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(54) METHODS AND THERAPEUTICS COMPRISING LIGAND-TARGETED ELPS

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(57) **ABSTRACT**

Disclosed herein are novel methods and compositions for targeting drug delivery systems to specific cells. One aspect relates to a drug delivery system comprising an elastin-like peptide (ELP) component and a ligand selected from the group consisting of mIgA and knob capable of either drug encapsulation or drug attachment. Further aspects relate to drug delivery systems comprising an elastin-like peptide (ELP) component and a ligand; wherein the ligand specifically binds to a receptor selected from the group consisting of CAR and pIgR. Further aspects include the novel transcytosing properties of the elastin-like peptide and the ligand, knob. Also provided are methods and pharmaceutical compositions comprising the disclosed therapeutics.

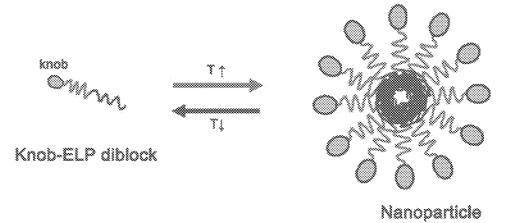
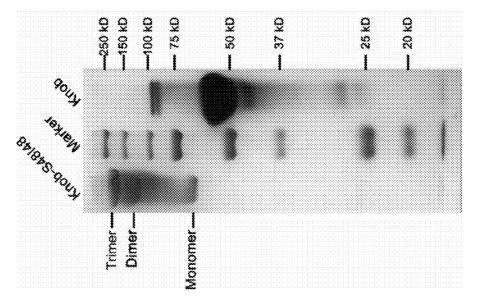
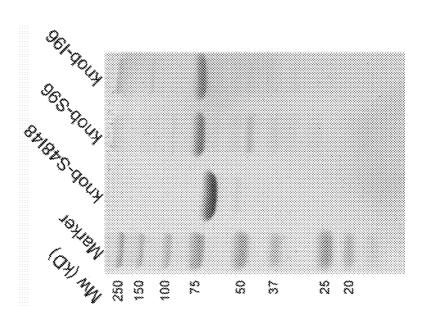


Fig. 1







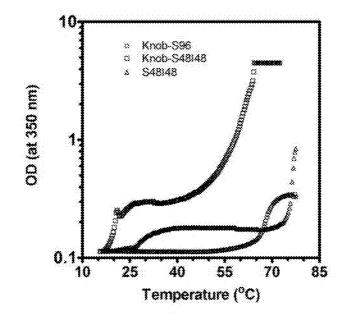


Fig. 4

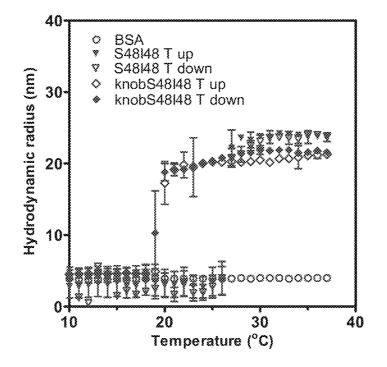


Fig. 5A

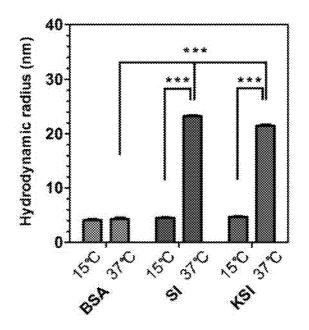
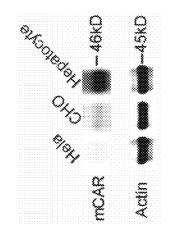


Fig. 5B



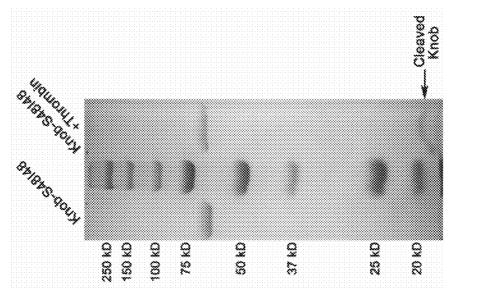


Fig. 7

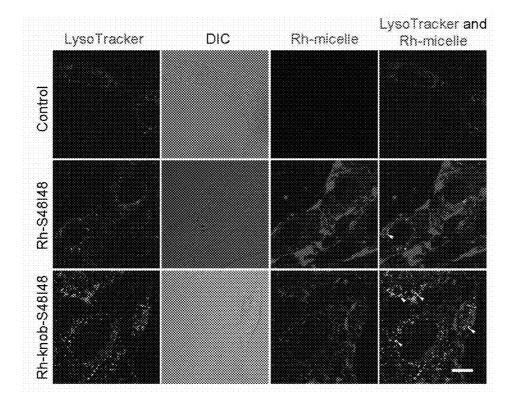


Fig. 8

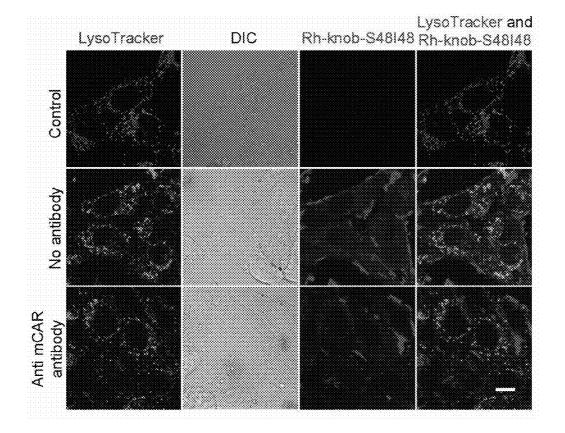


Fig. 9

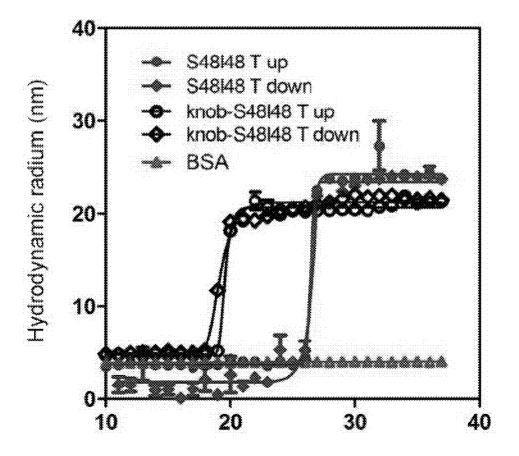
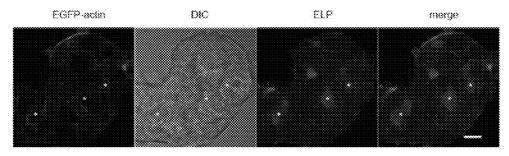
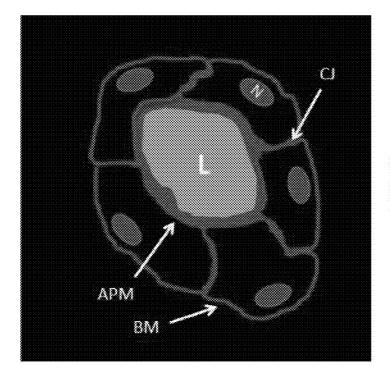


Fig. 10



*lumena. Scale bar: 10 µm

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L: acinar lumena N: nucleus APM: apical membrane BM: basal-lateral membrane CJ: cell junction

Fig. 12

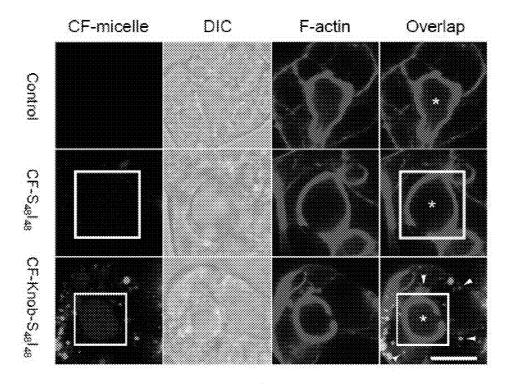
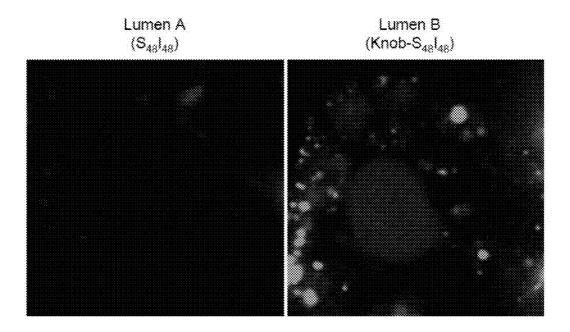


Fig. 13





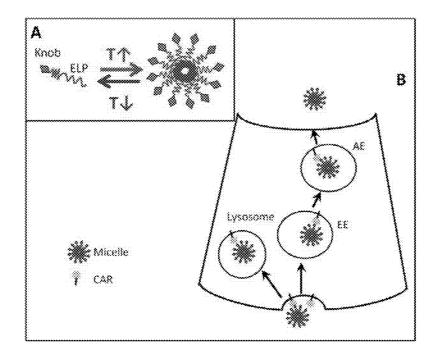


Fig. 15

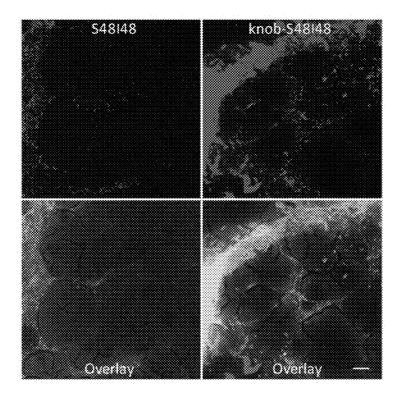
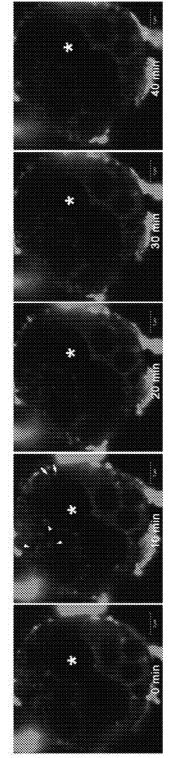


