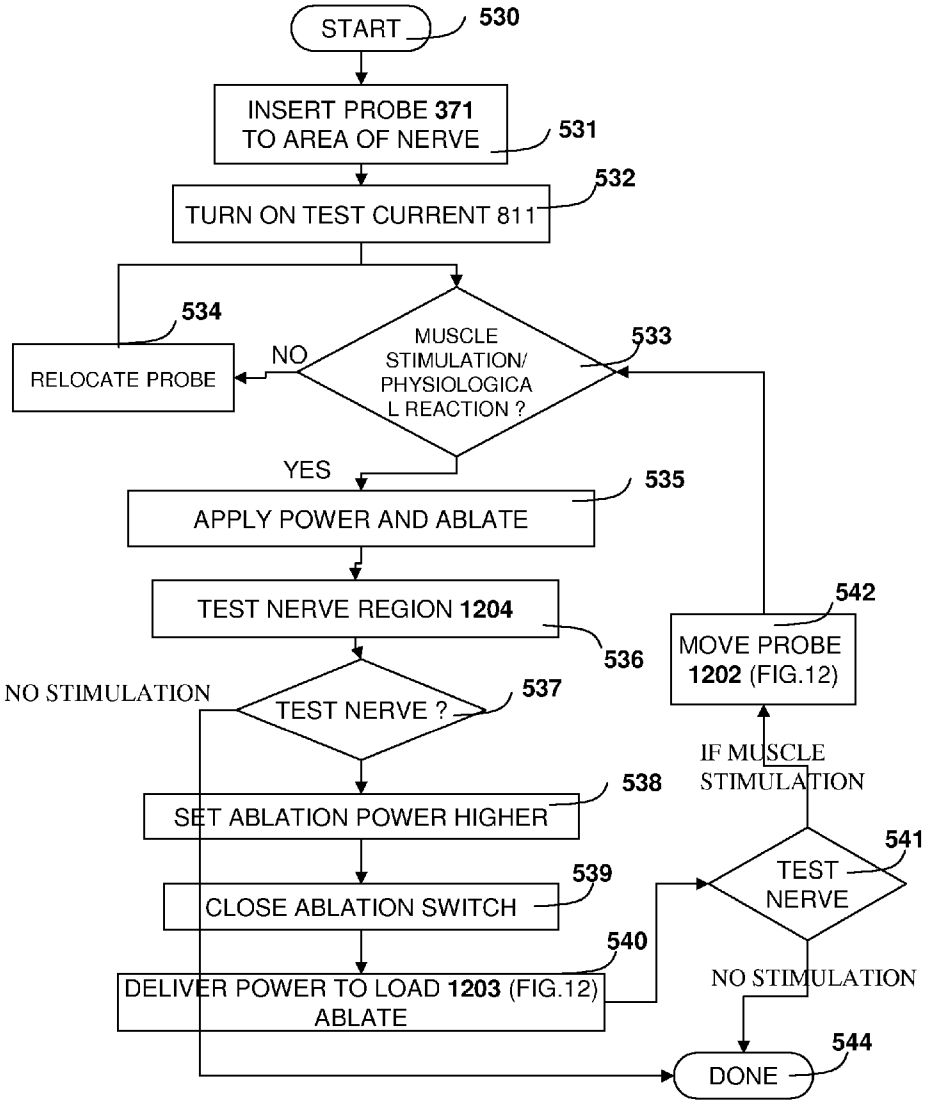

START
530
INSERT PROBE 371 TO AREA OF NERVE
531
TURN ON TEST CURRENT 811
532
MUSCLE STIMULATION/ PHYSIOLOGICA L REACTION ?
533
NO
RELOCATE PROBE
534
YES
APPLY POWER AND ABLATE
535
TEST NERVE REGION 1204
536
TEST NERVE ?
537
NO STIMULATION
SET ABLATION POWER HIGHER
538
CLOSE ABLATION SWITCH
539
DELIVER POWER TO LOAD 1203 (FIG.12) ABLATE
540
TEST NERVE
541
IF MUSCLE STIMULATION
MOVE PROBE 1202 (FIG.12)
542
NO STIMULATION
DONE
544

FIG. 5A

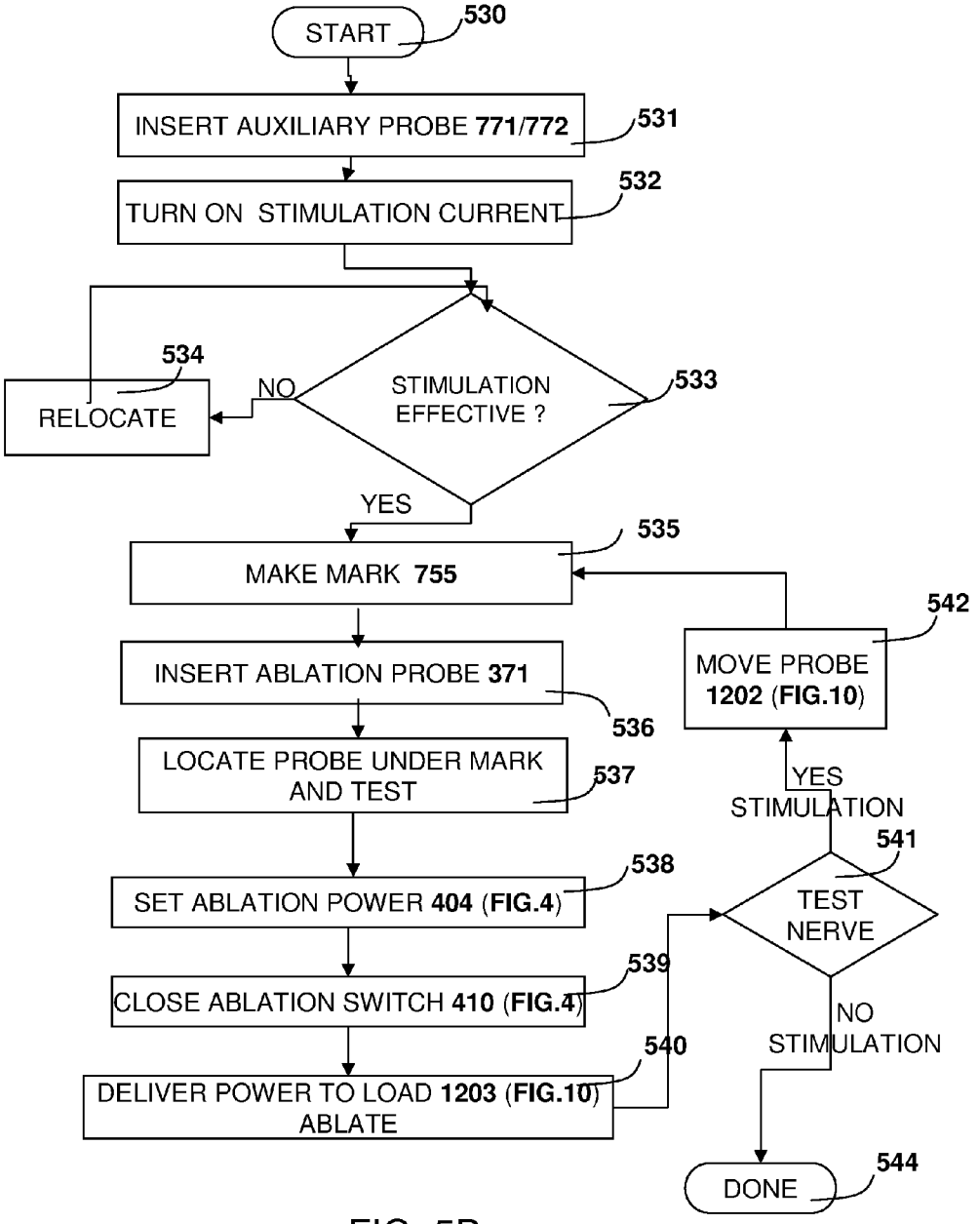

START
530
INSERT AUXILIARY PROBE 771/772
531
TURN ON STIMULATION CURRENT
532
STIMULATION EFFECTIVE ?
533
NO
RELOCATE
534
YES
MAKE MARK 755
535
INSERT ABLATION PROBE 371
536
LOCATE PROBE UNDER MARK AND TEST
537
SET ABLATION POWER 404 (FIG.4)
538
CLOSE ABLATION SWITCH 410 (FIG.4)
539
DELIVER POWER TO LOAD 1203 (FIG.10) ABLATE
540
TEST NERVE
541
YES STIMULATION
MOVE PROBE 1202 (FIG.10)
542
NO STIMULATION
DONE
544

FIG. 5B

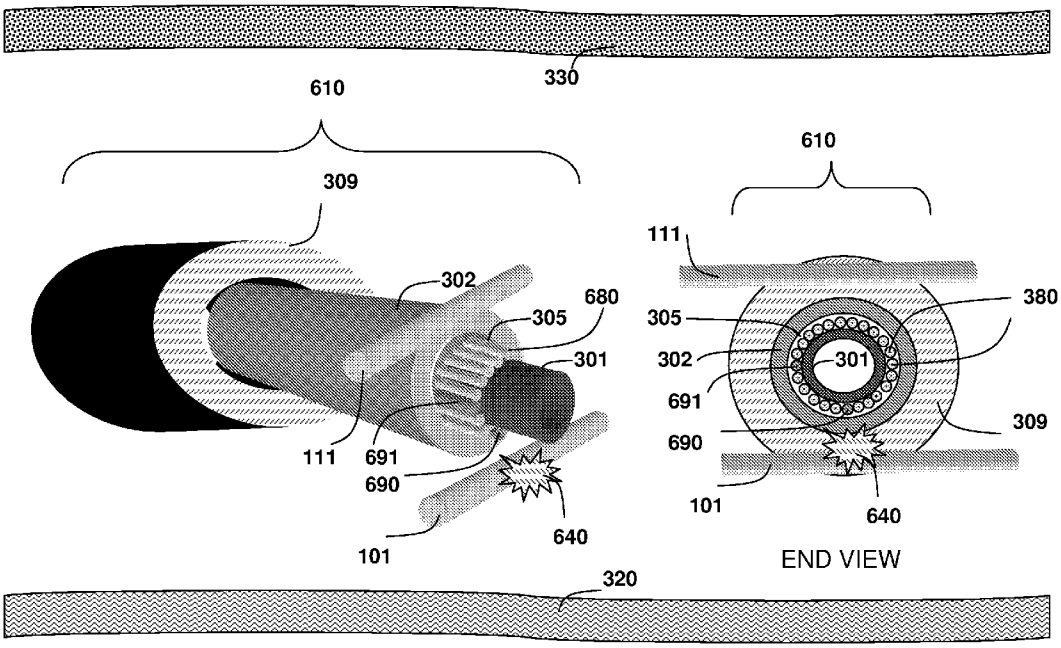
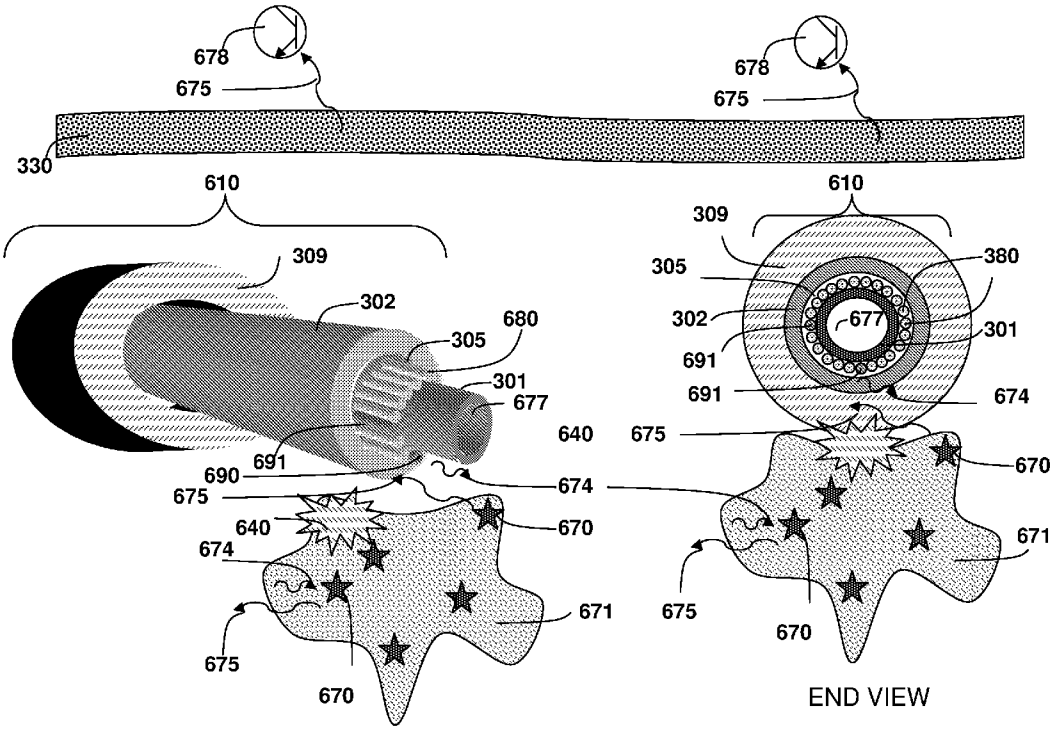

330
610
309
302
680
305
301
111
691
690
640
101
320
610
111
380
305
302
301
691
309
690
101
640
END VIEW

FIG. 6


678
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674
670
671
675
670
678
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302
677
301
691
691
674
640
675
670
671
675
670
END VIEW