Fig. 16



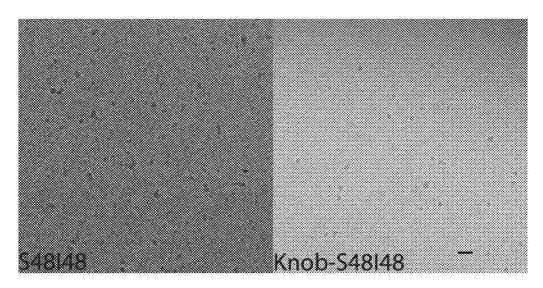


Fig. 18A

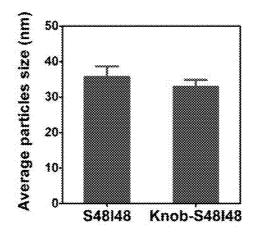


Fig. 18B

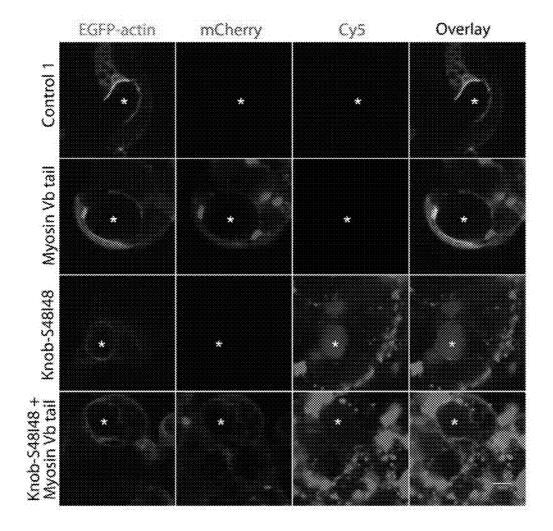


Fig. 19

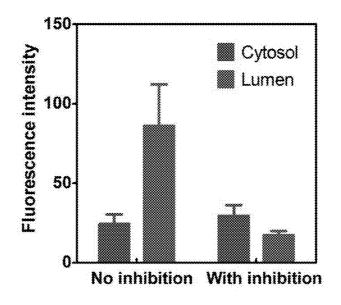


Fig. 20A

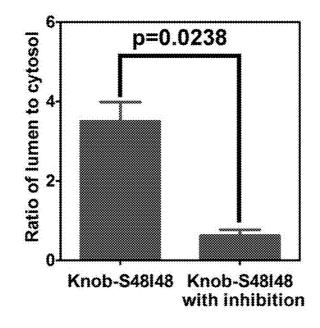


Fig. 20B

METHODS AND THERAPEUTICS COMPRISING LIGAND-TARGETED ELPS

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This application claims the benefit under 35 U.S.C. §119(e) to U.S. Provisional Application Ser. No. 61/598,298, filed Feb. 13, 2012, and U.S. Provisional Application Ser. No. 61/664,619, filed Jun. 26, 2012, each of which are hereby incorporated by reference in their entirety.

STATEMENT OF GOVERNMENT SUPPORT

[0002] The presently disclosed subject matter was made with United States Government support under Grant Nos. EY017293-S1, EY017293 and 5-P30-CA14089, awarded by the National Institutes of Health (NIH). The United States Government has certain rights in the presently disclosed subject matter.

BACKGROUND

[0003] Drug delivery to the eye (e.g. to retina, choroid, vitreous and optic nerve) is important for treating several disorders such as age-related macular degeneration, diabetic retinopathy, retinal venous occlusions, retinal arterial occlusion, macular edema, postoperative inflammation, infection, dryness, uveitis retinitis, proliferative vitreoretinopathy and glaucoma. Due to anatomic membrane barriers (i.e. cornea, conjunctiva and sclera) and the lacrimal drainage it can be quite challenging to target drugs and achieve therapeutic drug concentrations in the anterior parts of the eye after topical drug administration. Reaching the posterior part of the eye is an even more challenging task because of the anatomical and physiological barriers segregating this part of the eye from the anterior segment. Since those barriers cannot be altered with non-invasive methods, there is a need in the art for improved methods and pharmaceutical compositions that increase ocular bioavailability.

[0004] There is a need in the art for improved noninvasive, safe and patient-friendly drug delivery systems that are specific and effective for targeted delivery to the eye. In general, drugs can enter the eye via three distinctive routes, i.e. a) through conjunctiva/sclera after topical application, b) from the anterior part after topical application, and c) from the systemic circulation after topical application, parenteral, oral, and intranasal or other administration routes that deliver drugs to the blood circulation. Then drugs can be delivered to the eye via invasive methods such as direct drug injection into the vitreous humor or subconjunctival injections. Invasive methods can cause discomfort for the patient and can also lead to complications that are even more serious than the disease being treated. In most cases, topical or systemic administration is used to treat posterior diseases despite limited bioavailability from these formulations. There is also a need for sustained retention of drugs administered by topical administration onto the ocular surface since many diseases including inflammatory or infectious diseases require a greater drug concentration than can be achieved by infrequent topical administration due to issues with rapid clearance.

[0005] In the past few decades, research has focused on drug loaded nanoparticles, such as liposomes, micelles, dendrimers and polymersomes. Relatively few drug carriers have been approved for use in humans, which suggests that better strategies and materials may be required to generate successful nanomedicines. Traditional drug delivery systems have a number of deficiencies including a lack of targeted delivery, high toxicity, low cellular uptake, and poor biocompatibility. Therefore, there is a need in the art for improved drug delivery systems targeted to parts of the eye.

SUMMARY

[0006] Disclosed herein are novel methods and compositions for targeting therapeutics to specific cells. One aspect relates to a therapeutic agent comprising an elastin-like peptide (ELP) component and a ligand selected from the group consisting of mIgA and knob. Previous reports indicated that the fiber knob of adenovirus serotype 5 (Ad5) exhibits a high efficiency of internalization in liver after intravenous injection in mice (J. Virol. 78:6431-6438 (2004)). Both hepatocytes and lacrimal gland acinar cells (LGACs), also very efficiently transduced with Ad5 in a unique fiber-dependent pathway, display a very high level of coxsackie-adenovirus receptor (CAR) expression. Although CAR remains surfaceassociated in most cells, Applicants' research shows internalization of Ad5 in these cells is through a CAR-mediated and fiber-dependent endocytic pathway (J. Virol. 80:11833-11861 (2006)).

[0007] To develop new treatments for diseases of the lacrimal gland, new drug vehicles are required that are biocompatible, biodegradable and easily modified with bioactive peptides. An emerging approach to this challenge employs genetically engineered polypeptides to drive the assembly of nanostructures. Elastin-like-polypeptides possess unique phase transition behavior, that mediates self-assembly of nanoparticles.

[0008] A second aspect relates to a therapeutic agent comprising an elastin-like peptide (ELP) component and a ligand; wherein the ligand specifically binds to a receptor selected from the group consisting of CAR (GenBank acc.no. AF 200465.1) and pIgR (NCBI Reference Sequence NM_002644.3).

[0009] A further aspects relates to a method for delivering a therapeutic agent comprising an elastin-like peptide (ELP) to a cell, said method comprising: administering an (ELP) component and a ligand component to the cell; wherein the ligand component specifically binds to a receptor selected from the group consisting of CAR and pIgR.

[0010] Still further, there is provided a method for delivering a therapeutic agent comprising an elastin-like peptide (ELP) to a cell, said method comprising: administering an (ELP) component and a ligand component to the cell; wherein the ligand component is selected from the group consisting of mIgA and knob.

[0011] In another aspect, a method for delivering a drug to the luminal area of the lacrimal gland by transcytosis is provided, the method comprising, consisting essentially, or yet further consisting of, contacting the lacrimal gland with one or more of a drug delivery agent, a polynucleotide, or a composition, as described herein, wherein the ligand component specifically binds to a CAR and/or pIgR receptor; and/or wherein the ligand component is mIgA and/or knob. The contacting can be in vitro or in vivo. In one embodiment, the drug is in contact with the ocular surface of the eye. Transcytosis allows the durg to have access to the ocular surface of the surface of the eye for a variety of conditions like dry eye, scleritis, and the like.

[0012] In yet another aspect, provided is a method for treating a disease of the lacrimal gland, comprising, or alternatively consisting essentially of, or yet further consisting of, administering to a patient in need of such treatment one or more of a drug delivery agent, a polynucleotide, or a compositions, wherein the ligand component specifically binds to a CAR and/or pIgR receptor; and/or wherein the ligand component is mIgA and/or knob, thereby treating the patient. In one aspect, the disease is cancer.

[0013] In certain embodiments, the cell is any cell that expresses a CAR or pIGR receptor. Non-limiting examples include liver, heart, lacrimal gland, salivary gland, lung, brain, pancreatic acinar tissue, prostate or mucosal cells. In a related embodiment, the cell is the lacrimal acinar cell of the lacrimal gland (LGAC). CAR is detected in liver and lacrimal gland as well as in human umbilical vein endothelial cells and pancreatic acinar tissue (acinar cells and islets), as well as in prostate. Most mucosal epithelial cells display pIgR including the cells lining the gut, pulmonary epithelial cells, acinar cells (salivary, lacrimal gland) and other barrier epithelial tissues responsible for maintaining mucosal immunity. Accordingly, in one embodiment, the drug is released from interstitial to luminal surfaces on a mucosal epithelial cell.

BRIEF DESCRIPTION OF THE FIGURES

[0014] FIG. **1** is a schematic representation of knob-ELP fusion peptides. Full-length knob was expressed at the N-terminus of diblock ELPs. A thrombin cleavage site was engineered between the knob domain and the diblock ELP. The designed diblock knob-ELP can assemble into a nanoparticle, mediated by the first ELP phase transition of the diblock ELP. Above the first transition temperature, knob-ELP will reversibly self-assemble into a nanoparticle.

[0015] FIG. **2** shows denaturing SDS-PAGE for knob-ELPs. The knob-I96, knob-S96 and knob-S48I48 were purified by inverse phase transition cycling (ITC) and resolved by SDS-PAGE stained with Coomassie brilliant blue. The molecular weights of marker proteins lane are 250, 150, 100, 75, 50, 37, 25 and 20 kD, as listed.

[0016] FIG. **3** shows non-denatured-PAGE of knob-S48I48. The knob-S48I48 was mixed with non-denaturing sample buffer (without 2-mercapto-ethanol) and resolved by PAGE. The gel was then stained with Coomassie brilliant blue. The molecular weights of the marker lanes are 250, 150, 100, 75, 50, 37, 25 and 20 kD (from top to bottom), respectively.

[0017] FIG. 4 shows temperature-dependence of the optical density for ELP fusion peptides. Phase transition behavior of knob-S96, S48I48 and knob-S48I48. Each sample was diluted to $25 \,\mu$ M in PBS at 4° C. The OD of samples at 350 nm was measured using a spectrophotometer with increasing temperatures from 15 to 80° C.

[0018] FIG. **5**A-B shows the temperature-dependent assembly and disassembly for ELP fusion peptides. Dynamic light scattering was used to characterize S48I48 and knob-S48I48. (A) S48I48 and knob-S48I48 were diluted at $25 \,\mu$ M in PBS and passed through a 20 nm filter at 4° C. before measurement in a DynaPro plate reader. Readings were taken starting with an increase from 10° C. to 37° C. and then a decrease from 37° C. to 10° C. BSA was only measured from 10° C. to 37° C. (B) Statistical comparison for nanoparticles radius for BSA, S48I48 and knob-S48I48 at 15° C. and 37° C. *** indicates p<0.01 as determined using the Tukey post-hoc test.

[0019] FIG. **6** shows proteolytic release of knob from knob-ELP. Left lane is knob-S48148 before cleavage and right lane is knob-S48148 after incubation with thrombin overnight at room temperature. The gel was stained by Coomassie brilliant blue. The position of the cleaved knob domain near 20 kD is shown in the right lane.

[0020] FIG. **7** shows murine hepatocytes expresses coxsackie adenovirus receptor (CAR). Hepatocytes, CHO, and Hela cells were lysed with SDS-PAGE sample buffer and CAR expression detected with western blot via primary goat anti mouse CAR and mouse anti-actin antibodies, as well as secondary IRDye®800 donkey anti-goat and IRDye® 700 goat anti-mouse antibodies.

[0021] FIG. **8** demonstrates live cell imaging of cellular uptake for ELP and knob-ELP nanoparticles. Transformed mouse hepatocytes grown on 35 mm glass-bottomed dishes were incubated in medium containing 10 μ M rhodamine-conjugated S48I48 or knob-S48I48 (red) with 75 nM LysoTracker green (green) at 37° C. for 30 minutes and imaged using confocal microscopy. Knob-S48I48 exhibited markedly more co-localization with LysoTracker green while S48I48 exhibited more apparent surface association. The arrows indicated the internalized nanoparticles co-localized with lysosome. Scale bar: 10 μ m.

[0022] FIG. **9** shows competitive binding and uptake of knob-S48I48 with anti-mouse CAR antibody. Live cell imaging was performed on transformed mouse hepatocytes grown on 35 mm glass-bottomed dishes were pre-incubated with 20 μ g/mL anti-mouse CAR antibody at 37° C. for 30 minutes. Rhodamine-conjugated knob-S48I48 (red, 10 μ M) with LysoTracker green (green) was added into the medium. After 30 minutes the cells were rinsed with fresh warm medium and imaged using confocal microscopy. Scale bar: 10 μ m.

[0023] FIG. **10** shows self-assembly or disassembly of nanoparticles above or below their phase transition temperatures. S48I48 and Knob-S48I48 were passed through a 20 nm microfilter at 4° C. in PBS and characterized by dynamic light scattering spectroscopy (DynaPro plate reader). Readings were taken starting with an increase from 10° C. to 37° C. and then decrease from 37° C. to 10° C. BSA was only measured from 10° C. to 37° C.

[0024] FIG. 11 shows knob-ELP nanoparticles transcytosed in LGACs. Scale bar represents $10 \,\mu$ M.

[0025] FIG. **12** shows a schematic representation of reconstituted LG acinar cluster. L represents acinar lumena. N represents cell nucleus. APM represents apical membrane. BM represents basal-lateral membrane. CJ represents cell junction.

[0026] FIG. **13** shows intracellular uptake of carboxyfluorescein (CF)-conjugated ELPs in lacrimal gland acinar cells. Unlike CF-S48I48, CF-Knob-S48I48 exhibits strong internalization which was shown in green in reconstituted LGACs. Also endocytosed CF-Knob-S48I48 was transcytosed into reconstituted acinar lumen which was stained by expressed Lifeact-RFP proteins (red).

[0027] FIG. 14 shows lumen A (S48I48, left panel) and lumen B (Knob-S48I48, right panel). Arrowheads indicate internalized nanoparticels (Knob-S48I48). The symbol "*" indicates lumen. Box indicates luminal area of LGACs. Scale bar represents 10 μ m.

[0028] FIG. **15**A-B is a schematic representation showing knob-S48I48 nanoparticles targeted to CAR in LGACs.

[0029] FIG. **16** shows the in vivo retention of knob-S48I48 in the LG of BALB/c mice.

[0030] FIG. **17** shows the basal-to-apical transport of Cy5-Knob-S48I48 in primary cultures of Lacrimal Gland Acinar Cells (LGACs).

[0031] FIG. **18**A-B shows the spherical morphology of S48I48 protein polymer nanoparticles with and without the Knob domain. FIG. **18**A shows the Cryo-transmission electron microscopy (TEM) imaging of S48I48 and Knob-S48I48 (Scale bar: 100 nm) and FIG. **18**B shows the average particles sizes measured by Image J.

[0032] FIG. **19** shows the overexpression of Myosin Vb tail suppresses accumulation of knob-S48I48 nanopraticles at the acinar lumen. mCherry myosin Vb tail (red), an inhibitor of LGAC transcytosis from basolateral to apical membranes, significantly reduces the transcytosis of knob-S48I48 (purple). Green label associated with expression of EGFP-actin denotes the organization of the actin cytoskeleton while *, lumenal area of LGACs, surrounded by apical plasma membrane.

[0033] FIG. 20A-B shows the quantitative suppression of transcytosis of knob-S48I48 nanoparticles by myosin Vb overexpression. FIG. 20A shows the quantification of fluorescence intensity via Image J in the lumen vs. the cytosol for LGACs incubated with or without inhibition of myosin Vb tail and FIG. 20B shows the ratio of lumen to cytosol.

DETAILED DESCRIPTION

Definitions

[0034] The practice of the present invention will employ, unless otherwise indicated, conventional techniques of tissue culture, immunology, molecular biology, microbiology, cell biology and recombinant DNA, which are within the skill of the art. See, e.g., Sambrook et al., (1989) Molecular Cloning: A Laboratory Manual, 2nd edition; Ausubel et al., eds. (1987) Current Protocols In Molecular Biology; MacPherson, B. D. Hames and G. R. Taylor eds., (1995) PCR 2: A Practical Approach; Harlow and Lane, eds. (1988) Antibodies, A Laboratory Manual; Harlow and Lane, eds. (1999) Using Antibodies, a Laboratory Manual; and R. I. Freshney, ed. (1987) Animal Cell Culture.

[0035] All numerical designations, e.g., pH, temperature, time, concentration, and molecular weight, including ranges, are approximations which are varied (+) or (-) by increments of 1.0 or 0.1, as appropriate. It is to be understood, although not always explicitly stated that all numerical designations are preceded by the term "about". It also is to be understood, although not always explicitly stated, that the reagents described herein are merely exemplary and that equivalents of such are known in the art.

[0036] As used in the specification and claims, the singular form "a," "an" and "the" include plural references unless the context clearly dictates otherwise.

[0037] As used herein, the term "comprising" is intended to mean that the compositions and methods include the recited elements, but do not exclude others. "Consisting essentially of" when used to define compositions and methods, shall mean excluding other elements of any essential significance to the combination when used for the intended purpose. Thus, a composition consisting essentially of the elements as defined herein would not exclude trace contaminants or inert carriers. "Consisting of" shall mean excluding more than trace elements of other ingredients and substantial method steps. Embodiments defined by each of these transition terms are within the scope of this invention.

[0038] A "composition" is also intended to encompass a combination of active agent and another carrier, e.g., compound or composition, inert (for example, a detectable agent or label) or active, such as an adjuvant, diluent, binder, stabilizer, buffers, salts, lipophilic solvents, preservative, adjuvant or the like. Carriers also include pharmaceutical excipients and additives proteins, peptides, amino acids, lipids, and carbohydrates (e.g., sugars, including monosaccharides, di-, tri-, tetra-, and oligosaccharides; derivatized sugars such as alditols, aldonic acids, esterified sugars and the like; and polysaccharides or sugar polymers), which can be present singly or in combination, comprising alone or in combination 1-99.99% by weight or volume. Exemplary protein excipients include serum albumin such as human serum albumin (HSA), recombinant human albumin (rHA), gelatin, casein, and the like. Representative amino acid/antibody components, which can also function in a buffering capacity, include alanine, glycine, arginine, betaine, histidine, glutamic acid, aspartic acid, cysteine, lysine, leucine, isoleucine, valine, methionine, phenylalanine, aspartame, and the like. Carbohydrate excipients are also intended within the scope of this invention, examples of which include but are not limited to monosaccharides such as fructose, maltose, galactose, glucose, D-mannose, sorbose, and the like; disaccharides, such as lactose, sucrose, trehalose, cellobiose, and the like; polysaccharides, such as raffinose, melezitose, maltodextrins, dextrans, starches, and the like; and alditols, such as mannitol, xylitol, maltitol, lactitol, xylitol sorbitol (glucitol) and myoinositol.