FIG. 6A

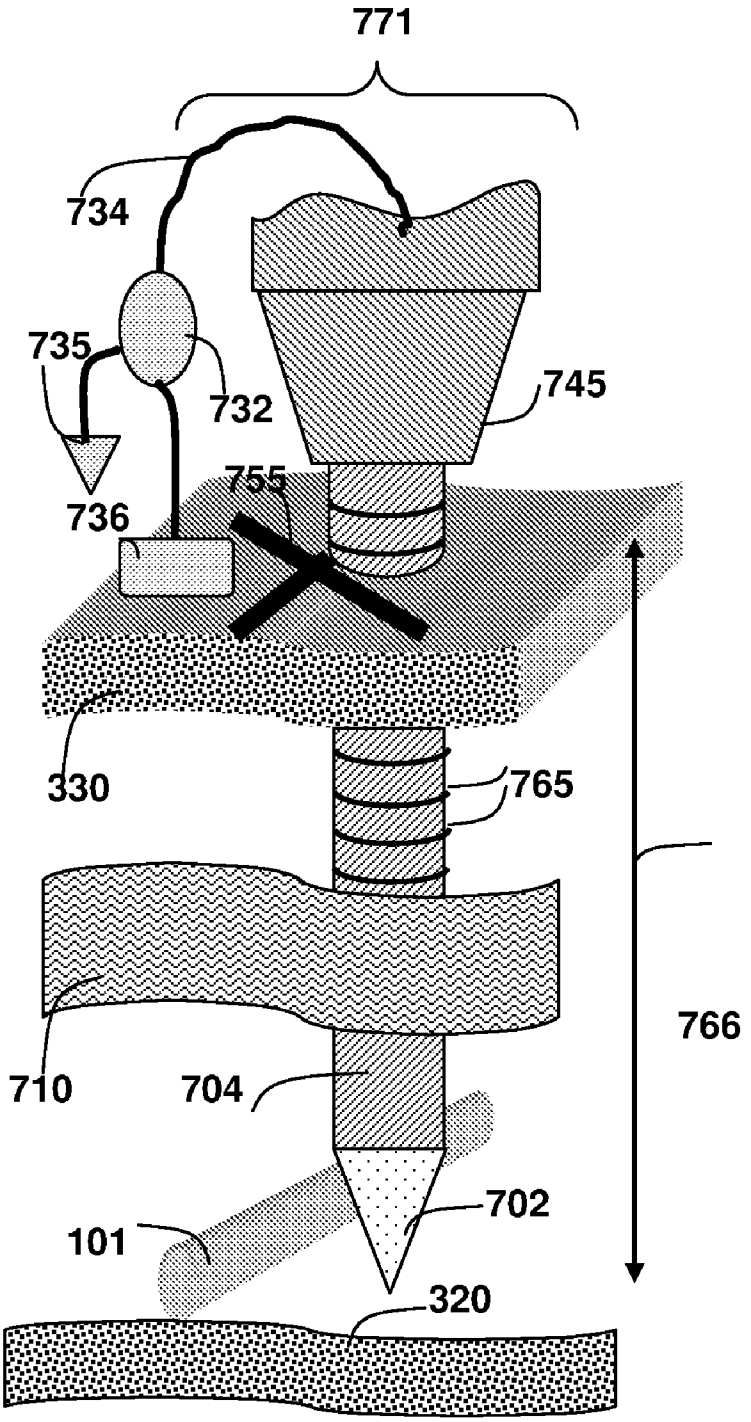


FIG. 7

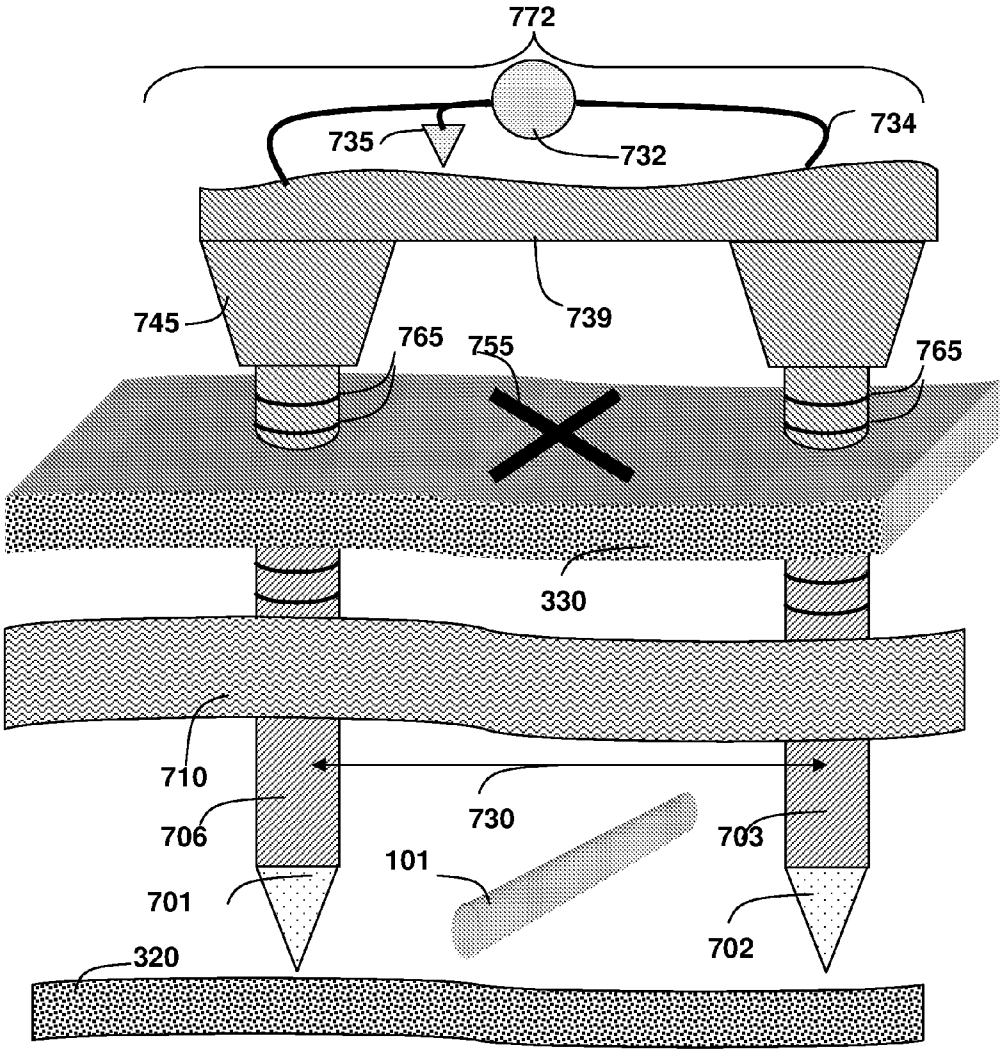
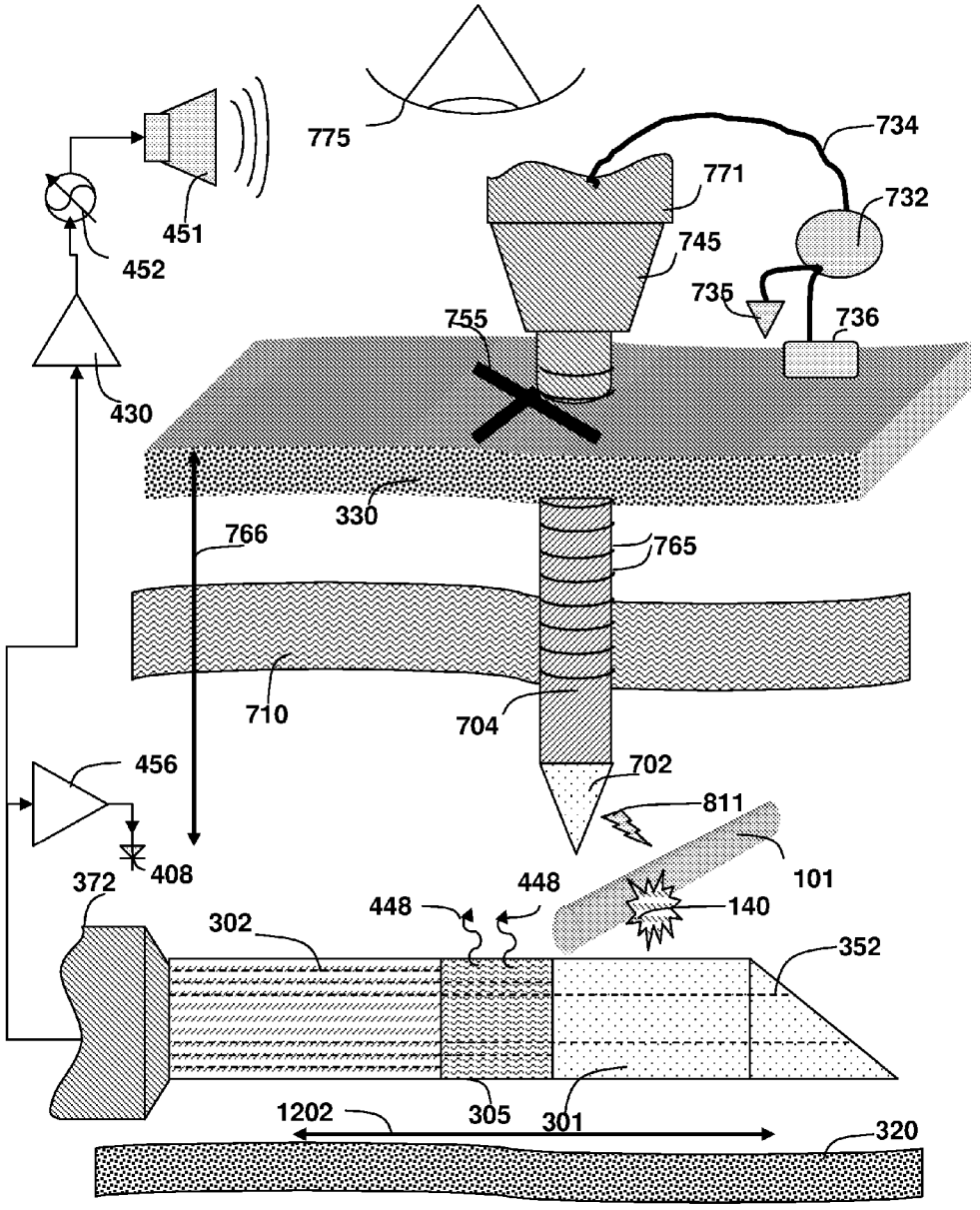

772
735
732
734
745
739
765
755
765
330
710
730
706
703
101
701
702
320

FIG. 7A


775
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330
766
765
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811
408
372
448
448
101
140
302
352
1202
305
301
320

FIG. 8

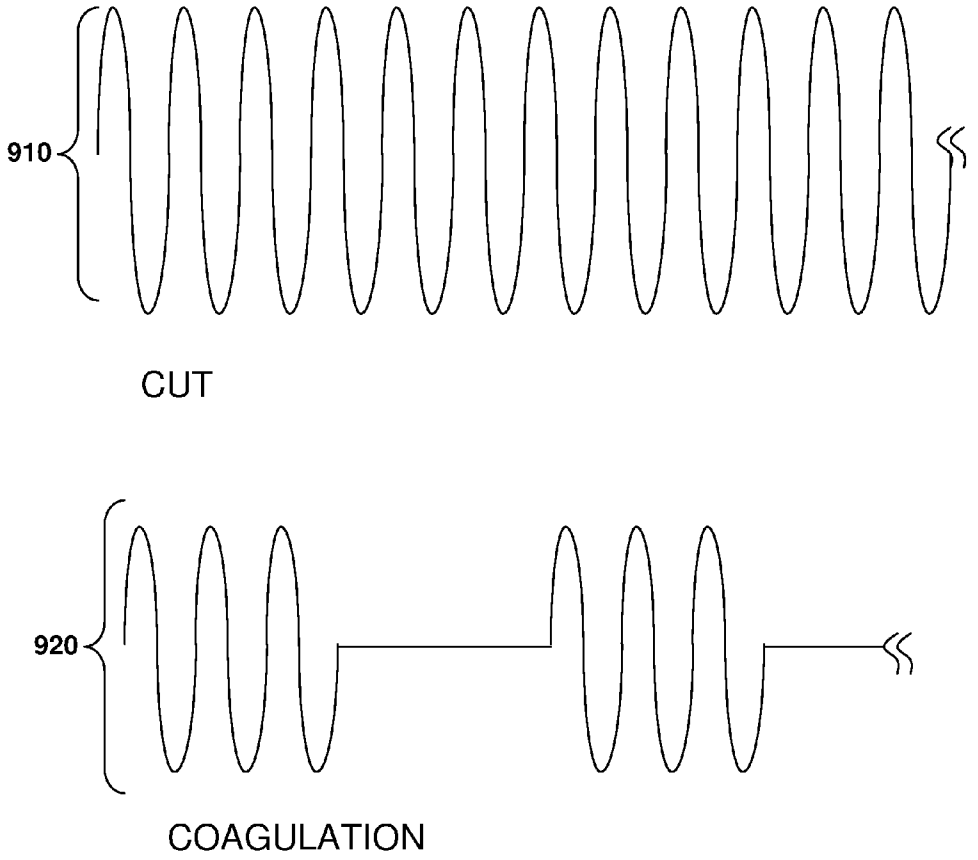
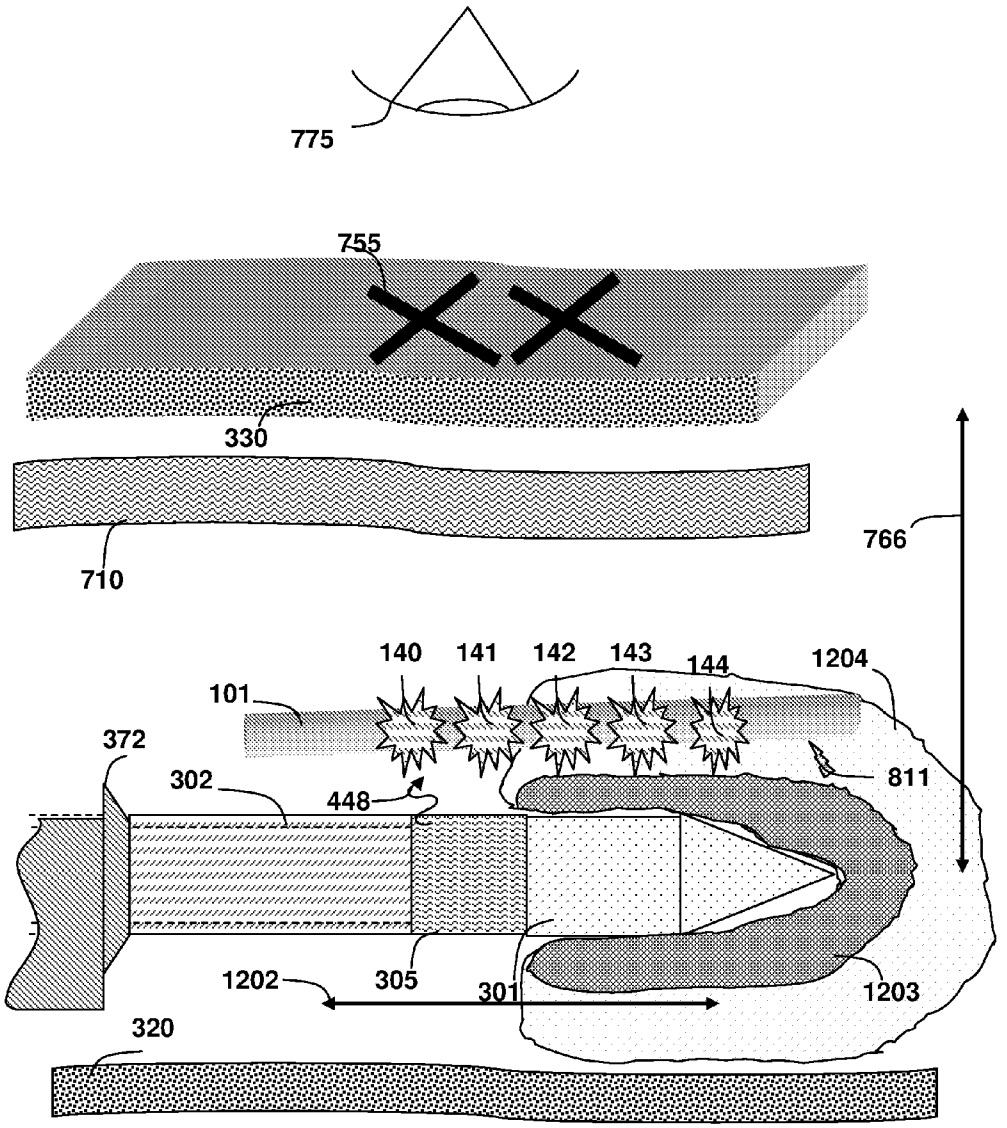


FIG. 9


775
755
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710
766
140
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142
143
144
1204
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372
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448
811
1202
305
301
1203
320