[0039] The term "pharmaceutically acceptable carrier" (or medium), which may be used interchangeably with the term biologically compatible carrier or medium, refers to reagents, cells, compounds, materials, compositions, and/or dosage forms that are not only compatible with the cells and other agents to be administered therapeutically, but also are, within the scope of sound medical judgment, suitable for use in contact with the tissues of human beings and animals without excessive toxicity, irritation, allergic response, or other complication commensurate with a reasonable benefit/risk ratio. Pharmaceutically acceptable carriers suitable for use in the present invention include liquids, semi-solid (e.g., gels) and solid materials (e.g., cell scaffolds and matrices, tubes sheets and other such materials as known in the art and described in greater detail herein). These semi-solid and solid materials may be designed to resist degradation within the body (nonbiodegradable) or they may be designed to degrade within the body (biodegradable, bioerodable). A biodegradable material may further be bioresorbable or bioabsorbable, i.e., it may be dissolved and absorbed into bodily fluids (water-soluble implants are one example), or degraded and ultimately eliminated from the body, either by conversion into other materials or breakdown and elimination through natural pathways.

[0040] As used herein, the term "patient" or "subject" intends an animal, a mammal or yet further a human patient. For the purpose of illustration only, a mammal includes but is not limited to a human, a feline, a canine, a simian, a murine, a bovine, an equine, a porcine or an ovine.

[0041] The term "purified protein or peptide" as used herein, is intended to refer to a composition, isolatable from other components, wherein the protein or peptide is purified to any degree relative to its naturally-obtainable state. A purified protein or peptide therefore also refers to a protein or peptide, free from the environment in which it may naturally occur. **[0042]** The term "therapeutic" refers to an agent or component capable of inducing a biological effect in vivo and/or in vitro. The biological effect may be useful for treating and/or preventing a condition, disorder, or disease in a subject or patient. A therapeutic may include, without limitation, a small molecule, a nucleic acid, or a polypeptide.

[0043] The term "coxsackievirus and adenovirus receptor" or "CAR" refers to a high affinity receptor that is present in many human tissues, including liver, heart, lacrimal gland, salivary gland, lung, and brain, pancreas and prostate.

[0044] The term "Polymeric Immunoglobulin Receptor" or "pIgR" refers to a high affinity receptor that is expressed by human mucosal cells.

[0045] "LGAC" or "lacrimal gland acinar cell" is a specific cell type of the lacrimal gland that expresses CAR and pIgR on the cell surface. These cells are also sometimes referred to lacrimal acinar epithelial cells.

[0046] This disclosure relates to genetically engineered polypeptide nanoparticles targeted to lacrimal gland acinar cells. To develop new treatments for disease of the lacrimal gland, new drug carriers are required that are biocompatible and easily modified with bioactive peptides. An emerging solution to this challenge utilizes genetically engineered polypeptide to drive the assembly of nanostructures. Elastin-like-polypeptide engages in a unique phase transition behavior, which can mediate self-assembly of nanoparticles. Described herein is a class of diblock ELP fusion proteins with high affinity peptides which are intended for targeting of lacrimal gland acinar cells (LGAC). The diblock mIgA-ELP fusion proteins are able to self assemble to nanoparticles, which can be utilized for gene therapy and drug delivery to LGAC and other mucosal epithelial cells.

[0047] As used herein, the term "biological equivalent thereof" is used synonymously with "equivalent" unless otherwise specifically intended. When referring to a reference protein, polypeptide or nucleic acid, intends those having minimal homology while still maintaining desired structure or functionality. Unless specifically recited herein, it is contemplated that any polynucleotide, polypeptide or protein mentioned herein also includes equivalents thereof. For example, an equivalent intends at least about 60%, or 65%, or 70%, or 75%, or 80% homology or identity and alternatively, at least about 85%, or alternatively at least about 90%, or alternatively at least about 95%, or alternatively 98% percent homology or identity and exhibits substantially equivalent biological activity to the reference protein, polypeptide or nucleic acid. Alternatively, a biological equivalent is a peptide encoded by a nucleic acid that hybridizes under stringent conditions to a nucleic acid or complement that encodes the peptide. Hybridization reactions can be performed under conditions of different "stringency". In general, a low stringency hybridization reaction is carried out at about 40° C. in about 10×SSC or a solution of equivalent ionic strength/temperature. A moderate stringency hybridization is typically performed at about 50° C. in about 6×SSC, and a high stringency hybridization reaction is generally performed at about 60° C. in about 1×SSC. Hybridization reactions can also be performed under "physiological conditions" which is well known to one of skill in the art. A non-limiting example of a physiological condition is the temperature, ionic strength, pH and concentration of Mg²⁺ normally found in a cell.

[0048] A polynucleotide or polynucleotide region (or a polypeptide or polypeptide region) having a certain percentage (for example, about 60%, 65%, 70%, 75%, 80%, 85%,

90%, 95% or 97%) of "sequence identity" to another sequence means that, when aligned, that percentage of bases (or amino acids) are the same in comparing the two sequences. The alignment and the percent homology or sequence identity can be determined using software programs known in the art, for example those described in Current Protocols in Molecular Biology (Ausubel et al., eds. 1987) Supplement 30, section 7.7.18, Table 7.7.1. Preferably, default parameters are used for alignment. A preferred alignment program is BLAST, using default parameters. In particular, preferred programs are BLASTN and BLASTP, using the following default parameters: Genetic code=standard; filter=none; strand=both; cutoff=60; expect=10; Matrix=BLOSUM62; Descriptions=50 sequences; sort by =HIGH SCORE; Databases=non-redundant, GenBank+ EMBL+DDBJ+PDB+GenBank CDS translations+SwissProtein+SPupdate+PIR. Details of these programs can be found at the following Internet address: ncbi.nlm.nih.gov/ cgi-bin/BLAST.

[0049] "Homology" or "identity" or "similarity" refers to sequence similarity between two peptides or between two nucleic acid molecules. Homology can be determined by comparing a position in each sequence which may be aligned for purposes of comparison. When a position in the compared sequence is occupied by the same base or amino acid, then the molecules are homologous at that position. A degree of homology between sequences is a function of the number of matching or homologous positions shared by the sequences. An "unrelated" or "non-homologous" sequence shares less than 40% identity, or alternatively less than 25% identity, with one of the sequences of the present invention.

[0050] An "equivalent" of a polynucleotide or polypeptide refers to a polynucleotide or a polypeptide having a substantial homology or identity to the reference polynucleotide or polypeptide. In one aspect, a "substantial homology" is greater than about 60%, 65%, 70%, 75%, 80%, 85%, 90%, 95% or 98% homology.

[0051] As used herein, "expression" refers to the process by which polynucleotides are transcribed into mRNA and/or the process by which the transcribed mRNA is subsequently being translated into peptides, polypeptides, or proteins. If the polynucleotide is derived from genomic DNA, expression may include splicing of the mRNA in an eukaryotic cell.

[0052] The term "encode" as it is applied to polynucleotides refers to a polynucleotide which is said to "encode" a polypeptide if, in its native state or when manipulated by methods well known to those skilled in the art, it can be transcribed and/or translated to produce the mRNA for the polypeptide and/or a fragment thereof. The antisense strand is the complement of such a nucleic acid, and the encoding sequence can be deduced therefrom.

[0053] "Regulatory polynucleotide sequences" intends any one or more of promoters, operons, enhancers, as know to those skilled in the art to facilitate and enhance expression of polynucleotides.

[0054] An "expression vehicle" is a vehicle or a vector, non-limiting examples of which include viral vectors or plasmids, that assist with or facilitate expression of a gene or polynucleotide that has been inserted into the vehicle or vector.

[0055] A "delivery vehicle" is a vehicle or a vector that assists with the delivery of an exogenous polynucleotide into

a target cell. The delivery vehicle may assist with expression or it may not, such as traditional calcium phosphate transfection compositions.

[0056] A "composition" is intended to mean a combination of active agent and another compound or composition, inert (for example, a solids support or pharmaceutically acceptable carrier) or active, such as an adjuvant.

[0057] A "pharmaceutical composition" is intended to include the combination of an active agent with a carrier, inert or active, making the composition suitable for diagnostic or therapeutic use in vitro, in vivo or ex vivo.

[0058] "An effective amount" refers to the amount of an active agent or a pharmaceutical composition sufficient to induce a desired biological and/or therapeutic result. That result can be alleviation of the signs, symptoms, or causes of a disease, or any other desired alteration of a biological system. The effective amount will vary depending upon the health condition or disease stage of the subject being treated, timing of administration, the manner of administration and the like, all of which can be determined readily by one of ordinary skill in the art.

[0059] As used herein, the terms "treating," "treatment" and the like are used herein to mean obtaining a desired pharmacologic and/or physiologic effect. The effect may be prophylactic in terms of completely or partially preventing a disorder or sign or symptom thereof, and/or may be therapeutic in terms of a partial or complete cure for a disorder and/or adverse effect attributable to the disorder.

[0060] As used herein, to "treat" further includes systemic amelioration of the symptoms associated with the pathology and/or a delay in onset of symptoms. Clinical and sub-clinical evidence of "treatment" will vary with the pathology, the subject and the treatment.

[0061] "Administration" can be effected in one dose, continuously or intermittently throughout the course of treatment. Methods of determining the most effective means and dosage of administration are known to those of skill in the art and will vary with the composition used for therapy, the purpose of the therapy, the target cell being treated, and the subject being treated. Single or multiple administrations can be carried out with the dose level and pattern being selected by the treating physician. Suitable dosage formulations and methods of administering the agents are known in the art. Route of administration can also be determined and method of determining the most effective route of administration are known to those of skill in the art and will vary with the composition used for treatment, the purpose of the treatment, the health condition or disease stage of the subject being treated, and target cell or tissue. Non-limiting examples of route of administration include oral administration, nasal administration, injection, topical application, intrapentoneal, intravenous and by inhalation. An agent of the present invention can be administered for therapy by any suitable route of administration. It will also be appreciated that the preferred route will vary with the condition and age of the recipient, and the disease being treated.

[0062] The agents and compositions of the present invention can be used in the manufacture of medicaments and for the treatment of humans and other animals by administration in accordance with conventional procedures, such as an active ingredient in pharmaceutical compositions.

[0063] As used herein, the term "detectable label" intends a directly or indirectly detectable compound or composition that is conjugated directly or indirectly to the composition to

be detected, e.g., N-terminal histadine tags (N-His), magnetically active isotopes, e.g., ¹¹⁵Sn, ¹¹⁷Sn and ¹¹⁹Sn, a non-radioactive isotopes such as ¹³C and ¹⁵N, polynucleotide or protein such as an antibody so as to generate a "labeled" composition. The term also includes sequences conjugated to the polynucleotide that will provide a signal upon expression of the inserted sequences, such as green fluorescent protein (GFP) and the like. The label may be detectable by itself (e.g. radioisotope labels or fluorescent labels) or, in the case of an enzymatic label, may catalyze chemical alteration of a substrate compound or composition which is detectable. The labels can be suitable for small scale detection or more suitable for high-throughput screening. As such, suitable labels include, but are not limited to magnetically active isotopes, non-radioactive isotopes, radioisotopes, fluorochromes, luminescent compounds, dyes, and proteins, including enzymes. The label may be simply detected or it may be quantified. A response that is simply detected generally comprises a response whose existence merely is confirmed, whereas a response that is quantified generally comprises a response having a quantifiable (e.g., numerically reportable) value such as an intensity, polarization, and/or other property. In luminescence or fluorescence assays, the detectable response may be generated directly using a luminophore or fluorophore associated with an assay component actually involved in binding, or indirectly using a luminophore or fluorophore associated with another (e.g., reporter or indicator) component.

[0064] Examples of luminescent labels that produce signals include, but are not limited to bioluminescence and chemiluminescence. Detectable luminescence response generally comprises a change in, or an occurrence of, a luminescence signal. Suitable methods and luminophores for luminescently labeling assay components are known in the art and described for example in Haugland, Richard P. (1996) Handbook of Fluorescent Probes and Research Chemicals (6th ed.). Examples of luminescent probes include, but are not limited to, aequorin and luciferases.

[0065] Examples of suitable fluorescent labels include, but are not limited to, fluorescein, rhodamine, tetramethyl-rhodamine, eosin, erythrosin, coumarin, methyl-coumarins, pyrene, Malacite green, stilbene, Lucifer Yellow, Cascade BlueTM, and Texas Red. Other suitable optical dyes are described in the Haugland, Richard P. (1996) Handbook of Fluorescent Probes and Research Chemicals (6th ed.).

[0066] In another aspect, the fluorescent label is functionalized to facilitate covalent attachment to a cellular component present in or on the surface of the cell or tissue such as a cell surface marker. Suitable functional groups, including, but not are limited to, isothiocyanate groups, amino groups, haloacetyl groups, maleimides, succinimidyl esters, and sulfonyl halides, all of which may be used to attach the fluorescent label to a second molecule. The choice of the functional group of the fluorescent label will depend on the site of attachment to either a linker, the agent, the marker, or the second labeling agent.

Elastin-Like Polypeptides (ELPs)

[0067] Elastin-like-polypeptides (ELPs) are a genetically engineered polypeptide with unique phase behavior (see for e.g. S. R. MacEwan, et al., Biopolymers 94(1) (2010) 60-77) which promotes recombinant expression, protein purification and self-assembly of nanostructures (see for e.g. A. Chilkoti, et al., Advanced Drug Delivery Reviews 54 (2002) 1093-

1111). ELPs are artificial polypeptides composed of repeated pentapeptide sequences, (VPGXG), (SEQ ID. NO: 1) derived from human tropoelastin, where X is the "guest residue" Which is any amino acid. In one embodiment, X is any amino acid except proline. This peptide motif displays rapid and reversible de-mixing from aqueous solutions above a transition temperature, Tr. Below Tr, ELPs adopt a highly water soluble random coil conformation; however, above T_{μ} they separate from solution, coalescing into a second aqueous phase. The T_t of ELPs can be tuned by choosing the guest residue and ELP chain length as well as fusion peptides at the design level (see for e.g. MacEwan S R, et al., Biopolymers 94(1): 60-77). The ELP phase is both biocompatible and highly specific for ELPs or ELP fusion proteins, even in complex biological mixtures. Genetically engineered ELPs are monodisperse, biodegradable, non-toxic. Throughout this description, ELPs are identified by the single letter amino acid code of the guest residue followed by the number of repeat units, n. For example, S48I48 represents a diblock copolymer ELP with 48 serine (S) pentamers ([VPGSG]₄₈, SEQ ID. NO: 2) at the amino terminus and 48 isoleucine (I) pentamers ([VPGIG]₄₈, SEQ ID. NO: 3) at the carboxy terminus. A "diblock" as used herein refers to an ELP with two blocks of repeated polypeptide sequence. For example, the diblock (VPGSG)₄₈ (VPGIG)₄₈ (SEQ ID. NO: 12) comprises 48 repeated units of a polypeptide having the sequence VPGSG (SEQ ID NO: 2) and 48 repeated units of a polypeptide having the sequence VPGIG (SEQ ID. NO: 3). In one embodiment, the drug delivery agent comprises a polypeptide with the sequence of SEQ ID. NO: 12.

[0068] In further embodiments, the drug delivery agent comprises, a consisting essentially of, or yet consists of, a polypeptide with the sequence (VPGSG)₉₆ (SEQ ID. NO: 13) or (VPGIG)₉₆ (SEQ ID. NO: 14) or a biological equivalent thereof.

[0069] Described herein are ELP fusion proteins, which can be self assembled into nanoparticles. The diameter of the nanoparticle can be from about 1 to about 1000 nm or from about 1 to about 500 nm, or from about 1 to about 100 nm, or from about 1 to about 50 nm, or from about 20 to about 50 nm. or from about 30 to about 50 nm, or from about 35 to about 45 nm. In one embodiment, the diameter is about 40 nm. These nanoparticles can be high efficiently internalized into LGAC. The fusion proteins are composed of elastin-like-polypeptides and high affinity polypeptides. These fusion proteins can be expressed from a variety of expression systems known to those skilled in the art and easily purified by the phase transition behavior of ELPs. These ELP fusion proteins are able to conjugate small molecules, such as, for example, chemotherapeutic agents, anti-inflammation agents, antibiotics and polypeptides and other water soluble drugs. In addition, the ELP nanoparticles are useful for carrying DNA, RNA, protein and peptide-based therapeutics.

[0070] ELPs have potential advantages over chemically synthesized polymers as drug delivery agents. First, because they are biosynthesized from a genetically encoded template, ELPs can be made with precise molecular weight. Chemical synthesis of long linear polymers does not typically produce an exact length, but instead a range of lengths. Consequently, fractions containing both small and large polymers yield mixed pharmacokinetics and biodistribution. Second, ELP biosynthesis produces very complex amino acid sequences with nearly perfect reproducibility. This enables very precise selection of the location of drug attachment. Thus drug can be

selectively placed on the corona, buried in the core, or dispersed equally throughout the polymer. Third, ELP can self assemble into multivalent nanoparticles that can have excellent site-specific accumulation and drug carrying properties. Fourth, because ELP are designed from native amino acid sequences found extensively in the human body they are biodegradable, biocompatible, and tolerated by the immune system. Fifth, ELPs undergo an inverse phase transition temperature, T_{ρ} above which they phase separate into large aggregates. By localized heating, additional ELP can be drawn into the target site, which may be beneficial for increasing drug concentrations.

[0071] A therapeutic such as a drug, for example, may be attached to the ELP through cysteine, lysine, glutamic acid or aspartic acid residues present in the polymer. In some embodiments, the cysteine, lysine, glutamic acid or aspartic acid residues are generally present throughout the length of the polymer. In some embodiments, the cysteine, lysine, glutamic acid or aspartic acid residues are clustered at the end of the polymer. In some embodiments of the presently described subject matter, therapeutics are attached to the cysteine residues of the ELP using thiol reactive linkers. In some embodiments of the presently described subject matter, therapeutics are attached to the lysine residues of the high molecular weight polymer sequence using NHS (N-hydroxysuccinimide) chemistry to modify the primary amine group present on these residues. In some embodiments of the presently described subject matter, therapeutics are attached to the glutamic acid or aspartic acid residues of the ELP using EDC (1-Ethyl-3-[3-dimethylaminopropyl]carbodiimide Hydrochloride) chemistry to modify the carboxylic acid group present on the ELP residues.

[0072] The therapeutic associated with the ELP may be hydrophobic or hydrophilic. Which the drug is hydrophobic, attachment to the terminus of the ELP may facilitate formation of the multivalent nanoparticle. The number of drug particles attached to the ELP can be from about 1 to about 30, or from about 1 to about 10, or about 1, 2, 3, 4, 5, 6, 7, 8, 9, or 10. In some embodiments, the attachment points for a therapeutic are equally distributed along the backbone of the ELP, and the resulting drug-ELP is prevented from forming nanoparticle structures under physiological salt and temperature conditions.

[0073] In addition to therapeutics, the ELPs may also be associated with a detectable label that allows for the visual detection of in vivo uptake of the ELPs. Suitable labels include, for example, fluorescein, rhodamine, tetramethyl-rhodamine, eosin, erythrosin, coumarin, methyl-coumarins, pyrene, Malacite green, Alexa-Fluor®, stilbene, Lucifer Yellow, Cascade BlueTM, and Texas Red. Other suitable optical dyes are described in Haugland, Richard P. (1996) Molecular Probes Handbook.

[0074] In certain embodiments, the ELP components include polymeric or oligomeric repeats of the pentapeptide VPGXG (SEQ ID. NO: 1), where the guest residue X is any amino acid, that in one aspect, excludes proline. X may be a naturally occurring or non-naturally occurring amino acid. In some embodiments, X is selected from alanine, arginine, asparagine, aspartic acid, cysteine, glutamic acid, glutamine, glycine, histidine, isoleucine, leucine, lysine, methionine, phenylalanine, serine, threonine, tryptophan, tyrosine and valine. In some embodiments, X is a natural amino acid other than proline or cysteine.

[0075] The guest residue X may be a non-classical (nongenetically encoded) amino acid. Examples of non-classical amino acids include: D-isomers of the common amino acids, 2,4-diaminobutyric acid, α -amino isobutyric acid, A-aminobutyric acid, Abu, 2-amino butyric acid, γ -Abu, ϵ -Ahx, 6-amino hexanoic acid, Aib, 2-amino isobutyric acid, 3-amino propionic acid, ornithine, norleucine, norvaline, hydroxyproline, sarcosine, citrulline, homocitrulline, cysteic acid, t-butylglycine, t-butylalanine, phenylglycine, cyclohexylalanine, β -alanine, fluoro-amino acids, designer amino acids such as β -methyl amino acids, C α -methyl amino acids, N α -methyl amino acids, and amino acid analogs in general.