FIG. 10

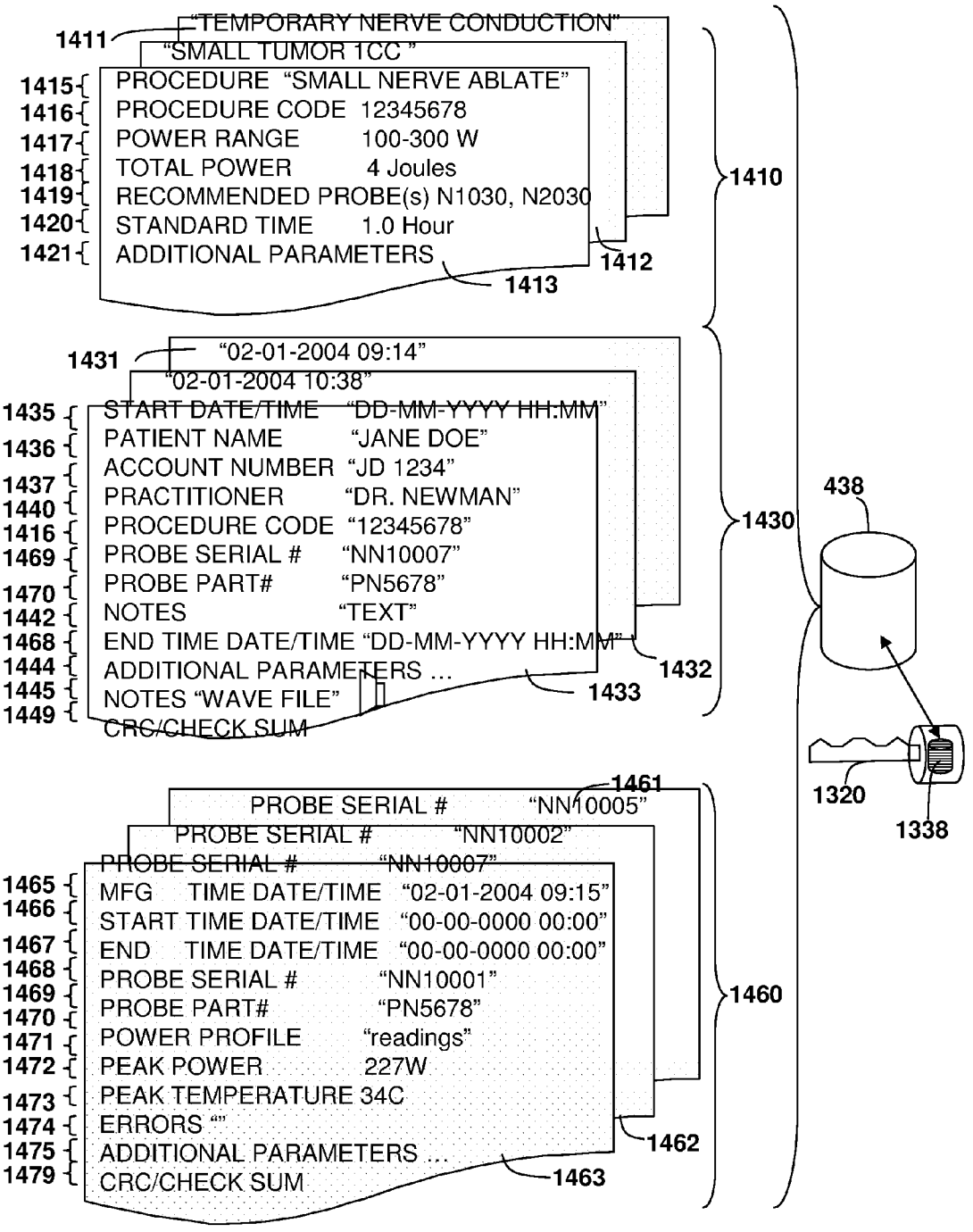

"TEMPORARY NERVE CONDUCTION"
1411
"SMALL TUMOR 1CC "
1415 PROCEDURE "SMALL NERVE ABLATE"
1416 PROCEDURE CODE 12345678
1417 POWER RANGE 100-300 W
1418 TOTAL POWER 4 Joules
1419 RECOMMENDED PROBE(s) N1030, N2030
1420 STANDARD TIME 1.0 Hour
1421 ADDITIONAL PARAMETERS
1412
1413
1410
1431
"02-01-2004 09:14"
"02-01-2004 10:38"
1435 START DATE/TIME "DD-MM-YYYY HH:MM"
1436 PATIENT NAME "JANE DOE"
1437 ACCOUNT NUMBER "JD 1234"
1440 PRACTITIONER "DR. NEWMAN"
1416 PROCEDURE CODE "12345678"
1469 PROBE SERIAL # "NN10007"
1470 PROBE PART# "PN5678"
1442 NOTES "TEXT"
1468 END TIME DATE/TIME "DD-MM-YYYY HH:MM"
1444 ADDITIONAL PARAMETERS ...
1445 NOTES "WAVE FILE"
1449 CRC/CHECK SUM
1432
1433
1430
438
1320
1338
1461
PROBE SERIAL # "NN10005"
PROBE SERIAL # "NN10002"
PROBE SERIAL # "NN10007"
1465 MFG TIME DATE/TIME "02-01-2004 09:15"
1466 START TIME DATE/TIME "00-00-0000 00:00"
1467 END TIME DATE/TIME "00-00-0000 00:00"
1468 PROBE SERIAL # "NN10001"
1469 PROBE PART# "PN5678"
1470 POWER PROFILE "readings"
1471 PEAK POWER 227W
1472 PEAK TEMPERATURE 34C
1473 ERRORS ""
1474 ADDITIONAL PARAMETERS ...
1475 CRC/CHECK SUM
1479
1462
1463
1460

FIG. 11

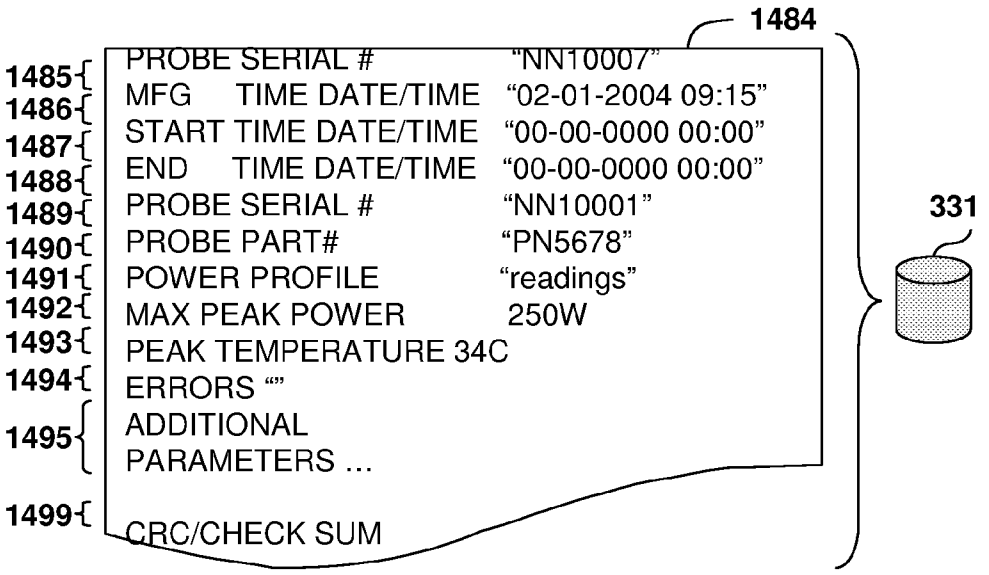

1484
1485
PROBE SERIAL # "NN10007"
1486
MFG TIME DATE/TIME "02-01-2004 09:15"
1487
START TIME DATE/TIME "00-00-0000 00:00"
1488
END TIME DATE/TIME "00-00-0000 00:00"
1489
PROBE SERIAL # "NN10001"
1490
PROBE PART# "PN5678"
1491
POWER PROFILE "readings"
1492
MAX PEAK POWER 250W
1493
PEAK TEMPERATURE 34C
1494
ERRORS ""
1495
ADDITIONAL PARAMETERS ...
1499
CRC/CHECK SUM
331

FIG. 11A

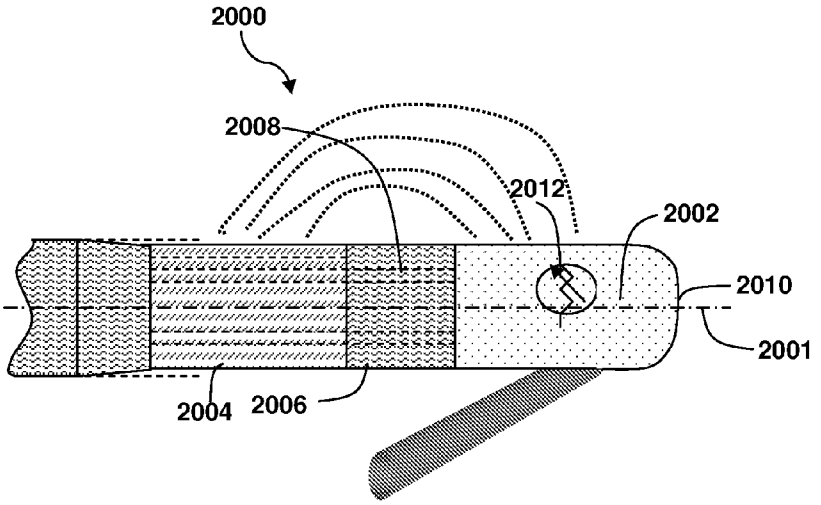

2000
2008
2012
2002
2010
2001
2004
2006

Fig. 12

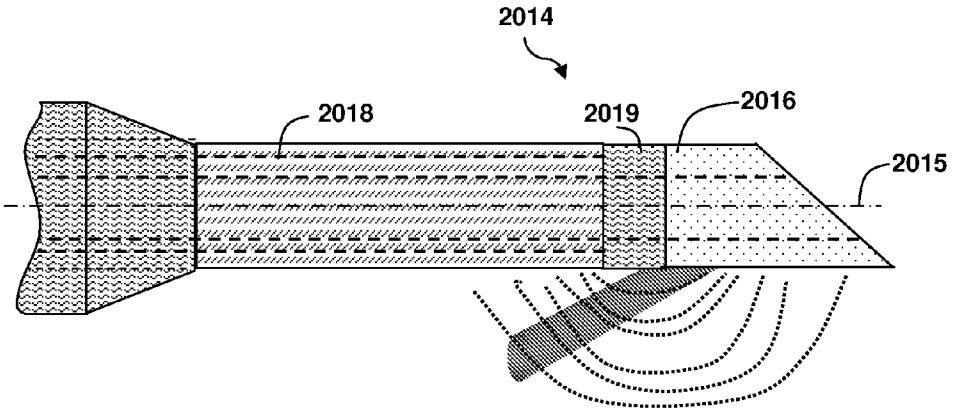

2014
2018
2019
2016
2015

FIG. 13

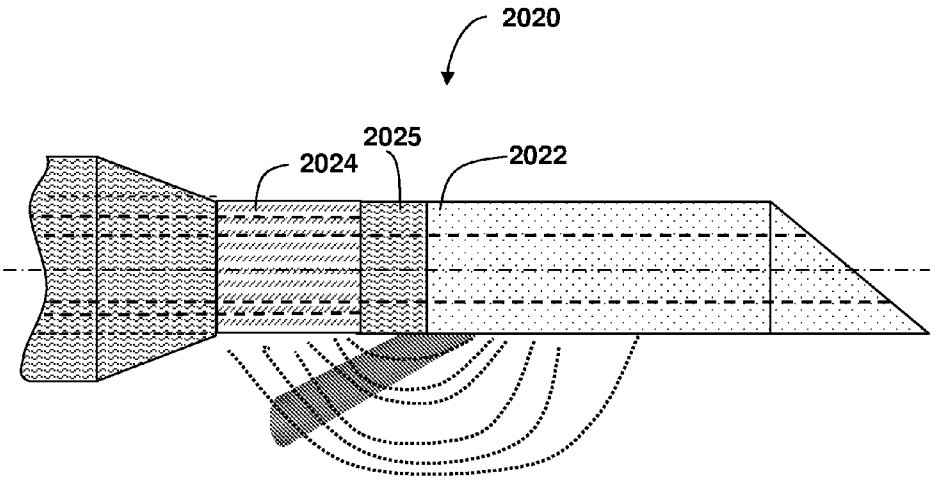


Fig. 14

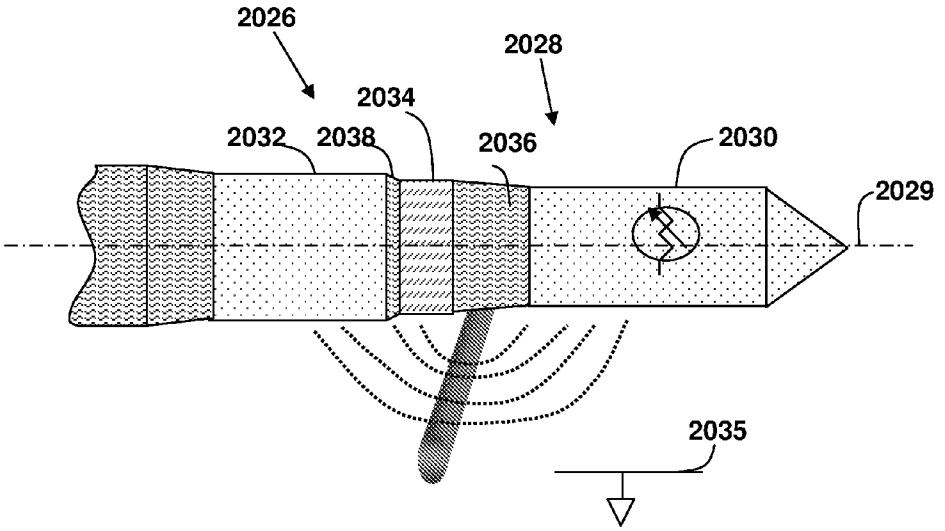


Fig. 15

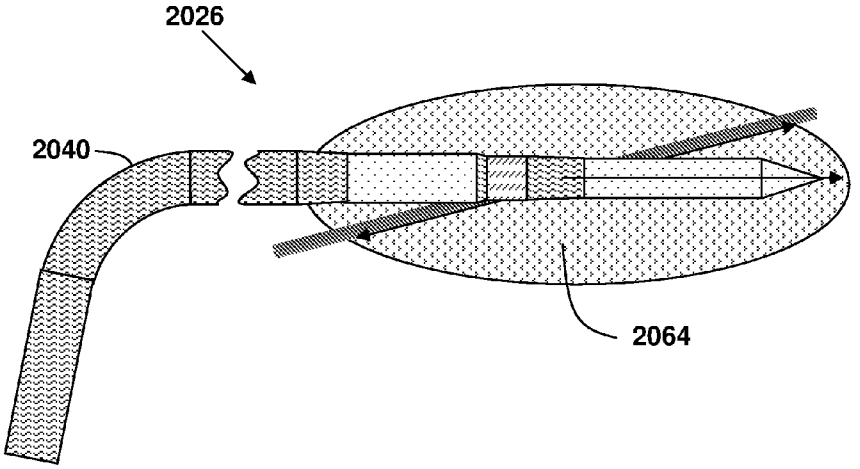
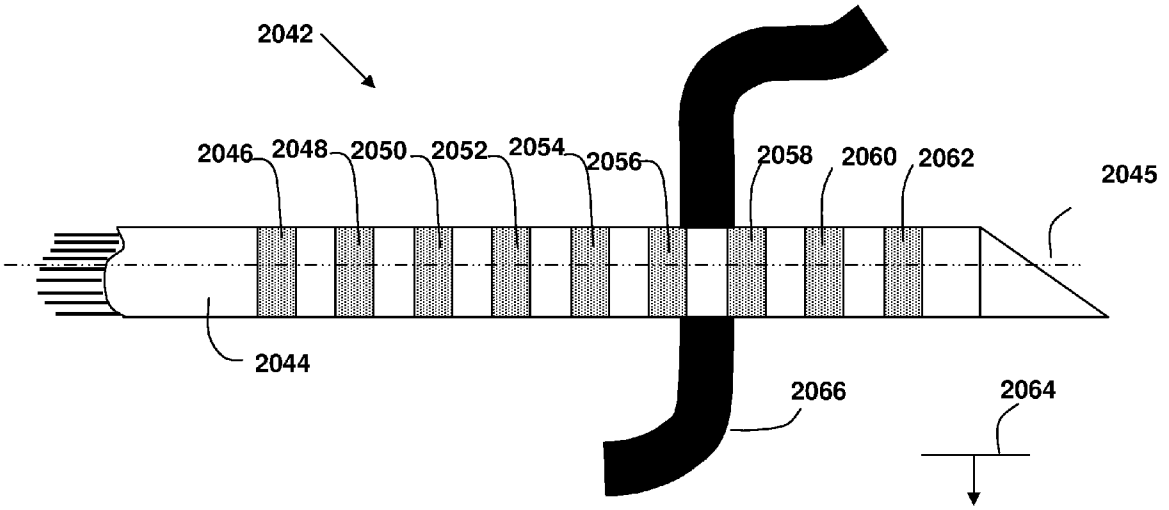


Fig. 16


2042
2046
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2054
2056
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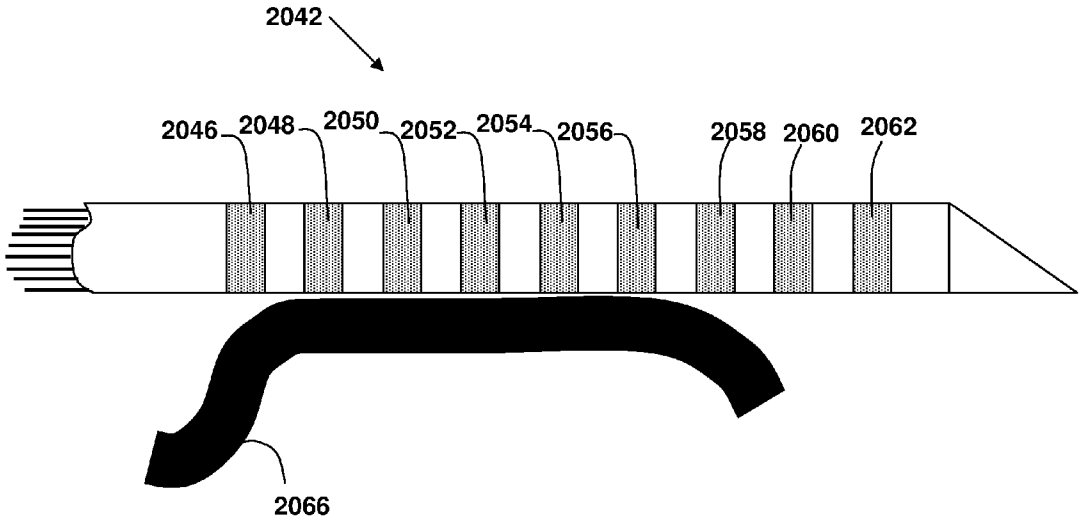
2062
2045
2044
2066
2064

FIG. 17


2042
2046
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2056
2058
2060
2062
2066

FIG. 18

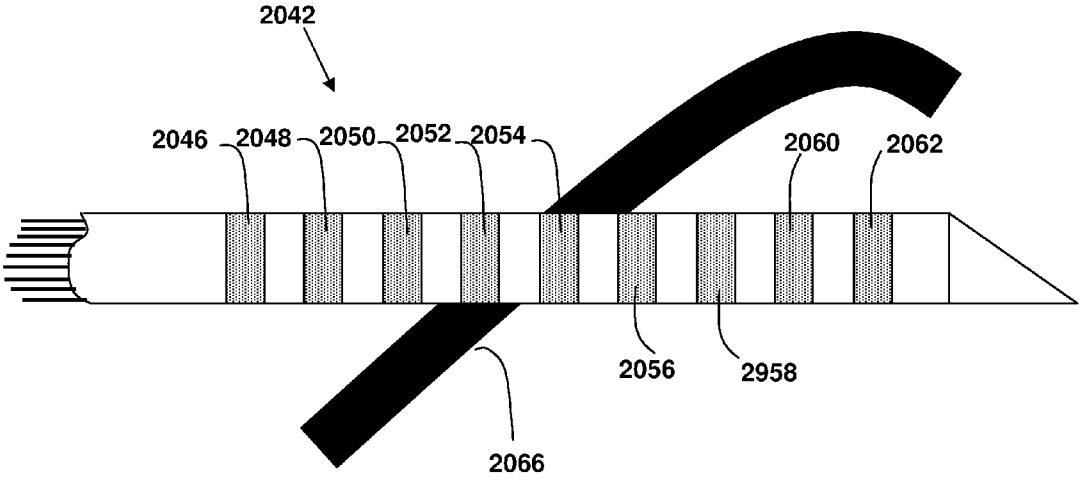

FIG. 19

ABLATION APPARATUS AND SYSTEM TO LIMIT NERVE CONDUCTION

RELATED APPLICATIONS

[0001] This application is a continuation-in-part of U.S. application Ser. No. 10/870,202, filed Jun. 17, 2004, entitled "Ablation apparatus and system to limit nerve conduction," now published, which is hereby incorporated by reference.

TECHNICAL FIELD

[0002] The present invention relates to a method and device used in the field of Minimally Invasive Surgery (or MIS) for interrupting the flow of signals through nerves. These nerves may be rendered incapable of transmitting signals either on a temporarily (hours, days or weeks) or a permanent (months or years) basis. One embodiment of the apparatus includes a single puncture system which features electrodes capable of creating areas of nerve destruction, inhibition and ablation.

BACKGROUND OF THE INVENTION

[0003] The human nervous system is used to send and receive signals. The pathway taken by the nerve signals conveys sensory information such as pain, heat, cold and touch and command signals which cause movement (e.g. muscle contractions).

[0004] Often extraneous, undesired, or abnormal signals are generated (or are transmitted) along nervous system pathways. Examples include, but are not limited to, the pinching of a minor nerve in the back, which causes extreme back pain. Similarly, the compression or other activation of certain nerves may cause referred pain. Certain diseases also may compromise the lining of nerves such that signals are spontaneously generated, which can cause a variety of maladies, from seizures to pain or (in extreme conditions) even death. Abnormal signal activations can cause many other problems including (but not limited to) twitching, tics, seizures, distortions, cramps, disabilities (in addition to pain), other undesirable conditions, or other painful, abnormal, undesirable, socially or physically detrimental afflictions.

[0005] In other situations, the normal conduction of nerve signals can cause undesirable effects. For example in cosmetic applications the activation of the corrugator supercilli muscle causes frown lines which may result in permanent distortion of the brow (or forehead); giving the appearance of premature aging. By interruption of the corrugator supercilli activation nerves, this phenomenon may be terminated. Direct surgical interruption of nerves is however a difficult procedure.

[0006] Traditional electrosurgical procedures use either a unipolar or bipolar device connected to that energy source. A unipolar electrode system includes a small surface area electrode, and a return electrode. The return electrode is generally larger in size, and is either resistively or capacitively coupled to the body. Since the same amount of current must flow through each electrode to complete the circuit; the heat generated in the return electrode is dissipated over a larger surface area, and whenever possible, the return electrode is located in areas of high blood flow (such as the biceps, buttocks or other muscular or highly vascularized area) so that heat generated is rapidly carried away, thus preventing a heat rise and consequent burns of the tissue. One advantage of a unipolar system is the ability to place the unipolar probe exactly where it is needed and optimally focus electrosurgical energy where desired. One disadvantage of a unipolar system is that the return electrode must be properly placed and in contact throughout the procedure. A resistive return electrode would typically be coated with a conductive paste or jelly. If the contact with the patient is reduced or if the jelly dries out, a high-current density area may result, increasing the probability for burns at the contact point.

[0007] Typical bipolar electrode systems are generally based upon a dual surface device (such as forceps, tweezers, pliers and other grasping type instruments) where the two separate surfaces can be brought together mechanically under force. Each opposing surface is connected to one of the two source connections of the electrosurgical generator. Subsequently, the desired object is held and compressed between the two surfaces. When the electrosurgical energy is applied, it is concentrated (and focused) so that tissue can be cut, desiccated, burned, killed, stunned, closed, destroyed or sealed between the grasping surfaces. Assuming the instrument has been designed and used properly, the resulting current flow will be constrained within the target tissue between the two surfaces. One disadvantage of a conventional bipolar system is that the target tissue must be properly located and isolated between these surfaces. Also, to reduce extraneous current flow the electrodes can not make contact with other tissue, which often requires visual guidance (such as direct visualization, use of a scope, ultrasound or other direct visualization methods) so that the target tissue is properly contained within the bipolar electrodes themselves, prior to application of electrical energy.

[0008] In recent years, considerable efforts have been made to refine sources of RF or electrical energy, as well as devices for applying electrical energy to specific targeted tissue. Various applications such as tachyarrhythmia ablation have been developed, whereby accessory pathways within the heart conduct electrical energy in an abnormal pattern. This abnormal signal flow results in excessive and potentially lethal cardiac arrhythmias. RF ablation delivers electrical energy in either a bipolar or unipolar configuration utilizing a long catheter, similar to an electrophysiology (EP) catheter. An EP catheter consisting of a long system of wires and supporting structures normally introduced via an artery or vein which leads into the heart is manipulated using various guidance techniques, such as measurement of electrical activity, ultrasonic guidance, and/or X-ray visualization, into the target area. Electrical energy is then applied and the target tissue is destroyed.

[0009] A wide variety of technology in the development of related systems, devices and EP products has already been disclosed. For example, U.S. Pat. No. 5,397,339, issued Mar. 14, 1995, describes a multipolar electrode catheter, which can be used to stimulate, ablate, obtain intercardiac signals, and can expand and enlarge itself inside the heart. Other applications include the ability to destroy plaque formations in the interior of lumens within the body; using RF energy applied near, or at the tip of, catheters such as described in U.S. Pat. No. 5,454,809 and U.S. Pat. No. 5,749,914. In these applications a more advanced catheter which is similar to the EP catheters described above contains an array of

electrodes that are able to selectively apply energy in a specific direction. Such devices allow ablation and removal of asymmetric deposits or obstructions within lumens in the body. U.S. Pat. No. 5,098,431 discloses another catheter based system for removing obstructions from within blood vessels. Parins, in U.S. Pat. No. 5,078,717 discloses yet another catheter to selectively remove stenotic lesions from the interior walls of blood vessels. Auth in U.S. Pat. No. 5,364,393 describes a modification of the above technologies whereby a small guide wire which goes through an angioplasty device and is typically **110** cm or longer has an electrically energized tip, which creates a path to follow and thus guides itself through the obstructions.

[**0010**] In applications of a similar nature, catheters which carry larger energy bursts, for example from a defibrillator into chambers of the heart have been disclosed. These catheters are used to destroy both tissues and structures as described in Cunningham (U.S. Pat. No. 4,896,671).

[**0011**] Traditional treatments for the elimination of glabellar furrowing have included surgical forehead lifts, resection of corrugator supercilli muscle, as described by Guyuron, Michelow and Thomas in *Corrugator Supercilli Muscle Resection Through Blepharoplastylncision.*, Plastic Reconstructive Surgery 95 691-696 (1995). Also, surgical division of the corrugator supercilli motor nerves is used and was described by Ellis and Bakala in *Anatomy of the Motor Innervation of the Corrugator Supercilli Muscle: Clinical Significance and Development of a New Surgical Technique for Frowning.*, J Otolaryngology 27; 222-227 (1998). These techniques described are highly invasive and sometimes temporary as nerves regenerate over time and repeat or alternative procedures are required.

[**0012**] More recently, a less invasive procedure to treat glabellar furrowing involves injection of botulinum toxin (Botox) directly into the muscle. This produces a flaccid paralysis and is best described in The New England Journal of Medicine, 324:1186-1194 (1991). While minimally invasive, this technique is predictably transient; so, it must be re-done every few months.

[**0013**] Specific efforts to use RF energy via a two needle bipolar system has been described by Hernandez-Zendejas and Guerrero-Santos in: *Percutaneous Selective Radio-Frequency Neuroablation in Plastic Surgery*, Aesthetic Plastic Surgery, 18:41 pp 41-48 (1994) The authors described a bipolar system using two parallel needle type electrodes. Utley and Goode described a similar system in Radiofrequency Ablation of the Nerve to the Corrugator Muscle for Elimination of Glabellar Furrowing, Archives of Facial Plastic Surgery, January-March, 99, VI P 46-48, and U.S. Pat. No. 6,139,545. These systems were apparently unable to produce permanent results possibly because of limitations inherent in a two needle bipolar configuration. Thus, as is the case with Botox, the parallel needle electrode systems would typically require periodic repeat procedures.

[**0014**] There are many ways of properly locating an active electrode near the target tissue and determining if it is in close proximity to the nerve. Traditional methods in the cardiac ablation field have included stimulation by using either unipolar and bipolar energy by means of a test pacemaker pulse prior to the implantation of a pacemaker or other stimulation device. A method of threshold analysis called the 'strength duration curve' has been used for many years. This curve consists of a vertical axis (or Y-axis) typically voltage, current, charge or other measure of amplitude, and has a horizontal axis (or X-axis) of pulse duration (typically in milliseconds). Such a curve is a rapidly declining line, which decreases exponentially as the pulse width is increased.

[**0015**] Various stimulation devices have been made and patented. One process of stimulation and ablation using a two-needle system is disclosed in U.S. Pat. No. 6,139,545. The stimulation may also be implemented negatively, where tissue not responsive to stimulation is ablated as is described in U.S. Pat. No. 5,782,826 (issued Jul. 21, 1998).

SUMMARY OF THE INVENTION

[**0016**] One aspect of the present invention is an electrosurgical probe including a probe body which defines a longitudinal probe axis. Thus the probe resembles a single needle and can be placed into tissue through a single opening. The electrosurgical probe also includes a first and second conductive electrode, each disposed along the probe axis. The surface area of the first conductive electrode is, in this aspect of the invention, greater than the surface area of the second conductive electrode. The ratio of the surface area of the first conductive electrode to the surface area of the second conductive electrode may be equal to or greater than 3:1 or equal to or greater than 8:1. The ratio of the surface area of the first conductive electrode to the surface area of the second conductive electrode may be adjustable.

[**0017**] The electrosurgical probe of the subject invention may further include a stimulation energy source in electrical communication with either the first or the second conductive electrode. Similarly, the electrosurgical probe may also include an ablation energy source communicating with either the first or second conductive electrode. A switch may be provided for the selective connection of the stimulation energy source or the ablation energy source to at least one of the conductive electrodes. Either the first or the second conductive electrode may be nearer the point of the electrosurgical probe at one end of the probe axis.

[**0018**] Another aspect of the present invention is an electrosurgical probe including a probe body defining a longitudinal probe axis, an active electrode operatively associated with the probe body at a first location along the probe axis, a stimulation electrode associated with the probe body at a second location along the probe axis and a return electrode operatively associated with the probe body at a third location along the probe axis. The stimulation electrode may be positioned between the active and return electrodes. The electrosurgical probe of this embodiment may further include a stimulation energy source in electrical communication with the stimulation electrode. The stimulation energy source may provide variable stimulation current. Either the active electrode, the return electrode or both may be connected to a ground for the stimulation energy source. Alternatively, a separate ground may be employed. This aspect of the present invention may also include an ablation energy source connected to the active electrode. The ablation energy source may be configured to provide variable ablation energy.

[**0019**] Another aspect of the present invention is an electrosurgical probe also having a probe body defining a longitudinal probe axis. At least three electrodes will be

associated with the probe body at distinct and separate locations along the probe axis. A stimulation energy source connected to at least one of the electrodes is also included.

[0020] The stimulation energy source of this embodiment of the present invention may be configured to provide variable stimulation energy. In addition, the stimulation energy source may be selectively connected by means of a switch to at least one or more of the various electrodes. Similarly, a ground for the stimulation energy source may be selectively connected to one or more of the electrodes.

[0021] Another aspect of the present invention is a method for positioning an electrosurgical probe. The method includes providing an electrosurgical probe such as those described immediately above, inserting the electrical surgical probe to a first position within tissue containing a target nerve and applying stimulation energy to an electrode. Upon the application of stimulation energy, a first response of a muscle associated with the target nerve may be observed. Thereupon, the electrosurgical probe may be moved to a second position and a second application of stimulation energy may be undertaken. The method further includes observing a second response of a muscle associated with the target nerve and comparing the second response with the first response. The method may also include varying the level of stimulation energy between the first and second applications of stimulation current. If the electrosurgical probe provided to implement the method has a third electrode, stimulation energy may be applied to a select third electrode as well. Certain advantages will be observed with respect to positioning the electrosurgical probe if stimulation energy is sequentially applied to first, second, third and subsequent electrodes.

BRIEF DESCRIPTION OF THE DRAWINGS

[0022] FIG. **1** Bi-Polar Driver System.

[0023] FIG. **2** Schematic diagram of the bi-polar needle.

[0024] FIG. **2**A Schematic diagram of the split bi-polar needle.

[0025] FIG. **3**A Magnified side view of conical bi-polar probe.

[0026] FIG. **3**B Magnified side view of hollow chisel bi-polar probe.

[0027] FIG. **3**C Magnified side view of tapered conical bi-polar probe.

[0028] FIG. **3**D Magnified side view of split conical bi-polar probe.

[0029] FIG. **4** Schematic diagram of the bi-polar driver system.

[0030] FIG. **5**A Ablation Procedure without Auxiliary probe.

[0031] FIG. **5**B Ablation Procedure with Auxiliary probe.

[0032] FIG. **6**. Side view Hybrid bi-polar needle for nerve ablation.

[0033] FIG. **6**A Side view Hybrid bi-polar needle for tumor ablation.

[0034] FIG. **7** Side view of auxiliary nerve probe.

[0035] FIG. **7**A Side view of auxiliary dual-tipped nerve probe.

[0036] FIG. **8** Side view of guided ablation procedure with auxiliary nerve probe(s).

[0037] FIG. **9** Sample electro-surgery waveforms.

[0038] FIG. **10** Side view of visually guided ablation procedure.

[0039] FIGS. **11**-**11**A Controller and probe data base structure.

[0040] FIG. **12** is a side view of a single axis electrosurgical probe having equal surface area electrodes.

[0041] FIG. **13** is a side view of a single axis electrosurgical probe having two electrodes of differing surface areas.

[0042] FIG. **14** is a side view of a single axis electrosurgical probe having two electrodes of differing surface areas.

[0043] FIG. **15** is a side view of a single axis electrosurgical probe having three electrodes.

[0044] FIG. **16** is a side view of a single axis electrosurgical probe having three electrodes and a curved handle portion.

[0045] FIG. **17** is a side view of a single axis electrosurgical probe having multiple electrodes transverse a nerve.

[0046] FIG. **18** is a side view of a single axis electrosurgical probe having multiple electrodes parallel to a nerve.

[0047] FIG. **19** is a side view of a single axis electrosurgical probe having multiple electrodes crossing a nerve at an angle.

[0048] Certain terms used herein are defined as follows:

[0049] Medical Terms

[0050] Corrugator supercili muscles—skeletal muscles of the forehead that produce brow depression and frowning.

[0051] Cepressor anguli oris—skeletal muscle of the corner of the mouth that produces depression of the corner of the mouth.

[0052] Depressor labii inferioris—skeletal muscle of the lower lip that causes the lip to evert and depress downward.

[0053] Dystonias—medical condition describing an aberrant contraction of a skeletal muscle which is involuntary.

[0054] Frontalis—skeletal muscle of the forehead that produces brow elevation or raising of the eyebrows.

[0055] Hyperhidrosis—condition of excessive sweat production.

[0056] Masseter—skeletal muscle of the jaw that produces jaw closure and clenching.

[0057] Mentalis—skeletal muscle of the lower lip and chin which stabilizes lower lip position.

[0058] Orbicularis oculio—skeletal muscle of the eyelid area responsible for eyelid closure.

[0059] Orbicularis ori—skeletal muscle of the mouth area responsible for closure and competency of the lips and mouth.

[0060] Parasymapathetic—refers to one division of the autonomic nervous system.

[0061] Platysma myoides—skeletal muscle of the neck that protects deeper structures of the neck.

[0062] Platysma—same as above.