[0076] Selection of X is independent in each ELP structural unit (e.g., for each structural unit defined herein having a guest residue X). For example, X may be independently selected for each structural unit as an amino acid having a positively charged side chain, an amino acid having a negatively charged side chain, or an amino acid having a neutral side chain, including in some embodiments, a hydrophobic side chain.

[0077] In each embodiment, the structural units, or in some cases polymeric or oligomeric repeats, of the ELP sequences may be separated by one or more amino acid residues that do not eliminate the overall effect of the molecule, that is, in imparting certain improvements to the therapeutic component as described. In certain embodiments, such one or more amino acids also do not eliminate or substantially affect the phase transition properties of the ELP component (relative to the deletion of such one or more amino acids).

[0078] The ELP component in some embodiments is selected or designed to provide a T, ranging from about 10 to about 80° C., such as from about 35 to about 60° C., or from about 38 to about 45° C. In some embodiments, the T, is greater than about 40° C. or greater than about 42° C, or greater than about 45° C., or greater than about 50° C. The transition temperature, in some embodiments, is above the body temperature of the subject or patient (e.g., >37° C.) thereby remaining soluble in vivo, or in other embodiments, the T, is below the body temperature (e.g., <37° C.) to provide alternative advantages, such as in vivo formation of a drug depot for sustained release of the therapeutic agent.

[0079] The T_t of the ELP component can be modified by varying ELP chain length, as the Tt generally increases with decreasing MW. For polypeptides having a molecular weight >100,000, the hydrophobicity scale developed by Urry et al. (PCT/US96/05186, which is hereby incorporated by reference in its entirety) is preferred for predicting the approximate T_t of a specific ELP sequence. However, in some embodiments, ELP component length can be kept relatively small, while maintaining a target T_t, by incorporating a larger fraction of hydrophobic guest residues (e.g., amino acid residues having hydrophobic side chains) in the ELP sequence. For polypeptides having a molecular weight <100,000, the T_t may be predicted or determined by the following quadratic function: T_t=M₀+M₁X+M₂X² where X is the MW of the fusion protein, and M₀=116.21; M₁=-1.7499; M₂=0.010349.

[0080] While the T, of the ELP component, and therefore of the ELP component coupled to a therapeutic component, is affected by the identity and hydrophobicity of the guest residue, X, additional properties of the molecule may also be affected. Such properties include, but are not limited to solubility, bioavailability, persistence, and half-life of the molecule.

Ligands

[0081] In certain embodiments of the invention, the therapeutic agent comprises an ELP component fused or conjugated to a LGAC-targeted ligand. A LGAC-targeted ligand is a peptide, polypeptide, or molecule that targets the ELP to the LGAC. In one embodiment, the ligand component of the drug delivery agent described herein is the adenovirus knob domain, which is a LGAC-targeted ligand. This domain is represented by the protein sequence: GAITVGNKNND-KLTLWTTPAPSPNCRLNAEKDAKLTLV-

LTKCGSQILATVSVLAVKGSL APISGTVQSAHLIIR-FDENGVLLNNSFLDPEYWNFRNGDLTEGTAYTNAV GFMPNLSAY PKSHGKTAKSNIVSQVYLNGDKTK-PVTLTITLNGTQETGDTTPSAYSMSFSWDWSGHN

YINEIFATSSYTFSYIAQE (SEQ ID. NO: 4), or a biological equivalent thereof. The term "biological equivalent" is defined above. In one aspect, a biological equivalent" is peptide encoded by a nucleic acid that hybrizes to a nucleic acid that encodes the LGAC-targeted ligand 2 or its complement under conditions of a high stringency hybridization reaction, that is performed at about 60° C. in about 1×SSC that has substantial identical biological activity to the abovenoted sequence. In one embodiment, the knob ligand comprises a polypeptide having the sequence of SEQ ID. NO: 4 or a biological equivalent thereof.

[0082] In certain embodiments, the ELP comprises knob or a polypeptide with at least 80% identity to knob. Alternatively, the polypeptide has about at least 85% or about at least 90% or about at least 95%, or about at least 99% identity to knob.

[0083] In further embodiments, the ELP comprises a mIgA ligand or double mIgA ligand. This ligand is represented by the amino acid sequence: TWASRQEPSQGTTTFAVTS (SEQ ID. NO: 5) or a biological equivalent thereof. In one embodiment, the mIgA ligand comprises a polypeptide having the sequence of SEQ ID. NO: 5 or a biological equivalent thereof. The term "biological equivalent" is defined above. In one aspect, a biological equivalent is a peptide encoded by a nucleic acid that hybrizes to a nucleic acid that encodes the mIgA ligand or double mIgA ligand or its complement under conditions of a high stringency hybridization reaction, that is performed at about 60° C. in about 1×SSC that has substantial identical biological activity to the above-noted sequence. In certain embodiments, the ELP comprises the mIgA ligand or a polypeptide with at least 80% identity to mIgA. Alternatively, the polypeptide has about at least 85% or about at least 90% or about at least 95%, or about at least 99% identity to mIgA. The term "mIgA" refers to the pIgR-binding site in the $C\alpha 3$ domain of dimeric human IgA. The $C\alpha 3$ domain is represented by the protein sequence: RP EVHLLPPPSE ELALNELVTL TCLARGFSPK DVLVRWLQGS QEL-PREKYLT WASRQEPSQG TTTFAVTSIL RVAAED-WKKG DTFSCMVGHE ALPLAFTQKT ID (SEQ ID. NO: 6) (See for e.g. Frank W. Putnam, et al. J. Biol. Chem. 254, 2865-2874).

Expression of Recombinant Proteins

[0084] ELPs and other recombinant proteins described herein can be prepared by expressing polynucleotides encoding the polypeptide sequences of this invention in an appropriate host cell, i.e., a prokaryotic or eukaryotic host cell This can be accomplished by methods of recombinant DNA technology known to those skilled in the art. It is know to those

skilled in the art that modifications can be made to any peptide to provide it with altered properties. Polypeptides of the invention can be modified to include unnatural amino acids. Thus, the peptides may comprise D-amino acids, a combination of D- and L-amino acids, and various "designer" amino acids (e.g., β -methyl amino acids, C- α -methyl amino acids, and N- α -methyl amino acids, etc.) to convey special properties to peptides. Additionally, by assigning specific amino acids at specific coupling steps, peptides with α -helices, β turns, β sheets, α -turns, and cyclic peptides can be generated. Generally, it is believed that beta-turn spiral secondary structure or random secondary structure is preferred.

[0085] The ELPs can be expressed and purified from a suitable host cell system. Suitable host cells include prokaryotic and eukaryotic cells, which include, but are not limited to bacterial cells, yeast cells, insect cells, animal cells, mammalian cells, murine cells, rat cells, sheep cells, simian cells and human cells. Examples of bacterial cells include Escherichia coli, Salmonella enterica and Streptococcus gordonii. In one embodiment, the host cell is E. coli. The cells can be purchased from a commercial vendor such as the American Type Culture Collection (ATCC, Rockville Md., USA) or cultured from an isolate using methods known in the art. Examples of suitable eukaryotic cells include, but are not limited to 293T HEK cells, as well as the hamster cell line BHK-21; the murine cell lines designated NIH3T3, NS0, C127, the simian cell lines COS, Vero; and the human cell lines HeLa, PER.C6 (commercially available from Crucell) U-937 and Hep G2. A non-limiting example of insect cells include Spodoptera frugiperda. Examples of yeast useful for expression include, but are not limited to Saccharomyces, Schizosaccharomyces, Hansenula, Candida, Torulopsis, Yarrowia, or Pichia. See e.g., U.S. Pat. Nos. 4,812,405; 4,818,700; 4,929,555; 5,736, 383; 5,955,349; 5,888,768 and 6,258,559.

Protein Purification

[0086] The phase transition behavior of the ELPs allows for easy purification. The ELPs may also be purified from host cells using methods known to those skilled in the art. These techniques involve, at one level, the crude fractionation of the cellular milieu to polypeptide and non-polypeptide fractions. Having separated the polypeptide from other proteins, the polypeptide of interest may be further purified using chromatographic and electrophoretic techniques to achieve partial or complete purification (or purification to homogeneity). Analytical methods particularly suited to the preparation of a pure peptide or polypeptide are filtration, ion-exchange chromatography, exclusion chromatography, polyacrylamide gel electrophoresis, affinity chromatography, or isoelectric focusing. A particularly efficient method of purifying peptides is fast protein liquid chromatography or even HPLC. In the case of ELP compositions protein purification may also be aided by the thermal transition properties of the ELP domain as described in U.S. Pat. No. 6,852,834.

[0087] Generally, "purified" will refer to a protein or peptide composition that has been subjected to fractionation to remove various other components, and which composition substantially retains its expressed biological activity. Where the term "substantially purified" is used, this designation will refer to a composition in which the protein or peptide forms the major component of the composition, such as constituting about 50%, about 60%, about 70%, about 80%, about 90%, about 95% or more of the proteins in the composition. **[0088]** Various methods for quantifying the degree of purification of the protein or peptide will be known to those of skill in the art in light of the present disclosure. These include, for example, determining the specific activity of an active fraction, or assessing the amount of polypeptides within a fraction by SDS/PAGE analysis. A preferred method for assessing the purity of a fraction is to calculate the specific activity of the initial extract, and to thus calculate the degree of purity, herein assessed by a "-fold purification number." The actual units used to represent the amount of activity will, of course, be dependent upon the particular assay technique chosen to follow the purification and whether or not the expressed protein or peptide exhibits a detectable activity.

[0089] Various techniques suitable for use in protein purification will be well known to those of skill in the art. These include, for example, precipitation with ammonium sulfate, PEG, antibodies and the like or by heat denaturation, followed by centrifugation; chromatography steps such as ion exchange, gel filtration, reverse phase, hydroxylapatite and affinity chromatography; isoelectric focusing; gel electrophoresis; and combinations of such and other techniques. As is generally known in the art, it is believed that the order of conducting the various purification steps may be changed, or that certain steps may be omitted, and still result in a suitable method for the preparation of a substantially purified protein or peptide.