[0063] Procerus muscles—skeletal muscle of the central forehead responsible for frowning and producing horizontal creasing along the nasofrontal area.

[0064] Procerus—same as above.

[0065] Rhinorrhea—excessive nasal mucous secretions.

[0066] Supercilli—a portion of the corrugator muscle that sits above the eyelids.

[0067] Temporalis—skeletal muscle of the jaw that stabilized the temporamandibular joint.

[0068] Zygomaticus major—skeletal muscle of the face that produces smiling or creasing of the midface.

[0069] Electrical Terms.

[0070] ADC: Analog to digital converter.

[0071] ASCII: American standard of computer information interchange.

[0072] BAUD: Serial communication data rate in bits per second.

[0073] BYTE: Digital data 8-bits in length.

[0074] CHARACTER: Symbol from the ASCII set.

[0075] CHECKSUM: Numerical sum of the data in a list.

[0076] CPU: Central processing unit.

[0077] EEPROM: Electronically erasable programmable read only memory.

[0078] FLASH MEMORY: Electrically alterable read only memory. (See EEPROM)

[0079] UI: Graphical user interface.

[0080] HEXADECIMAL: Base **16** representation of integer numbers.

[0081] 12C BUS: Inter Integrated Circuit bus. Simple two-wire bidirectional serial bus developed by Philips for an independent communications path between embedded ICs on printed circuit boards and subsystems.

[0082] The I2C bus is used on and between system boards for internal system management and diagnostic functions.

[0083] INTERRUPT: Signal the computer to perform another task.

[0084] PC: Personal computer.

[0085] PWM: Pulse-width modulation.

[0086] ROM: Read only memory.

[0087] WORD: Digital data **16**-bits in length

DETAILED DESCRIPTION OF THE INVENTION

[0088] FIG. **1** illustrates two main components and one optional component, which are the energy generator **400**, the probe **371** (alternate probes are described in FIGS. **3**A-D) and optionally probes **771** or **772** that may be used.

[0089] In normal operation, the novel probe **371** would combine a unique bipolar configuration in a single MIS needle, is inserted into the patient using MIS techniques. The probe, which may contain and/or convey various functions described later, is initially guided anatomically to the region of the anticipated or desired location. Various means of locating the tip **301** are utilized of placing the zone of ablation in the proper area to interrupt signal flows through the nerve **101**.

Device Operation

[0090] Many combinations of electrode diameters and tip shapes are possible. The 'novel' probe performs a variety of functions, such as stimulation, optical and electronic guidance, medication delivery, sample extraction, and controlled ablation. This bi-polar electrode is designed as a small diameter needle inserted from a single point of entry thus minimizing scaring and simplifying precise electrode placement. This low cost, compact design provides a new tool to the art.

[0091] Probes may emit fiber optic illumination for deep applications using electronic guidance as taught in FIGS. **1** and **8**. The invention offers a simple low cost ablation probe that is capable of performing precise ablation while minimizing damage to nearby tissue structures. The metered ablation energy and precise probe targeting give the practitioner a tool is also not available in prior art. The practitioner has unprecedented control of treatment permanence in a minimally invasive procedure. Such a procedure is typically performed in less than one hour with only local anesthetic and would require no stitches or chemicals common to prior medical art.

[0092] Stimulation/Ablation

[0093] First the probe electrode **301** must be in the desired location relative to the target nerve **101** (FIG. **4**), then the user initiates the treatment via switch(s) **410** and **310** using the selected power setting **404** (FIG. **4**). The controller configures the generators **411** (FIG. **4**) and **412** to the amplitude frequency and modulation envelope, delivering 50 KHz-2.5 MHz of 5 to 500 watts of available energy. The summing junction **413** combines the RF outputs as the application requires and passes them to the pulse-width modulator **415** for output power control. The output of modulation generator **420** is applied to the multiplier **415** with radio frequency RF signals **422** and **423**. This permits complex energy profiles to be delivered to a time variant non-linear biologic load. All of these settings are based on the information provide to the generator by the installed probe **371** the selected power **404** settings, and the modulation envelope **420** (FIG. **4**) settings, which are then loaded by the generator **421**.

[0094] For example, both a high amplitude sine wave **910** (FIG. **9**), used for cutting, and a pulse-width modulated (or PWM) sine wave **920**, used for coagulation, are well known to electro-surgery art. Precise power rates and limits of average total power are controlled via integrator **435** minimizing damage to nearby structures or burning close to the skin for shallow procedures. Where nearby structures **111**(FIG. **2**A) are too close to be avoided by electrodes such as **371** (FIG. **3**), **372** (FIG. **3**A), and **372** (FIG. **3**B), addi-

tional probe geometries as taught in FIGS. **3**D, **6** and **6**A offer novel methods to direct energy and limit ablation to a smaller region, thereby avoiding other structures. For safety a hardwired switch **436** disables the power amplifier in the event of a system fault, the probe is unplugged or over power condition, thus protecting both the patient and practitioner.

[**0095**] The output of the modulator **415** is applied to the input of the power amplifier **416** section. The power amplifier's **416** outputs are then feed into the impedance matching network **418**, which provides dynamic controlled output to the biologic loads that are highly variable and non-linear, and require dynamic control of both power levels and impedance matching. The tuning of the matching network **418** is performed for optimal power transfer for the probe, power level, and treatment frequencies settled. The system's peak power is 500 watts for this disclosed embodiment. Precise control is established by the proximity of the tip and the control loops included in the generator itself The final energy envelope **420** is delivered to probe tip **301** and return electrodes **302**.

[**0096**] This precise control of energy permits extension of the ablation region(s), **140** and **1203** (FIG. **10**), and the duration of treatment efficiency. Low or medium energy settings **404** permit temporary nerve-conduction interruption for 3-6 months. Higher energy settings at **404** may result in a longer nerve conduction interruption of 1 year to permanent. In the prior art, procedures had little control over duration of termination of such signal flow through the nerve. This invention gives the practitioner enhanced control of such duration. Patients can evaluate controlled temporary treatment before choosing longer or permanent treatment options.

[**0097**] A low energy nerve stimulator **771** has been integrated into the system to assist in more precise identification of nearby structures and for highly accurate target location. Lastly, additional sensors, such as temperature **311**, voltage, frequency, current and the like are read directly from the device and/or across the communications media **403** to the probe.

[**0098**] Directed Ablation

[**0099**] In addition to the substantial radially-symmetric ablation patterns with probes as taught in **371** (FIG. **3**) and **372**, switching or dividing ablation power to multiple electrodes (FIG. **3**D) can generate an asymmetric ablation zone. This high intensity source **608** with probe **610** (FIGS. **6** and **6**A) minimizes damage to nearby structures **111** or the burning of skin **330** in shallow procedures. Also, FIGS. **2**A and **3**D identify probe configurations for selective or asymmetric ablation.

[**0100**] Power Feedback

[**0101**] The power amplifier output**430** and buffered the feedback signals **437** are connected to an Analog to Digital converter (or ADC) **431** for processor analysis and control. Said signals **437** control power modulation **420** settings and impact the impedance matching control signals **419**. This integrated power signal **437** is recorded to the operating-condition database (FIG. **11**) for later procedure review. This power level is also compared to reading taken from the probe **1492** (FIG. **11**A) as compared against procedure maximums, which if exceeded will in turn disable the amplifier output, thereby protecting the patient from error or equipment fault. Similarly, limits from the probe and generator sensors such as temperature **330** are also used to terminate or substantially reduce the modulated power levels and ultimately the procedure.

[**0102**] Probe Identification

[**0103**] At power startup, the controller **401**(FIG. **4**) reads the probe status and internal identification kept within the probe itself **331** (and **371**) via serial communications **403** (or bus). Serial communications is used because it is commonly available to most single-chip microprocessors. This or similar methods (e.g. I2C, or SPI) may be used, but this disclosed embodiment will use serial for its simplicity. Serial communications **403** permits the generator to address and control EEROM memory **331**, temperature sensors **330**, processors, ADC and DACs within the single-chip microprocessor embedded in the probe itself The user selects the desired power setting **404** and based on probe identification read from the EEROM or microprocessor **331** makes the appropriate configurations. The probe **371** is connected via cable **1334** (FIG. **1**) to control unit **101** or generator. This probe is not intended for multiple procedural uses. So to prevent such use of the probe, the controller **401** (FIG. **4**) reads the stored time register from ID memory module **331**. If the probe's initialized time **1467** (FIG. **14**) is zero, the current real-time clock **482** value is written to probe's **331**'s initial time register via serial bus **403**. If time read on module **331** is non-zero, the probe's initial time register is added to two(2) times the procedural time (based on the probe type) FIG. **141420**. If that value when compared to current real-time clock **482**, is less than current time, the controller will alert the practitioner via display **450**, speaker **451** and, flashing probe illumination **608**, that the procedure will be terminated and the probe rendered invalid.

[**0104**] The controller **401** also verifies selected procedure **1415** (FIG. **11**) for compatibility with installed probe. If incompatible, the user is also prompted to select a different power setting **404**, procedure, or probe **371**. If probe **371** matches power setting **404**, the system enables power amplifier **416**, guide light source **408**, and low-voltage nerve simulation **732**. Both of these procedures are enforced by a mandatory "hand shake" protocol and the serialized information, which must be present and properly verified by the electronic circuitry for a procedure to be instituted. During a clinical procedure, information is required to be conveyed by the embedded electronics contained within the probe, which provides another way of enforcing this protection and thus again preventing unauthorized re-use. The ultimate goal is prevent cross-contamination between patients. The probe will accomplish this by being unique, serialized, and given the above procedures. Once plugged in, the probe will enter the serial number into the data logging system via the serial bus **403** and circuit logic will thereafter prevent re-use of the probe and cross-contamination that would occur. Further, this scheme will prevent the use of unauthorized third party probes, for they will not be activated, preventing potential inferior or uncertified probes from being used and presenting potential danger to the patient.

[**0105**] Nerve Target Location Tools

[**0106**] Prior to treatment, the practitioner may use auxiliary probe **771**(FIG. **4**), to locate target **101** and nearby structures **111** as taught in FIGS. **4**, **7**, **7**A, **8**, and **10**. When needle **771** is in place, the practitioner may locate and place

a mark or marks on the surface of the skin **755** (see FIGS. **7** and **8**) or leaves auxiliary probe **771** in place. For shallow sub-cutaneous procedures, probe tip illumination **448** from source **408** is visible to practitioner aiding in probe placement to pre-marked location.

[**0107**] Location Via Florescence Marker Dye.

[**0108**] In other procedures, whereby somewhat larger targets are sought, such as more diffuse nerve structures or small areas of abnormal growth (e.g. such as cancer) the injection of specially designed dyes that attach to target structures are used, as taught in FIG. **6**A. The probe **610** (FIG. **6**) is moved into the proximity of the target **671**. The light source **608** illuminates quantum-dot/dye tagged antibody **670**. The dye fluoresces **675** at a frequency/wavelength of a particular material and will typically emit light in the visible to infrared (or IR) or potentially other wavelength regions. The return fiber(s) **680** deliver emissions **675** to the detector **478** for measurement and are the result is then displayed on bar graph **554** (FIG. **1**) and/or an audio tone sounded via speaker **451** based on proximity. Visible and IR light emissions propagate over limited distances permitting additional external detectors **678** to be used for shallow targets just under the skin **330**. Location via this method is similar to the electronically guided probe method taught in FIG. **8** where probe **610** movement maximizes the signal output when in close proximity. IR emissions propagate and can permit deeper (typically several centimeters) detection with optional additional external sensors **678**. Unfortunately, many dyes fluoresce in the visible region making external detection imposable for deep targets or when obscured by bone. However, probe **610** (FIG. **6**A) solves this problem by integrating target illumination **674**, emission **675** detector, ablation, biopsy, and medication delivery in single compact probe. Electronic probe guidance (FIG. **8**) if required is used in combination with florescence detection to rapidly locate target. The instant invention offers a minimally invasive system for locating and treating small/deep tumors and other tissue that are to be ablated, destroyed or removed.

[**0109**] Electronic Probe Guidance

[**0110**] Low energy nerve stimulation current **810** (FIG. **8**) assist in locating desired treatment region and avoiding nearby structures. Probe **771** is selectable between nerve stimulator and current measurement to/from auxiliary probe tip **702**(FIG. **8**). Return electrode **736** provides a return path for local ground **735**. Ablation probe switch **367** selects low-energy stimulator/receiver and high-energy ablation to/from probe **372**. Amplitude of measured guidance current **811** and light **478** are transmitted to display **554**, and audio feedback **452** through the speaker **451**.

[**0111**] Optical Probe Guidance

[**0112**] Disclosed invention provides optical sources **408** that aid in probe placement (FIG. **10**) by supplementing stimulation source **732** and acting as preliminary guide. Probe **771** is selectable between nerve stimulator or current **811** measurement and to or from the auxiliary probe tip **702**. The ablation probe switch **367** selects low-energy stimulator/receiver or high-energy ablation to or from probe **371**, **372**, **373**, and **374**. In this mode, the physician operator will have previously placed marks **755** on the surface of the skin by various means described. The physician operator **775** will then see the tip when the **448** if the optical illumination is turned on. It **448** will provide a bright spot under the skin indicating the location of the tip in relation to the marks **755**. The physician **775** will then guide the probe tip **301** into precise alignment under these marks **755** so as to enable ablation of that target tissue **101**.

[**0113**] Data and Voice

[**0114**] Real-time engineering parameters are measured such as average power **437**, luminous intensity **478**, probe current **811**, energy **438** and, temperature **330** to be recoded into USB memory **438**. Simultaneously, the internal parameters disclosed such as frequency **423**, modulation **420** and such are recoded into USB memory **438** as well. Additionally probe, patient, and procedure parameters (FIG. **11**) are written to local storage **438**. The practitioner dictates text and voice notes via microphone **455**, which are saved to memory **438** (FIG. **1**). All data and records are time stamped using the real-time clock **482**. This permits detailed post procedure graphing and analysis.

[**0115**] Data Transfer

[**0116**] At procedure conclusion, the system transfers the data **438** recorded to the USB removable memory **1338** and to a file server(s) **1309** and **1307**. In the disclosed embodiment, data transfer is performed over Ethernet connection **480**. Probe usage records **1460**(FIG. **11**) that are stored in local memory **438** are then written to removable memory module **1338**. Parallel records are mirrored to local storage **1309** and remote server **1306** storage **1307** via Ethernet connection **480** or similar means. Sensitive records are encrypted and transferred via secure network connection and also written to removable module **1320**. The database contained on the remote server tracks the following information: equipment by manufacture, probe accessory inventory, usage, billing, repair/warranty exchange information, and program recorders. As a system **400** is certified for new procedures **1410** (FIG. **11**), the relational databases are automatically updated to reflect new billing/procedure codes **1416**, potential power settings **1417** and the like. This insures that the equipment is current and alerts the practitioner to new probes/procedures as they are developed and certified.

[**0117**] Before further explaining the disclosed embodiment of the present invention in detail, it is to be understood that the invention is not limited in its application or to the details of the particular arrangement shown. The invention is capable of other embodiments. Further, the terminology used herein is for the purpose of describing the probe and its operation. Each apparatus embodiment described herein has numerous equivalents.

[**0118**] FIG. **1** Bi-Polar Driver System

[**0119**] FIG. **1** identifies the two required components of the system, various modules and optional items. The two components always utilized during a procedure will be the energy generator/controller/data storage device **400** and probe **371**. **400** contains advanced electronic systems capable of recognizing a properly authorized probe, preventing re use of a previously used probe, generating appropriate energy as described, performing safety checks, storing data, and other functions as described. Main functions of **400** may include, but not be limited to, generation of light, generation of location-stimulation currents, generation of ablation energies, data logging, storage, communication and retrieval,

and other functions critical to a MIS procedure. Probe **371** and its various forms are single puncture bipolar surgical tools that may be used in identifying proper location of its tip **301**, in relation to target tissue **101** which is desired to be ablated, modified or destroyed. Probe **771** and its various derivatives may optionally be used to assist in locating and properly positioning tip **301** of probe **371**.

[**0120**] FIG. **2** Isometric View of the Bi-Polar Probe

[**0121**] Bi-polar probe **310** represents probes **371**, **372**, **373** shown in FIGS. **3**A-C with exception to type of needlepoint on the probe. FIG. **3**D varies from the other because it has a split return probe. Bi-polar probe **310** (not drawn to scale) consists of insulating dielectric body **309** made from a suitable biology inert material, such as Teflon, PTFE or other insulative material, covering electrode **302** except for where **302** is exposed as a return electrode. Conductive return electrode **302** tube is fabricated from medical grade stainless steel, titanium or other conductive material. Hollow or solid conductive tip electrode **301** protrudes from surrounding dielectric insulator **305**. Sizes of **309**, **302**, **305**, and **301** and its inner lumen (diameter, length, thickness, etc.) may be adjusted so as to allow for different surface areas resulting in specific current densities as required for specific therapeutic applications.

[**0122**] Hollow Electrode **301** often used as a syringe to deliver medication such as local anesthetic. Tip electrode **301** is connected to power amplifier **416** via impedance matching network **418** (FIG. **4**). Return electrode(s) **302** delivers return current to power amplifier **416** via impedance matching network **418**. Dielectric insulator in the disclosed embodiment is a transparent medical grade polycarbonate acting as a light pipe or fiber optic cable. Light source LED or laser **408** (FIG. **4**) provides illumination at the far end of the probe via fiber optic cable/transparent dielectric **305** for guiding the probe under the skin i.e. shallow procedures. In an alternate embodiment dielectric insulator is replaced with a plurality of optical fibers for viewing and illumination as taught in FIG. **6**.

[**0123**] Ablation regions **306** and **140** extend radially about electrode **301** generally following electric field lines. For procedures very close to skin **330** a chance of burning exists in region **306**. To minimize the chance of burning, a split return electrode probe **374** in FIG. **3**D is offered. Thereby concentrating the current away from region **306** to **140** or vice versa. In FIG. **2**A, insulator **307** splits the return electrode into two sections **302** and **303**, dividing return current ratio from 0-50%, which may also be selectively activated. Active electrodes are also split into two sections **301** and **311** so energy may be directed in a desired direction. This electrode configuration is identified on the proximal portion of the probe so the operator may position the needle and electrodes accordingly. FIG. **6** teaches a laser directed ablation for more precise energy delivery.

[**0124**] FIG. **2**A Isometric View of Split Bi-Polar Probe.

[**0125**] The bi-polar probe **380** (not drawn to scale) consists of an insulating dielectric body **309** made from a suitable biologically inert material, such as Teflon PTFE or other electrical insulation, that covers split return electrodes **302** and **303**. The disclosed conductive return electrodes **302** and **303** are fabricated from medical grade stainless steel, titanium or other electrically conductive material. Hollow or solid split conductive tip electrodes **301** and **311** protrude from the surrounding dielectric insulator **305**. The operation of the hollow/split conductive tip is very similar to probe tip **310** as taught in FIG. **3**D. Ablation regions **1203** (FIG. **10**) and **140-144** extend radially about electrode **301** generally following electric field lines. For procedures very close to skin **330** a chance of burning exists in region **306**. To minimize chance of burning a split return electrode probe **311** is used, thereby concentrating the current away from region **306** to **140**. For procedures where there is a risk to nearby structures **111**, the ablation region **1203** must be a non-radial ablation zone. The disclosed split electrode **380** permits dividing or splitting energy delivered to electrode pairs **301**/**302** and **311**/**303**. The disclosed division or ratio between pairs is 0-100%. Dual amplifiers or time multiplexing/switching main amplifier, **416** located between electrode pairs, directs energy to target **101** avoiding **111**. This simple switch network reliably ratios electrical energy while minimizing damage to nearby structures.

[**0126**] FIG. **3**A Conical Bi-Polar Needle

[**0127**] Bi-polar probe **371** discloses conical shaped electrode **301** and tip **351** for minimally invasive single point entry. Probe diameter **358** is similar to a 20-gage or other small gauge syringe needle, but may be larger or smaller depending on the application, surface area required and depth of penetration necessary. In disclosed embodiment, electrode shaft **302** is **30** mm long with approximately 5 mm not insulated. Lengths and surface areas of both may be modified to meet various applications such as in cosmetic surgery or in elimination of back pain. The conductive return electrode **302** is fabricated from medical grade stainless steel, titanium or other conductive material. The dielectric insulator **305** in the disclosed embodiment is a transparent medical grade material such as polycarbonate, which may double as a light pipe or fiber optic cable. The high intensity light source **408** LED/laser (FIG. **4**) provides guidance Illumination **448** at working end of probe. The illumination source modulation/flash rate is proportional to the received stimulation current **810** as taught in FIG. **8**. A small diameter electrode permits a minimally invasive procedure that is typically performed with local anesthetic. This configuration may contain lumens for delivery of agents as described elsewhere.

[**0128**] FIG. **3**B Hollow Chisel.

[**0129**] The hollow chisel electrode **352** is often used as a syringe to deliver medication such as local anesthetic, medications,/tracer dye. The hollow electrode may also extract a sample. Dielectric insulator **305** in the disclosed embodiment is a transparent medical grade polycarbonate and performs as a light pipe or fiber optic cable. The novel dual-purpose dielectric reduces probe diameter and manufacturing costs. Light source **408**, typically a LED or laser (FIG. **4** not shown), provides Illumination **448** at the working end of probe. It provides an illumination source for guiding the probe under the skin. A second embodiment, as taught in FIG. **6**, dielectric insulator is replaced/combined with plurality of optical fibers for viewing/illumination.

[**0130**] FIG. **3**C Tapered Conical

[**0131**] The bi-polar probe **373** discloses a tapered conical shaped probe for minimally invasive single point entry. It is constructed similarly to probe **371** as taught in FIG. **3**A.

Probe tip is not drawn to scale to teach the tip geometry. In disclosed embodiment, electrode **301** is approximately **5** mm long and fabricated from medical grade stainless steel but may be of various lengths to accommodate specific application and surface area requirements. The solid tapered conductive tip electrode **353** protrudes from tapered dielectric insulator **305**. Transparent dielectric insulator **305** also performs as light pipe or fiber optic cable terminated to high intensity light source **408** (FIG. **4**) providing illumination **448**. The electrode assembly is mounted in an ergonomic handle **388** (which has not been drawn to scale). Handle **388** holds ablation on/off switch **310**, ablation/stimulation mode switch **367**, identification module **331** and terminations for cable **1334** (FIG. **13**). Temperature sensor **330** (located close to tip) monitors tissue temperature.

[**0132**] FIG. **3**D Split Conical Bi-Polar Probe

[**0133**] Description of this probe is described in both drawings **2**A and **3**D. Bi-polar probe **374** (not drawn to scale) consists of insulating dielectric body **309** made from a suitable biologically inert material, such as Teflon, that covers split return electrodes **302** and **303**. Conductive return electrodes **302** are fabricated from medical grade stainless steel, titanium or other suitable conductive material. Hollow or solid split conductive tip electrodes **301** and **311** protrude from surrounding dielectric insulator **305**. Their operation is very similar to probe tip **380** as taught in FIG. **2**A. Solid tapered conductive tip electrodes **311** and **301** protrude from transparent dielectric insulator **305**. Dielectric insulator **305** also performs as a light pipe or fiber optic cable terminated to high intensity light source **408** providing illumination **448**.

[**0134**] Probe handle (not drawn to scale) encloses memory module **331**, on/off switch **310** and mode switch **367**. Temperature sensor **330** (located close to tip) monitors tissue temperature. Split electrode **380** (FIG. **2**A) permits dividing or splitting energy delivered to electrode pairs **301**/**302** and **311**/**303**. Dual amplifiers or time multiplexing/switching main amplifier **416** are located between electrode pairs directing energy to target **101** avoiding **111** creating asymmetric ablation volume. A small diameter electrode needle is injected from a single point of entry minimizing scaring and simplifying precise electrode placement.

[**0135**] Connections consist of a tapered dielectric sleeve **309** covering the ridged stainless electrode tube **302**. Insulating sleeve **309** is made from a suitable biologically inert material, which covers electrode **302**. Dielectric **305** insulates conical tipped electrodes **351** and **301**.

[**0136**] FIG. **5**A Ablation Procedure (Without Auxiliary Probes)

[**0137**] Ablation probe **371** is inserted and directed anatomically into the area where the target nerve to be ablated (Box **531**) is located. Test current **811** is applied (Box **532**). If probe is located in the immediate proximity of the target nerve a physiological reaction will be detected/observed (Example: During elimination of glabellar furrowing, muscle stimulation of the forehead will be observed). If reaction is observed, then a mark may optionally be applied on the surface of the skin to locate the area of the nerve. Power is applied (Box **535**) in an attempt to ablate the nerve. If physiological reaction is not observed, (Box **534**) the probe will be relocated closer to the target nerve and the stimulation test will be repeated (Box **536** & **537**). If no physiological reaction is observed, the procedure may be terminated (Box **544**). Also, the probe may be moved in any direction, up, down, near, far, circular, in a pattern, etc. to create a larger area of ablation for a more permanent result.

[**0138**] In Box **537**, if stimulation is observed again, then the ablation power may be set higher (Box **538**), alternatively, as mentioned, the needle may be moved in various directions, or a larger dosage of energy may be reapplied, to form a larger area of ablation for more effective or permanent termination of signal conduction through the nerve. After delivery of power (Box **540**), stimulation energy may be applied again (Box **541**). If there is no stimulation, the procedure is completed (Box **544**). If there is still signal flow through the nerve (stimulation or physiological reaction) then the probe may be relocated (Box **542**) and the procedure is started over again (Box **533**).

[**0139**] FIG. **5**B Flow Chart of Visually Guided Ablation Procedure Using Auxiliary Probes Such As **771** and **772**.

[**0140**] Auxiliary probes **771** and **772** (FIGS. **7** and **7**A) provide a method to quickly and accurately locate target structure **101** and subsequently mark target location **755**. Auxiliary probes may be much smaller (like acupuncture needles) than ablation probes. Structures are marked typically with an ink or similar pen allowing the illuminated ablation probe **371** or other ablation probe to be quickly guided to mark **755**. Optionally, non-illuminated probes may be used allowing the practitioner to simply feel for the probe tip. For deep structures, probe **771**(FIG. **8**) us employed as an electronic beacon. Small current **811**, which is similar to the stimulation current but smaller, from probe tip **702** is used to guide ablation probe **372** (FIG. **8**).

[**0141**] Operation **530** (FIG.**5**B) inserts auxiliary probe **771** or **772** (FIGS. **7** and **7**A) thru skin **330** and muscle layer(s) **710** near nerve **101**. Target **101** depth **766** is measured (FIGS. **7** and **7**A) using auxiliary probe markings **765**. Decision **533** checks if the probe is in position if not adjustments are performed in **534**. Operation **532** enables nerve simulation current **811**. When muscle stimulation is obtained or physiological reaction is obtained, Auxiliary probe tip is in place. Depth may be noted by reading marks **765** and location marks **755** may be made in operation **535**. With the probe in position under mark in operations **536** and **537**, operation **538** sets power level **404** and closes ablation switch **410**. Alternatively, stimulation may be applied directly from the ablation probe as taught elsewhere. Operation **540** and controller **401** set generator **411** (FIG. **4**) frequencies, modulation **420** envelope and enables power amplifier **416** to deliver preset ablation energy. Region **1203** (FIG. **10**) shows the general shape of the ablation region for conical tip **301** for example.

[**0142**] Between each ablation, procedure **540** (FIG. **5**C) (nerve conduction) is tested in **541**. Probe amplifier **416** delivers small nerve stimulation current **811** from electrode **301** or Auxiliary probe **771** or both. Based on the nerve conduction test **541** if the desired level of conduction is achieved the procedure is compete. Operation **542** moves the probe to the next position and repeats conduction test **541**. If compete, the probe(s) is removed in operation **544**. Number and ablation intensity/energy are set by the particular procedure and the desired permanence. The practitioner selects the procedure/power level **404** (FIG. **4**) and control-

ler **401** compares the installed probe via identification **331** (FIG. **4**) for compatibility with selected procedure. The practitioner is alerted if the installed probe is incompatible with selected power range **404**.

[**0143**] As an example and not a limitation, five ablation regions (**140**, **141**, **142**, **143**, and **144**) are shown in FIG. **10**. Ablation starts with area **144**, then the probe is moved to **143** and so on to **140**. Alternatively, movement may be during insertion, moved laterally, in a circular manner or other manner to enlarge the area of targeted nerve destruction. Nerve responses may be tested after each ablation allowing the practitioner to immediately check the level of nerve conduction. Probe position and power adjustments are made before applying additional ablations if required. Accurate probe location tools and methods taught herein permit use of minimal ablation energy thereby minimizing damage to non-target structures. This translates to reduced healing time and minimal patient discomfort. The instant invention gives the practitioner a new tool to perform a minimally invasive nerve conduction limiting procedure with the ability to select, temporary or permanent nerve conduction interruption with a new level of confidence. This new tool offers a low cost procedure performed typically in office or outpatient setting often taking less than one hour with local anesthetic. In contrast to prior art where surgical procedures require stitches and longer healing intervals with limited control of permanence (nerve re-growth).

[**0144**] FIG. **6** Side View of the Bi-Polar Probe **610** With Enhanced Laser Targeting.

[**0145**] Probe insertion and placement is same as taught in FIG. **3**. Probe construction is the same as FIG. **3** with the dielectric **305** having embedded optical fibers **690** and **680** providing imaging/illumination. Additional fiber(s) **690-691** are illuminated by a high intensity laser source.

[**0146**] In special cases were target nerve **101** or ablation region **640** is in close proximity to second nerve **111** or skin **330** bi-polar probes **371** or **372** (FIG. **3**) create an annular ablation region between electrodes **301** and/or **302**, potentially damaging nearby structures such as other nerves **111**. With probe **610** in the desired position, laser **608** (FIG. **4**) is turned on target **670** (FIG. **6**A) with illuminating fiber(s) **690**. Fiber(s) transmitting high intensity laser light to ionized region **640** is illuminated by fiber(s) **690**. Simultaneous with laser illumination, RF energy **470** is delivered to electrodes **301** and **302**. A relatively low impedance path is created by the high intensity laser illumination wherein RF energy will follow this newly created path. Thus very specific regions may be selected for ablation. By permitting operation at a lower power, energy is concentrated where it is needed and eliminates or reduces damage to nearby structures such as skin **330** or nerves **111**. Probe **610** improves on the already very precise ablation taught in FIG. **3** with the addition of a low power laser (or other type light source) and fiber delivery system. In the disclosed embodiment a diode pumped Nd:YAG (Neodymium Doped Yttrium Aluminum Garnet) laser is offered as an example and not a limitation.

[**0147**] FIG. **6**A Side View is the Florescence Emission Guided Hybrid Bi-Polar Tumor Probe.

[**0148**] Probe construction is similar to FIGS. **3**A and **6** with dielectric **305** embedded with a plurality of optical fibers **380**, **690**, and **680** for illumination detection/imaging. These enhanced systems and processed augments the selective nature of previously disclosed probes. Fiber(s) **690-691** are illuminated by a high intensity light source(s) **608** which is typically a tunable laser or UV LED. Source(s) **608** (FIG. **4**) provides illumination for tagged marker(s) **670** in the disclose embodiment where a tunable laser is employed. Excitation/illumination wavelength(s) are specific to the dye/nano-particle used with marker **670** that is very specific for the desired target **671**. The marker/tag is typically a protein specific antigen combined with a florescent marker. The novel probe illumination permits delivery of intense illumination to the target for maximum system sensitivity. Many dyes excited by short (Blue/UV) wavelength light are transmitted poorly in tissue but are easily delivered by fiber **690**. A second application offered for hybrid bi-polar ablation probe **610** is for locating/destroying small cancer lesions. The probe addresses cases where surgery is not practical or it dangerous due to location or sub-operable size. Quantum-dot or dye tagged antibody materials **670** are injected into the patients where it attaches to target structure **671**. Once tagged, cancer node(s) may be located, tested, and treated.

[**0149**] FIG. **7** Side View of Auxiliary Single Tipped Nerve Probe

[**0150**] This probe may be used in conjunction with any of the therapeutic probes **371** and their derivatives. The needle itself will be very fine in nature, such as an acupuncture type needle. By its small size, numerous needle insertions may be accomplished with no scarring and minimal pain. The probe **771** will be inserted in the vicinity of the target tissue through skin **330**. The exposed tip of **771**, **702** will be exposed and electrically connected to generator **732** via wire **734**. The surface of probe **771** is covered with dielectric **704** so the only exposed electrical contact is surface **702** and return electrode **736**. Exposed tip **702** will be advanced to the vicinity of target **101** and test stimulation current will be applied. Appropriate physiological reaction will be observed and when the tip **702** is properly located, depth will be noted via observing marks **765**. External mark **755** may be applied for reference. Ablation probe **371** may then be advanced to the proximity of the target tissue under the X mark **755** and ablation/nerve destruction as described elsewhere may be performed.

[**0151**] FIG. **7**A Side View of Auxiliary Dual-Tipped Nerve Probe.