Pharmaceutical Compositions

[0090] Pharmaceutical compositions are further provided. The compositions comprise a carrier and ELPs as described herein. The carriers can be one or more of a solid support or a pharmaceutically acceptable carrier. In one aspect, the compositions are formulated with one or more pharmaceutically acceptable excipients, diluents, carriers and/or adjuvants. In addition, embodiments of the compositions include ELPs, formulated with one or more pharmaceutically acceptable auxiliary substances.

[0091] The invention provides pharmaceutical formulations in which the one or more of an isolated polypeptide of the invention, an isolated polynucleotide of the invention, a vector of the invention, an isolated host cell of the invention. or an antibody of the invention can be formulated into preparations for injection in accordance with the invention by dissolving, suspending or emulsifying them in an aqueous or nonaqueous solvent, such as vegetable or other similar oils, synthetic aliphatic acid glycerides, esters of higher aliphatic acids or propylene glycol; and if desired, with conventional additives such as solubilizers, isotonic agents, suspending agents, emulsifying agents, stabilizers and preservatives or other antimicrobial agents. A non-limiting example of such is a antimicrobial agent such as other vaccine components such as surface antigens, e.g. a Type IV Pilin protein (see Jurcisek and Bakaletz (2007) J. of Bacteriology 189(10):3868-3875) and antibacterial agents.

[0092] Aerosol formulations provided by the invention can be administered via inhalation. For example, embodiments of the pharmaceutical formulations of the invention comprise a compound of the invention formulated into pressurized acceptable propellants such as dichlorodifluoromethane, propane, nitrogen and the like.

[0093] Embodiments of the pharmaceutical formulations of the invention include those in which the ELP is formulated in an injectable composition. Injectable pharmaceutical for-

mulations of the invention are prepared as liquid solutions or suspensions; or as solid forms suitable for solution in, or suspension in, liquid vehicles prior to injection. The preparation may also be emulsified or the active ingredient encapsulated in liposome vehicles in accordance with other embodiments of the pharmaceutical formulations of the invention.

[0094] Suitable excipient vehicles are, for example, water, saline, dextrose, glycerol, ethanol, or the like, and combinations thereof. In addition, if desired, the vehicle may contain minor amounts of auxiliary substances such as wetting or emulsifying agents or pH buffering agents. Methods of preparing such dosage forms are known, or will be apparent upon consideration of this disclosure, to those skilled in the art. See, e.g., Remington's Pharmaceutical Sciences, Mack Publishing Company, Easton, Pa., 17th edition, 1985. The composition or formulation to be administered will, in any event, contain a quantity of the compound adequate to achieve the desired state in the subject being treated.

[0095] Routes of administration applicable to the methods and compositions described herein include intranasal, intramuscular, subcutaneous, intradermal, topical application, intravenous, nasal, oral, inhalation, intralacrimal, retrolacrimal profusal along the duct, intralacrimal, and other enteral and parenteral routes of administration. Routes of administration may be combined, if desired, or adjusted depending upon the agent and/or the desired effect. An active agent can be administered in a single dose or in multiple doses. Embodiments of these methods and routes suitable for delivery, include systemic or localized routes. In one embodiment, the composition comprising the ELP is administered intralacrimally through injection. In further embodiments, the composition is administered systemically, topically on top of the eye, by retrolacrimal profusion, or intranasally.

Treatment of Disease

[0096] Methods and compositions disclosed herein are useful in treating disorders of the eye. The lacrimal gland acinar cell targeted ELPs provide a site-specific target therapeutic. Accordingly, these ELP nanoparticles may be useful to encapsulate or attach drugs for treating disorders localized to the eye. By way of example, these disorders can include, age-related macular degeneration, Sjögren's syndrome, autoimmune exocrinopathy, diabetic retinopathy, graft versus host disease (exocrinopathy associated with) retinal venous occlusions, retinal arterial occlusion, macular edema, postoperative inflammation, uveitis retinitis, proliferative vitreoretinopathy and glaucoma. In one embodiment, the disease is Sjögren's syndrome. In another embodiment, the disease is keratoconjunctivitis sicca (dry eye). In another embodiment the disease is scleritis. In another embodiment the disease is glaucoma.

Combination Treatments

[0097] Administration of the therapeutic agent or substance of the present invention to a patient will follow general protocols for the administration of that particular secondary therapy, taking into account the toxicity, if any, of the treatment. It is expected that the treatment cycles would be repeated as necessary. It also is contemplated that various standard therapies, as well as surgical intervention, may be applied in combination with the described therapy.

Example 1

ELPs Comprising Targeting Ligands

[0098] Since discovered a half century ago, human adenovirus has attracted attention because different types cause significant levels of respiratory, ocular, and gastrointestinal disease. Because of its pathological effects, a significant amount of information is therefore available on its mode of interaction with cells. Adenovirus serotype 2 and serotype 5 within subgroup C, the best understood types of this virus, attach to cells through the initial binding of the fiber protein to the cell-surface coxsackievirus and adenovirus receptor (CAR). CAR is a 46-kDa high affinity receptor that is present in many human tissues, including liver, heart, lacrimal gland, lung, and brain and which is thought to function as a cell adhesion protein. Upon surface binding, adenovirus entry in most cells is facilitated through interaction of an additional adenoviral capsid protein, the penton base, with integrin receptors on the plasma membrane, a process facilitating efficient entry via endocytosis. This mechanism, which occurs in cells expressing the most abundant CAR protein in the body, has been reported to deliver a region of the fiber capsid protein, the knob, to a subcellular degradative compartment. After entry, through either fiber/knob- or pentondependent interactions, mechanisms have been described for the subsequent interactions between the virus and other intracellular transport machinery, which facilitate efficient trafficking of the viral DNA to the nucleus. For these and other reasons, most notably the ability of adenovirus to transduce non-dividing cells, adenovirus serotype 5 and other serotypes have been explored as vectors for gene therapy. However, despite their relatively efficient cellular endocytosis and gene transfer, viral vectors in general have intrinsic drawbacks, such as limited opportunities for repeat administrations due to acute inflammatory responses and delayed humoral or cellular immune responses. In addition, some viral vectors integrate DNA into the genome, resulting in insertional mutagenesis.

[0099] In the past few decades, numerous research groups have focused on drug carriers, such as liposomes, micelles, dendrimers, and polymersomes. Relatively few drug carriers have been approved for use in humans, which suggests that better strategies and materials may be required to generate successful nanomedicines. One emerging strategy is to design genetically engineered protein polymers that self-assemble directly into nanoparticles. For example, the elastinlike-polypeptides (ELP) are a genetically engineered polypeptide with unique phase behavior, which promotes recombinant expression, protein purification and self-assembly of nanostructures. Genetically engineered ELPs are biodegradable and biocompatible. ELPs are composed of the repeated amino acid sequence (VPGXG), (SEQ ID. NO: 1), where the hydrophobicity of X determines the polypeptide phase behavior. Exemplified herein, ELPs are identified by the single letter amino acid code of the guest residue followed by the number of repeat units, n. For example, S48I48 represents a diblock copolymer ELP with 48 serine (S) pentamers at the amino terminus and 48 isoleucine (I) pentamers at the carboxy terminus.

[0100] Lacrimal acinar epithelial cells exhibit a unique fiber-dependent internalization mechanism for adenovirus type 5, and this internalization mechanism can be recapitulated by the knob domain of the fiber protein. This mechanism seems to operate in hepatocytes as well to enable internaliza-

tion of free knob protein to intracellular degradative compartments. This is in contrast to other demonstrations that fiber is responsible only for the initial binding of adenovirus to the cell via CAR, and not for internalization, which is driven by the penton base capsid protein and integrin receptors on the plasma membrane, a process facilitating efficient entry. Some studies have recently shown that CAR, which is a cell adhesion protein and thought to be largely surface associated, can in fact be endocytosed. Altogether these studies suggest that in certain cells, such as acinar cells and hepatocytes where CAR is highly abundant, that a subpopulation may serve as an internalization receptor when bound to fiber or knob proteins. The physiological relevance of this endocytotic population of CAR in these cells is so far unknown. To exploit this apparent CAR internalization pathway and high affinity interaction with viral proteins for drug delivery while minimizing the use of the entire viral capsid, described herein is the development of a simple gene product that assembles nanoparticles decorated with the knob domain of adenovirus fiber protein. The most significant advantages of this platform include: (i) compatibility with genetic engineering; (ii) no bioconjugate chemistry is required to link fusion proteins to the nanoparticle; (iii) and the resulting polypeptides assemble into nanoparticles that are monodisperse, multivalent, and biodegradable. These particles are predominantly composed of diblock copolymers of ELP. ELP block copolymers self-assemble multimeric nanoparticles above a transition temperature that can be controlled by adjusting their hydrophobicity and molecular weight (FIG. 1). Above the critical temperature for the ELP diblock copolymer, the knob-ELP fusion protein also assembles nanoparticles. It was investigated whether nanocarriers displaying the knob domain may exhibit selective internalization into tissues expressing unique CAR-dependent endoyctosis of fiber and knob. Described herein are the biophysical properties and cellular uptake of a knob-ELP, which self assembles nanoparticles that have potential applications for drug delivery and gene therapy.

Materials and Reagents

[0101] TB dry powder growth medium was purchased from MO BIO Laboratories, Inc. (Carlsbad, Calif.). NHS-Rhodamine was purchased from Thermo Fisher Scientific (Rockford, Ill.). Thrombin CleanCleave™ Kit, Polyethylenimine, Copper Chloride and insulin were obtained from Sigma-Aldrich (St. Louis, Mo.). The knob domain gene sequence was ordered from Integrated DNA Technologies (Coralville, Iowa). LysoTracker Green CN 26 was purchased from Invitrogen (Carlsbad, Calif.). Goat anti-mouse CAR antibody was obtained from R&D Systems (Minneapolis, Minn.). IRDye®800-conjugated donkey anti-goat second antibody was purchased from Rockland (Gilbertsville, Pa.). Blocking buffer was purchased from Li-COR Biosciences (Lincoln, Nebr.). The QIAprep Spin Miniprep Kit and QIAquick Gel Extraction Kit were purchased from Qiagen (Valencia, Calif.).