[**0152**] Dual tipped probe **772** offers an additional embodiment that eliminates return electrode pad **736**. Probe frame/handle **739** holds two fine needles, **702** and **701**, in the disclosed embodiment that are spaced a short distance (a few mm)-mm apart (**730**). The shaft of conductive needle **701** is covered with dielectric insulator **706**, similar to the construction of probe **771** (FIG. **7**). The shaft of the second conductive needle **702** is covered with dielectric insulator sleeve **703**. Electric generator **732** provides current to the probes via conductors **734** and **735**. Current originates from **701** and returns via electrode **702**. Large probe handle **739** is drawn out to teach the dual probes. To aide in probe depth measurement, markers **765** are printed on needle shafts. Dielectric insulating sleeves **703** and **706** isolate the needle shaft current from muscle layer **710**. Current applied via generator **732** stimulates the nerve directly while avoiding

muscle **710**. Smaller probe tips with smaller current permits accurately locating small structures.

[**0153**] Probes **702** and **701** are very small gage needles similar in size to common acupuncture needles, thus permitting repeated probing with minimal discomfort, bleeding, and insertion force. Sharp probes are inserted thru skin **330** and muscle layer(s) **710** near nerve **101**. The practitioner locates target nerve **101**, then the skin surface may be marked **755** as location aide for ablation step as shown in flow chart (FIG. **5**B). Once the desired site of ablation is located, ablation probe(s) **610**(FIG. **6**), **371** and related probes (FIG. **3**), may be inserted under skin **330**, illuminated **448** by tip **305**. They are visible through skin (via illumination **448** from tip **305**) and are guided to mark **755** (FIG. **8**). The observed intensity **765** from illumination source **305** is used as an estimator of measured depth **765**. This simple probe system permits rapid, accurate locating of target structures with minimal pain and injury. Accurate target location permits use of lower ablation energy thereby minimizing damage to nearby structures.

[**0154**] FIG. **8** Side View of Guided Ablation Procedure With Auxiliary Nerve Probe(s).

[**0155**] Auxiliary probes **771** and **772** (FIGS. **7** and **7**A) are used to accurately locate target structure **101**. Probe **771** holds a fine conductive needle **702** that has a shaft covered with dielectric insulator **704**. Electric generator **732** provides a small current to the auxiliary probe via conductor **734** and return conductor **735** via return electrode **736**. The sharp auxiliary probe is inserted thru skin **330** and muscle layer(s) **710** near target nerve **101**. Dielectric insulating sleeve **704** isolates needle shaft from muscle layer **710**. Current is applied via generator **732** thereby stimulating the nerve directly while avoiding muscles **710**. Prior art probes without insulating sleeve **704** stimulate both the nerve and muscle simultaneously, masking nerve **101** and subsequently making nerve location difficult.

[**0156**] Auxiliary probe **771** and **772** provide a method to quickly locate shallow or deep target structures. Shallow structures are typically marked with ink pen allowing illuminated ablation probe **371** or its equivalents to be quickly guided to mark **755**. Optionally, non-illuminated probes may be used by the practitioner who simply feels for the probe tip. For deep structures, probe **771** may also be employed as an electronic beacon; small current **811** (which will be lower intensity and different from the stimulating current) from probe tip **702** is used to guide ablation probe **372**. Amplifier **430** (FIG. **4**) detects current from tip electrode **301** for reading and displays it by controller **401**. Alternately probe **701** is used as a receiver detecting current **811** from electrode **301** Moving probe tip **301** horizontally **1202** and in depth **766** relative to auxiliary probe **702** changes current **810** inversely proportional to distance. Detected signal current **811** isolated and buffered by amplifier **430**, is measured and the current is displayed to simple bar graph **554** for rapid reading. In addition, audio feedback, in which the tone is modulated by proximity of probe tip **351**, **352** or equivalent in relation to auxiliary probe tip **702** is provided to minimize or eliminate the practitioner having to look away from the needle, thus assisting in accurate probe placement. Variable frequency/pitch and volume audio signal are proportional to sensed current **811** that is generated by **452**. The tone signal emitted by speaker **451** (FIGS. **4** and **1**) provides a pleasant and accurate method to aide in probe placement. Simultaneously, illumination source **408** is modulated by amplifier **456** to blink at a rate proportional to the sensed current. This permits the practitioner to quickly and accuracy guide ablation probe **372** into position using a combination of audio and visual guides. The audio and visual aides also reduce the practitioner's training/learning time. The novel real-time probe placement feedback gives the practitioner confidence that the system is working correctly so he/she can concentrate on the delicate procedure. Accurate probe location permits use of minimal energy during ablation, minimizing damage to non-target structures and reducing healing time and patient discomfort.

[**0157**] FIG. **9** A High-Energy Electro-Surgery Sinusoid Cutting Waveform **910**.

[**0158**] Lower energy pulse width modulated (or PWM) sinusoid **920** for coagulation is also well known to electrosurgery art. Variations of cut followed by coagulation are also well known.

[**0159**] FIG. **10** Side View of Visually Guided Ablation Procedure.

[**0160**] Auxiliary probes **771** and **772** (FIGS. **7** and **7**A) have accurately located target structure **101** and subsequently marked target locations **140** to **144**. Shallow structures are marked typically with ink pen (**755**) allowing illuminated ablation probe **371**, **372** or equivalent to be quickly guided to that point. For deep structures, probe **771** is employed as electronic beacon, small current **811** from probe tip **702** is used to guide ablation probe **372** as taught in FIG. **8**.

[**0161**] Ablation probe **372** is inserted thru skin **330** and muscle layer(s) **710** near nerve **101**. Illumination source **408** permits practitioner to quickly and accuracy guide illuminated **448** ablation probe **372** into position. Illumination **448** from ablation probe as seen by practitioner **775** is used as an additional aide in depth estimation. Selectable nerve simulation current **811** aids nerve **101** location within region **1204**. This novel probe placement system gives practitioner confidence system is working correctly so s/he can concentrate on the delicate procedure. Accurate probe location permits use of minimal energy during ablation, minimizing damage to non-target structures and reducing healing time and patient discomfort.

[**0162**] Region **1203** shows the general shape of the ablation region for conical tip **301**. Tip **301** is positioned in close proximity to target nerve **101**. Ablation generally requires one or a series of localized ablations. Number and ablation intensity/energy are set by the particular procedure and the desired permanence.

[**0163**] Five ablation regions are illustrated **140**, **141**, **142**, **143**, and **144**; however, there could be more or less regions. Ablation starts with area **144**, then the probe is moved to **143** and so on to **140**, conversely, ablations could start at **140** and progress to **144**. Also, the practitioner could perform rotating motions, thus further increasing the areas of ablation and permanence of the procedure. Between each ablation procedure **540** (FIG. **5**C), a small nerve stimulation test current **811** is emitted from electrode **301**. The approximate effective range of the nerve stimulation current **811** is shown by **1204**. Testing nerve response after each ablation allows the practitioner to immediately check level of nerve conduction.

Without probe **372** removal, the practitioner receives immediate feedback as to the quality of the ablation. Then minor probe position adjustments are made before conducting additional ablations (if required).

[**0164**] FIG. **11-11**A Controller and Probe Data Base Structure

[**0165**] Controller **101** maintains local probe **1460**, patient **1430**, and procedure **1410** databases. All work together to insure correct probes and settings are used for the desired procedure. Automatically verifying that the attached probe matches selected procedure and verifying probe authentication and usage to avoid patient cross contamination or use of unauthorized probes. Automatic probe inventory control quickly and accurately transfers procedure results to the billing system.

[**0166**] FIG. **11**—Procedure Parameters Code(s) Database **1410**

[**0167**] From a touch screen, the practitioner selects the desired procedure from list **1410**. For example "TEMPORARY NERVE CONDUCTION"**1411**, "SMALL TUMOR 1CC"**1412**, and "SMALL NERVE ABLATE"**1413** are a few of the choices. Each procedure has a unique procedure code **1416** to be used in the billing system. Power range parameter **1417** is a recommended power setting via power level control **404**. The recommended probe(s) Associated with procedure **1415** and power range parameter **1417** are listed in parameters **1419**. With the probe connected, the part number is read from memory **331** (FIGS. **1**, **3** and **4**) and compared to list **1419**. The total power parameter **1418** is the maximum energy that the system may deliver for this procedure and is determined by the procedure code, probe being used and software parameters. These parameters may be modified, updated and changed as required by addition of new probes and procedures allowed/approved. Power is delivered, measured and totaled with integrator **435** (FIG. **4**). The power integration circuit is designed as a hardwired redundant safety circuit that turns off the power amplifier if maximum energy is exceeded. This novel feature protects patients from system fault or practitioner error. Standard procedure time **1420** is doubled and added to current RTC **482** then written to probe memory **331** (in FIG. **1**).

[**0168**] FIG. **11** & **11**A—Probe Usage Authorization Database **1460**

[**0169**] From touch screen **450** (FIGS. **1** and **4**) practitioner selects desired procedure from list **1410**. Probe **371** and equivalents (FIGS. **3**A-D) type is selected from recommended list **1419** and is connected via cable **1334** (FIG. **1**) to control unit **101**. Once connected, controller **401** (FIG. **4**) reads the stored time register from ID memory module **331** (FIG. **1**). If start time **1487** read is zero (factory default), current real time clock **482** (FIG. **4**) is written to database **1460** in the start time field **1467**, **1430** and **1435**. Simultaneously, twice the standard procedure time **1420** parameter is added to RTC **482** and written to time register **1487** via serial bus **403**. If probe start time **1487** reads (**331**) non-zero, the value compared to real time clock **482**. If greater than current time plus twice the standard selected procedure duration **1420**, the controller alerts the practitioner via display **450**, speaker **451** and flashing probe illumination **608** of previously probe used condition. To correct the situation, the practitioner simply connects a new sterile probe and repeats the above process. FIG. **13** teaches additional detail regarding probe verification usage and related database operations. Periodically controller **401** performs the above verification to alert practitioner that he/she has forgotten to change probe(s).

[**0170**] During the procedure (FIG. **10**), various parameters such as peak temperature **1473**, power **1472**, impedance, etc. . . . are read, scaled, stored and displayed. Parameters such as procedure start **1467**; end time **1468**, serial number **1469**, and part number **1468** are recorded as well. Critical parameters are written to local high-speed memory **438** for display and analysis. On a time permitting or end of procedure, data is mirrored to removable USB **1320** memory stick **1338**. Probe specific parameters **1463** are copied and written to probe memory **1338** for use at probe refurbishment facility. Database checksum/CRC(s) **1449**, **1479**, and **1499** are check and updated as required. Faults such as shorts (dielectric **305** (FIG. **3**) breakdown) that are detected are saved to error field **1494** and **1474**. If network connection **1305** is available, email request for replacement probe are automatically sent to repair/customer service center **1308**. Defective probe **374** with saved failure information **1494** is returned for credit and repair.

[**0171**] Use of a USB memory stick permits continued operation in the event of a network **1326** failure Data is loaded to memory **1338** for simple transfer to office computer **1306** (FIG. **1**) for backup. Commonly available USB memory sticks **1320** have large data capacities in the tens to hundreds of megabytes at a low cost with long retention times. USB memory sticks also can support data encryption for secure transfer of patient data. Sealed versions are available as well compatible with chemical sterilization procedures.

[**0172**] If computer network **1326** such as Ethernet 802.11 or wireless 802.11x is available, files are mirrored to local storage **1309**, remote server **1307**. The remote server (typically maintained by equipment manufacture) can be remotely update procedure(s). To insure data integrity and system reliability a high availability database engine made by Birdstep of Americas Birdstep technology, Inc 2101 Fourth Ave. Suite 2000, Seattle Wash. is offered as an example. The Birdstep database supports distributed backups, extensive fault and error recovery while requiring minimal system resources.

[**0173**] FIG. **11**—Patient/Procedure Database **1430**

[**0174**] From a touch screen, the practitioner selects or enters patient name from previous procedure **1430** and creates a new record **1433**. Similarly, a procedure is selected from **1410** (for example "TEMPORARY NERVE CONDUCTION"**1411**, "SMALL TUMOR 1CC"**1412**, and "SMALL NERVE ABLATE"**1413**). Each procedure has a unique procedure code **1416** that is used for the billing system. Other information such as practitioners name **1440**, date **1435** is entered to record **1433**. As taught above probe appropriate for the procedure is connected and verified, part **1470** and serial number **1469** recorded.

[**0175**] FIG. **11**—Voice and Notes

[**0176**] The practitioner enters additional text notes to file **1442** or records them with microphone **455** (FIG. **5**) to wave file **1445** for later playback or transcription. The instant invention permits temporary/permanent nerve conduction

interruption. Thus, procedures are performed at intervals from months to years apart. A hands free integrated voice recorder is extremely useful. Detailed text and voice notes made while probing/ablating are also recording specific settings, and patient response. A feature that is very helpful when reviewing treatment progress and saves valuable time instead of writing notes. Practitioners play back voice/wave files **1445** with standard audio tools a his/or hers desk. Audio files **1445** can be sent via email or file transfer for transcription, updating note field **1442**.

[**0177**] At the end of procedure, records are updated and stored to memory **438**. Backup copies are written to USB **1320** memory stick **1338** (FIG. **1**). If computer network **1326** such as Ethernet 802.11 or wireless 802.11x is available, files are mirrored to local storage **1309**, remote server **1307**. Patient name **1436**, procedure date **1435**, and procedure codes **1416** are automatically transferred via network or USB device **1320** to billing system **1306**. USB memory stick permits continued operation in the event of a network **1326** failure. Data is loaded to USB memory **1338** for simple transfer to office computer **1306** (FIG. **1**) for backup. USB memory sticks **1320** have large data capacities in the tens to hundreds of megabytes at a low cost with long retention times. USB memory stick also support data encryption for secure transfer of patient data. Insuring patient is accurately billed with minimal office paper work. Probe inventory is automatic maintained with replacement probes automatic shipped as needed.

[**0178**] Alternative Probe Configurations

[**0179**] FIG. **12** is a schematic view of an alternative embodiment of a single axis electrosurgical probe **2000** having a longitudinal probe axis **2001**, which is similar to the probe of FIG. **3**. However, probe **2000** of FIG. **12** features substantially equal surface area conductive electrodes **2002** and **2004** located along a longitudinal axis. A probe **371** also having substantially equal surface area electrodes **301** and **302** is shown in FIG. **3**A.

[**0180**] In an equal electrode surface area implementation, one of the conductive electrodes **2002**, **2004** may be selectively connected to a stimulation current source or an ablation current source as described above. The other electrode **2002**, **2004** may be unconnected or connected as a ground or return path for the connected current source. In the embodiment shown in FIG. **12** conductive electrode **2002** is configured to be connected to the ablation source making electrode **2002** the active electrode. Thus electrode **2004** is in this embodiment a return electrode. Either electrode **2002**, **2004** may be connected to a current source or return with appropriate switches.

[**0181**] Since electrodes **2002** and **2004** have substantially equal surface area, the local heating formed upon the application of RF ablation energy to the active electrode **2002** results in a heating zone having a substantially symmetrical ellipsoid form.

[**0182**] The single axis electrosurgical probe **2000** of FIG. **12** also features a dielectric insulator **2006** positioned along the probe axis between the conductive electrodes **2002** and **2004**. The dielectric insulator **2006** may have any suitable length, and probes with alternative length insulators may be manufactured for specific ablation procedures. Varying the length of the dielectric insulator **2006** varies the gap dimension **2008** between the electrodes **2002** and **2004**. Varying the gap dimension **2008** provides for optimization of the current density within the ablation zone, varies the length of the ablation zone and permits the use of higher voltages, if desired. Thus, the gap dimension may be selected in conjunction with other parameters such as electrode surface area and ablation current to achieve select ablation volumes and tissue temperatures for specific applications.

[**0183**] The probe **2000** of FIG. **12** also features a blunt tip **2010** rather than the conical tip **351**, chiseled tip **352** or other tips of FIG. **3**. The blunt tip **2010** of FIG. **12** has a smooth rounded profile and is advantageous in certain instances to allow the probe to be easily advanced and maneuvered under the skin minimizing the risk of puncture or the cutting of adjacent tissue or anatomical structures. Thus, a blunt tip **2010** may significantly reduce the bruising or other trauma associated with a procedure.

[**0184**] The probe **2000** of FIG. **12** may include a sensor **2012**. The sensor may be a temperature sensor **2012**. A temperature sensor provides for active temperature monitoring within the ablation zone. Alternatively, a single axis electrosurgical probe of any configuration may be implemented with a Kalman filter as taught by Conolly U.S. Pat. No. 6,384,384 which patent is incorporated herein by reference in its entirety. Kalman filters are also used to estimate tissue temperature within an ablation volume. Kalman filters are suitable for use where well-defined tissue state changes occur at specific temperatures due to protein denaturation such as the denaturation of collagen at 65 C. Kalman filter temperature monitoring is advantageous because the bulk and cost of a separate temperature sensor can be avoided.

[**0185**] FIG. **13** is a schematic view of an asymmetrical single axis probe **2014** also defining a longitudinal probe axis **2015**. The probe **2014** features a first conductive electrode **2016** and a second conductive electrode **2018** having different surface areas. In the embodiment shown in FIG. **13**, the first electrode **2016** is an active electrode and the second electrode **2018** having a larger surface area is a return electrode. A probe having any surface area ratio between an active and return electrode may be fabricated and used to achieve specific ablation results. In addition, the relative positions of the active electrode **2016** and the return electrode **2018** with respect to the tip of a given probe may be switched. In one embodiment the ratio of the active electrode **2016** to the surface area of the return electrode **2018** is **1**:**3**. Other ratios including **1**:**8** may be implemented to achieve specific results. The surface area ratio may further be adjustable using a sleeve or other mechanism which will shield or cover a portion of on or both electrodes thus increasing or decreasing the length of the gap defining dielectric insulator **2019**. Generally, asymmetrical electrode surface areas will result in asymmetrical heating and ablation because of the higher current density of the RF ablation energy at the electrode with smaller surface area. For example, upon the application of RF energy to the active electrode of the FIG. **13** embodiment, a tissue volume proximal the active electrode **2016** may be asymmetrically heated due to the greater current density resulting from the relatively small surface area of the active electrode **2016**. Asymmetrical tissue heating coupled with precise RF power integration taught herein and various probe geometries permits the formation of selected repeatable and controlled ablation volumes.

[0186] FIG. **14** schematically illustrates an alternative asymmetrical probe **2020**, which is similar in many respects to the asymmetrical probe **2014** of FIG. **13**. The asymmetrical probe **2020** of FIG. **14**, however, features an active electrode **2022** having a surface area greater than that of the return electrode **2024**. In the FIG. **14** embodiment current density is higher at the relatively smaller surface area electrode **2024**, thus ablation energy is concentrated in the dielectric insulator gap **2025** between the electrodes **2022** and **2024** nearer return electrode **2024** and away from the tip of the probe.

[0187] FIG. **15** is a schematic view of one embodiment of a multiple electrode probe **2026**. The multiple electrode probe **2026** includes a substantially needle-shaped probe body **2028** which defines a longitudinal probe axis **2029**. More than two electrodes are associated with the probe body and positioned at various locations along the probe axis. In the FIG. **15** embodiment the electrodes include an active electrode **2030**, a return electrode **2032**, and a stimulation electrode **2034**. In this embodiment the active electrode is positioned near the tip of the multiple electrode probe **2026**, the return electrode **2032** is positioned away from the tip and the stimulation electrode **2034** is positioned between the active electrode **2030** and the return electrode **2032**. It should be noted that the position of the various electrodes with respect to each other and the tip may be varied to achieve specific ablation and probe positioning advantages. In addition, the connection of any given physical electrode as an active electrode, return or stimulation electrode may be varied at the discretion of the user with a simple switching mechanism between the electrode and the ablation or stimulation energy sources. Alternatively, a separate ground or return path **2035** may be utilized with any configuration of electrodes. The various electrodes of the multiple electrode probe **2026** are separated by a first dielectric insulator **2036** and a second dielectric insulator **2038**. FIG. **16** schematically illustrates the multi-polar probe **2026** of FIG. **15** with the addition of a curved section **2040** opposite the portion of the probe body **2028** associated with the electrodes. The curved section **2040** may in certain instances allow the practitioner to achieve optimal probe positioning with a minimum of unnecessary tissue disruption. A multiple electrode probe **2026** may be implemented with dielectric insulators **2036**, **2038** of varying dimensions, sensors or electrodes of different surface areas, all as described above, to achieve desired ablation results.

[0188] FIG. **17-19** schematically illustrates an alternative embodiment of a multiple electrode probe **2042**. The multiple electrode probe **2042** of FIG. **17-19** includes a probe body **2044** which defines a longitudinal probe axis **2045**. Multiple electrodes **2046-2062** are associated with the probe body **2044** at separate locations along the probe axis. In the embodiment shown in FIG. **17-19** the electrodes are uniformly sized and spaced. It is important to note, however, that different sizes of electrodes and non-uniform spacing of the electrodes may be implemented to achieve specific ablation results. Preferably, each of the electrodes **2046-2062** may be selectively connected with one or more switches to a stimulation current source, an ablation current source, a ground for the stimulation current source a ground for an ablation energy source or left unconnected. As described in detail below, the flexibility provided by switched connection of each electrode to a current source or ground provides certain advantages in probe location and ablation. In addition, the multiple electrode probe **2042** could be deployed in conjunction with a separate return electrode **2064**, typically placed in contact with tissue away from the ablation site.

Placement Methods

[0189] Several methods of properly positioning a probe adjacent to a selected nerve for ablation energy application are discussed above. For example, probe placement methods featuring florescence marker dyes, optical probe guidance and electronic probe guidance with the use of low energy nerve stimulation current are discussed in detail. Certain of the alternative probe configurations as illustrated in FIGS. **13-19** provide for refined probe placement methods using variations of the basic electrical stimulation techniques described above.

[0190] The single axis electrosurgical probe **2000** of FIG. **12** or the asymmetric probes **2014**, **2020** of FIG. **13** and **14** may each be properly positioned using an iterative technique, as described above with reference to FIGS. **5**A-C. The iterative placement method may be refined for uses with multiple electrode probes such as are depicted in FIGS. **15-19**.

[0191] For example, the FIG. **15** embodiment of a multiple electrode probe **2026** includes a separate stimulation electrode **2034**. The stimulation electrode **2034** is located along the longitudinal axis **2029** of the probe body, typically though not necessarily between an active electrode **2030** and a return electrode **2032**. During the stimulation and positioning phases of a probe placement procedure the active electrode **2030**, return electrode **2032** or a separate electrode **2035** not associated with the probe body **2028** may serve as the ground for the stimulation current source. As is described above with respect to FIG. **5** a practitioner will typically monitor target nerve response by observing muscle reaction elicited by the stimulation current as the multiple electrode probe **2026** is iteratively guided closer to the target nerve **101**. The level of stimulation currently applied may be adjusted to increase or decrease the effective stimulation range depending upon the muscle response observed by the practitioner. Typically, stimulation current will be continuously or stepwise reduced with a switch or other control to decrease the stimulation range as the stimulation electrode **2034** is guided in close proximity to the subject nerve **101**, assuring that the nerve is ultimately placed adjacent to the stimulation electrode.

[0192] In probe embodiments where the stimulation electrode is positioned in between the ablation electrodes **2030**, **2032**, the above described iterative method guarantees that the target nerve is positioned within an elliptical ablation zone **2064** (see FIG. **16**) which will be formed between the active electrode **2030** and return electrode **2032** upon the application of RF ablation energy.

[0193] FIG. **17-19** shows an alternative embodiment of a multiple electrode probe **2042** placed in various orientations with respect to a target nerve **2066**. For example in FIG. **17**, the multiple electrode probe **2042** is placed transverse the nerve **2066**, in FIG. **18** the multiple electrode probe **2042** is placed parallel to a portion of the nerve **2066** and FIG. **19** shows the multiple electrode probe **2042** placed across the target nerve **2066** at an angle. As is described in detail above, each of the electrodes **2046-2065** may preferably be selec-

tively connected to a stimulation current source, an ablation energy source, a ground or left unconnected. The electrodes **2046-2062** may be connected manually or switched and activated electronically.

[**0194**] The multiple electrodes of the FIG. **17-19** embodiment of the multiple electrode probe **2042** provides for certain advanced placement and ablation procedures. For example, FIG. **17** illustrates a method for locating and selectively ablating a target nerve **2066**, which runs substantially transverse the probe at a point along the axial length of the probe **2042**. This placement method features the practitioner initially positioning the probe across the target nerve **2066**. The electrodes **2046** through **2062** are then activated sequentially with stimulating current, in adjacent active/ground pairs (bipolar mode) or individually with reliance upon an external ground **2064** (mono-polar mode). The practitioner may then observe the response of one or more muscles associated with the target nerve as stimulation current is applied to successive electrodes **2046-2062**.

[**0195**] For example, with reference to FIG. **17**, stimulation current may be applied between electrodes **2046** and **2048**. The practitioner notes that there is no corresponding muscle response. Stimulation current may next be applied between electrodes **2048** and **2050**. Again, no muscle response is observed by the practitioner. Sequentially, stimulation current is then applied to successive electrode pairs. When the stimulation current is applied between electrodes **2054** and **2056** there may be a mild muscle response. When the stimulation current is applied between electrodes **2056** and **2058** however, a strong muscle response will be observed. Continuing on, the stimulation is then applied between electrodes **2058** and **2060**. Here a greatly reduced muscle response is observed indicating that the nerve is crossing the probe substantially between electrodes **2056** and **2058**. Subsequently, ablation energy may be applied between designated electrodes **2056** and **2058** to ablate nerve **2066**.

[**0196**] FIG. **18** illustrates a similar nerve location and ablation procedure wherein the nerve **2066** is substantially parallel to and adjacent to the axial length of the probe **2042** adjacent electrodes **2048** through **2056**. In this second example the practitioner first applies stimulation current is applied between electrodes **2046** and **2048**. A mild muscle response or no muscle response may be observed. When stimulation current is applied between electrodes **2048** and **2050**, a strong muscle response is noted by the practitioner.

[**0197**] Sequentially, the stimulation current is then applied between electrodes **2050** and **2052** with similar strong muscle response observed. This sequential stimulation and response process is observed through the activation of electrodes **2056** and **2058** where the muscle response is substantially diminished or not observable. This is an indication that electrodes **2048** through **2056** are all in contact with the nerve **2042**. The electrodes **2048** through **2056** may then be switched to the ablation current source activated and sequentially or simultaneously in bi-polar pairs or individually in bi-polar or mono-polar mode to ablate the nerve **2042**. The nerve could be ablated along a select length defined by the number of electrodes activated by the practitioner. This method could also be implemented in mono-polar mode whereby stimulation or ablation energy is applied between one or more electrodes **2046** through **2062** and a separate return electrode applied externally on the body.

[**0198**] FIG. **19** illustrates a substantially similar nerve location and ablation procedure wherein the multiple electrode probe **2042** crosses the nerve **2066** diagonally or at an oblique angle to the probe axis. Thus, FIG. **19** illustrates a method for angular positioning of the probe **2042** relative to the nerve **2066**. In this example stimulation current applied as described above at electrodes **2052**, **2054**, and perhaps **2056** would result in a response in the associated muscle. If a larger number of electrodes elicit a muscle response, this is an indication of a broader nerve/probe contact area resulting from a more parallel contact placement of the probe **2042** relative to the nerve **2066**. Such a determination of angular placement can be enhanced by fabricating a probe with relatively short distance between adjacent electrodes, relative to the diameter of a nerve of interest. The practitioner may also maneuver the probe to attain a muscle response from more or less electrodes as desired providing the opportunity to ablate a greater or lesser length of the never without axially repositioning the probe.

[**0199**] The above methods of angular probe positioning and sequential stimulation may be combined with the iterative techniques also described above. For example, the stimulation current generator may be set at a relatively high level initially and reduced when the general location of the nerve with respect to certain electrodes is determined.

[**0200**] For example, the stimulation current threshold (to elicit an observable response) between electrodes **2048** and **2050** of FIG. **19** would be higher than the threshold between electrodes **2050** and **2053**. This information could be indicated graphically, numerically or audibly to allow the practitioner to reposition the probe for more parallel or more transverse positioning of probe **2042** relative to nerve **2066**.

[**0201**] While the invention has been particularly shown and described with reference to a number of embodiments, it would be understood by those skilled in the art that changes in the form and details may be made to the various embodiments disclosed herein without departing from the spirit and scope of the invention and that the various embodiments disclosed herein are not intended to act as limitations on the scope of the claims.

What is claimed is:

1. An electrosurgical probe comprising:

a probe body defining a longitudinal probe axis; and

a first and a second conductive electrode operatively disposed along the probe axis wherein the surface area of the first conductive electrode is substantially greater than the surface area of the second conductive electrode.

2. The electrosurgical probe of claim 1 wherein a ratio of the surface area of the first conductive electrode to the surface area of the second conductive electrode is equal to or greater than 3:1.

3. The electrosurgical probe of claim 1 wherein a ratio of the surface area of the first conductive electrode to the surface area of the second conductive electrode is equal to or greater than 8:1.

4. The electrosurgical probe of claim 1, wherein a ratio of the surface area of the first conductive electrode to the surface area of the second conductive electrode is adjustable.

5. The electrosurgical probe of claim 1 further comprising a stimulation energy source in electrical communication with at least one of the first or second conductive electrodes.

6. The electrosurgical probe of claim 5 further comprising an ablation energy source in electrical communication with at least one of the first or second conductive electrodes.

7. The electrosurgical probe of claim 6 further comprising a switch providing for the selective connection of the stimulation energy source or the ablation energy source to at least one of the conductive electrodes.

8. An electrosurgical probe comprising:

a probe body defining a longitudinal probe axis;

an active electrode operatively associated with the probe body at a first location along the probe axis;

a stimulation electrode operatively associated with the probe body at a second location along the probe axis; and

a return electrode operatively associated with the probe body at a third location along the probe axis.

9. The electrosurgical probe of claim 8 wherein the stimulation electrode is positioned along the probe axis between the active electrode and the return electrode.

10. The electrosurgical probe of claim 8 further comprising a stimulation energy source in electrical communication with the stimulation electrode.

11. The electrosurgical probe of claim 10 wherein the stimulation energy source provides variable stimulation current.

12. The electrosurgical probe of claim 10 wherein at least one of the active electrode and the return electrode is in electrical communication with a ground for the stimulation energy source.

13. The electrosurgical probe of claim 10 wherein both of the active electrode and the return electrode are in electrical communication with a ground for the stimulation energy source.

14. The electrosurgical probe of claim 7 further comprising an ablation energy source in electrical communication with the active electrode.

15. The electrosurgical probe of claim 13 wherein the ablation energy source provides variable ablation energy.

16. The electrosurgical probe of claim 15 wherein the ablation energy source provides energy which has at least one of variable voltage, current and waveform.

17. An electrosurgical probe comprising:

a probe body defining a longitudinal probe axis;

at least three electrodes operatively associated with the probe body at separate locations along the probe axis; and

a stimulation energy source in electrical communication with at least one of the electrodes.

18. The electrosurgical probe of claim 17 wherein the stimulation energy source provides variable stimulation energy.

19. The electrosurgical probe of claim 17 wherein the stimulation energy source may be selectively connected to at least one or more of the electrodes.

20. The electrosurgical probe of claim 17 further comprising a stimulation energy ground in electrical communication with the stimulation energy source, wherein the stimulation energy ground may be selectively connected to at least one or more of the electrodes.

21. The electrosurgical probe of claim 17 further comprising an ablation energy source in electrical communication with at least one of the electrodes.

22. The electrosurgical probe of claim 21 wherein the ablation energy source provides variable ablation energy.

23. The electrosurgical probe of claim 22 wherein the ablation energy source provides energy which has at least one of variable voltage, current and waveform.

24. The electrosurgical probe of claim 21 wherein the ablation current source may be selectively connected to at least one or more of the electrodes.

25. The electrosurgical probe of claim 21 further comprising an ablation energy ground for the ablation energy source, wherein the ablation energy ground may be selectively connected to one or more of the electrodes.

26. A method of positioning an electrosurgical probe comprising:

providing an electrosurgical probe having a probe body defining a longitudinal probe axis, multiple conductive electrodes operatively disposed along the probe axis, and a stimulation energy source in electrical communication with at least one of the conductive electrodes;

inserting the electrosurgical probe to a first position within tissue containing a target nerve;

applying first stimulation energy to the stimulation electrode;

observing a first response of a muscle associated with the target nerve;

moving the electrosurgical probe to a second position within the tissue containing the target nerve;

applying second stimulation energy to the stimulation electrode; observing a second response of a muscle associated with the target nerve; and

comparing the second response of the muscle associated with the target nerve to the first response of the muscle associated with the target nerve.

27. The method of claim 26 further comprising:

providing a variable stimulation energy source; and

varying the stimulation energy between the first and the second applications of stimulation energy.

28. A method of positioning an electrosurgical probe comprising:

providing an electrosurgical probe having a probe body defining a longitudinal probe axis, multiple conductive electrodes operatively disposed along the probe axis, and a stimulation energy source which may be connected sequentially to more than one of the conductive electrodes;

inserting the electrosurgical probe into tissue containing a target nerve;

applying stimulation current to a select first electrode;

observing a first response of a muscle associated with the target nerve; applying stimulation energy to a select second electrode;

observing a second response of the muscle associated with the target nerve; and

comparing the second response of the muscle associated with the target nerve to the first response of the muscle associated with the target nerve.

29. The method of claim 28 further comprising:

applying stimulation energy to a select third electrode; observing a third response of the muscle associated with the target nerve; and

comparing the third response of the muscle associated with the target nerve to the second response of the muscle associated with the target nerve.

30. The method of claim 29 further comprising sequentially applying stimulation energy to the first, second and third electrodes.

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