Knob-ELP Vector Design

[0102] The plasmids encoding ELP were designed similarly to those reported previously (see, for e.g., A. Chilkoti, et al., Advanced Drug Delivery Reviews 54 (2002) 1093-1111 and J. R. McDaniel, et al., Biomacromolecules 11(4) (2010) 944-952 which is incorporated by reference). The knob domain gene sequence was designed with restriction enzyme

NdeI and BamHI at 5' and 3' of the knob gene respectively. A thrombin amino acid recognition site (GLVPRGS; SEQ ID. NO: 7) was incorporated between the knob sequence and the ELP sequence. A recognition site for BseRI was also incorporated to facilitate the insertion of ELP genes with complementary two base pair 5' overhang(s). The plasmids containing genes that encode for ELP and knob were double digested by BseRI and BssHII, and the DNA pieces containing ELP and knob were purified using a gel extraction kit and then ligated together. Successful clones were confirmed by diagnostic DNA digestion, DNA sequencing, and mass spectrometry of the polypeptide gene products.

Purification of ELP Fusion Proteins

[0103] E. coli strain BLR (Novagen Inc., Milwaukee, Wis.) was transformed with the modified pET-25(+) expression vectors containing the ELP or knob-ELP genes. The bacteria were grown overnight in 5 mL TB dry medium supplemented with 1 µg/mL ampicillin in an orbital shaker at 37° C. Then bacteria were centrifuged down, and the pellet was resuspended in 2 liters TB dry medium and cultured for 24 hours in an orbital shaker at 37° C. The bacteria were again harvested by centrifugation at 4° C. and resuspended in phosphate buffer saline (PBS). The bacteria were lysed by discontinuous pulsed ultrasonication in an ice-water bath. The insoluble debris was removed from the lysate by centrifugation and nucleic acids were precipitated by adding polyethylenimine (0.5% w/v final concentration) and removed by centrifugation at 4° C. From the clarified bacterial lysates, the ELPs and knob-ELPs were purified by inverse transition cycling (ITC), which has been described previously [20-22]. Briefly, ELP solutions were warmed at room temperature and NaCl was added (1-3 M final concentration) to induce the ELP phase separation. The aggregated ELP fusion polypeptides were separated from the lysate by centrifugation at room temperature. The ELP pellet was resolubilized in PBS within an ice-water bath. The resolubilized ELP solution was centrifuged at 4° C. to remove remaining aggregated proteins. It was previously reported that purification cycles were repeated for two to six rounds as needed to purify various ELP fusion proteins (See, for e.g., D. E. Meyer, et al., Nature Biotechnology 17 (1999) 1112-111520, and K. Trabbic-Carlson, et al., Protein Sci 13(12) (2004) 3274-3284 which is herein incorporated by reference). In this study, the purification cycle was repeated five times to remove nearly all of the contaminating E. coli proteins, which was essential because contaminants may aggregate during heating and bias the hydrodynamic radius. The purity of purified knob-ELP was measured using SDS-PAGE in a 10% gel. After electrophoresis, the gel was stained with Coomassie brilliant blue.

Characterization of Knob-ELP

[0104] As described above, the knob-ELP was designed as a fusion protein consisting of a knob domain and an ELP. To study these multifunctional polypeptides, they were characterized by non-denaturing PAGE, turbidometric analysis of their temperature-dependent phase behavior, and dynamic light scattering. Native fiber/knob proteins are trimeric; therefore, the ability of knob-ELPs to self-associate was characterized using non-denaturing PAGE. Knob-S48I48 and recombinant knob was mixed with sample buffer without 2-mercaptoethanol, and then loaded onto a 10% polyacrylamide gel without SDS at 4° C. At this temperature, the ELP

nanoparticles remain dissociated, which enables the polypeptides to enter the gel. After three hours of electrophoresis, the gel was stained with Coomassie brilliant blue.

[0105] To explore the temperature-dependent phase behavior of the ELPs, optical density and hydrodynamic radius were observed over a range of temperatures. Knob-596, S48I48 and knob-S48I48 were diluted to 25 µM in PBS on ice and the absorbance at 350 nm was monitored with a DU800 UV-Vis spectrophotometer (Beckman Coulter, Brea, Calif.) at a temperature gradient of 1° C./minute. For dynamic light scattering studies, S48I48 and knob-S48I48 were diluted to 25 µM in PBS and passed through 20 nm membrane filters at 4° C., and BSA, a protein with a similar molecular to knob-S48I48 was used as a control. Then 90 µL sample of was transferred into a 384 well microplate and covered with 20 μL mineral oil. The microplate and mineral oil were pre-chilled at 4° C. at least for 1 hour. The microplate was centrifuged at 4° C. to remove air bubbles from samples before and after addition of mineral oil. Then the sample was measured in a DynaPro plate reader (Wyatt Inc., Santa Barbara, Calif.) at temperature intervals of 1° C. The resulting hydrodynamic radii were collected and analyzed by Dynamics (Wyatt Inc., Santa Barbara, Calif.). The measurements were repeated three times and particle radius for BSA, S48I48 and knob-S48I48 at 15° C. and 37° C. were analyzed by a one-way analysis of variance (R^2 =1.000, p=10⁻²⁰, n=18).

Thrombin Cleavage of Knob-ELP

[0106] A thrombin recognition site was designed between the knob domain and ELP sequence (Table 1), which was cleaved by thrombin (Sigma-Aldrich, St. Louis, Mo.). Thrombin immobilized on agarose beads was centrifuged to remove the storage buffer and washed with cleavage buffer (from the thrombin cleavage kit). The knob-S48I48 was then diluted with cleavage buffer to 1 mg/mL and suspended with thrombin agarose slurry for 24 hours at room temperature. After incubation, the thrombin agarose beads were removed by centrifugation. The cleaved knob (21.7 kD) was resolved by SDS-PAGE and gels were stained with Coomassie brilliant blue. The SDS-PAGE gel was scanned with a Molecular Imager Gel Doc XR System (Bio-Rad, Hercules, Calif.) and analyzed with software Quantity one (Bio-Rad).

TABLE 1

	Summary of	Expressed Po	lypeptides		
Peptide label	*Amino acid sequence	**Critical aggregation temperature (° C.)	Expected molecular weight (kD)	*** Measured molecular weight (kD)	1 1
knob-S96	knob-(VPGSG) ₉₆ Y (SEQ ID. NO: 8)	68.2	60.179	_	5.3
knob-196	knob-(VPGIG) ₉₆ Y (SEQ ID. NO: 9)	_	62.682	-	_
knob-S48I48	knob- G(VPGSG) ₄₈ (VPGIG) ₄₈ Y (SEQ ID. NO: 10)	19.5	61.431	61.241	21.7
S48I48	G(VPGSG) ₄₈ (VPGIG) ₄₈ Y (SEQ ID. NO: 10)	26.5	39.643	39.670	23.7

*Knob amino acid sequence with thrombin cleavage site underlined:

GAITVGNKNNDKLTLWTTPAPSPNCRLNAEKDAKLTLVLTKCGSQILATVSVLAVKGSLAPISGTVQSAHLIIRFDENGVLLNNSFLDPEYMNFRNG DLTEGTAYTNAVGFMPNLSAYPKSHGKTAKSNIVSQVYLNGDKTKPVTLTITLNGTQETGDTTPSAYSMSFSWDWSGHNYINEIFATSSYTFSYIAQ E<u>GLVPRGSG</u> (SEQ ID. NO: 11)

**determined using optical density by UV-Vis spectrophotometer.

***determined using MALDI mass spectrometry.

****determined using dynamic light scattering.

Self-Assembly or Disassembly of Nanoparticles-Above/Below their Phrase Transition Temperatures

	TABLE :	2		
	Summary of Expressed	Polypeptides	1	
		Measured molecular weight	Trans: Temper (° (ature
Peptide	Amino acid sequence	(kDa)	Τ1	Τ2
S48I48	$G(VPGSG)_{48}(VPGIG)_{48}Y$ (SEQ ID. NO: 10)	39.67	26.5	75
knob-S48I48	8 knob-G(VPGSG) ₄₈ (VPGIG) ₄₈ Y (SEQ ID. NO: 10)	61.24	19.5	60

Conjugation with NHS-Rhodamine

[0107] To track cellular uptake, the ELPs S48I48 and knob-S48I48 were conjugated with a detectable label, NHS-Rhodamine (Thermo Fisher Scientific Inc, Rockford, Ill.) via covalent modification of primary amines at the amino end of the peptide. For S48I48, the only available amine is at the amino terminus; however, knob-S48I48 has an additional 11 lysine residues that may be sites of modification. The conjugation was performed in 100 mM borate buffer for 2 hours at 4° C., and the conjugated ELP was separated by size exclusion chromatography on a PD10 desalting column (GE Healthcare, Piscataway, N.J.).

Cellular Uptake of Knob-ELP/ELP

[0108] Hepatocytes were expected to be enriched in the CAR receptor, according to previous reports (see, for e.g., J. Xie, L. et al., J. Virol. 80(23) (2006) 11833-11851). To confirm this, a western blot was performed on a murine hepatocyte cell-line. CHO cells were used as a negative control. 2×10^4 cells were mixed with SDS-PAGE sample buffer and heated above 95° C. for 5 minutes. CAR was detected by western blotting using a goat anti-mouse CAR antibody as the primary antibody and IRDye®800-conjugated donkey antigoat antibody as the secondary antibody. The result was scanned using an Odyssey® Imaging System (Li-COR, Lincoln, Nebr., USA) and quantified with the Odyssey® 1.1 software.

[0109] To observe uptake into mouse hepatocytes, cells were cultured on 35 mm glass coverslip-bottomed dishes with medium [(DMEM (4.5 g/L) containing 10% fetal bovine serum, 5 µg/ml insulin, and 0.02 µg/ml epidermal growth factor]. Uptake studies were conducted when hepatocytes reached 70% confluence. After washing with warm fresh medium, hepatocytes were cultured in medium containing 10 µM of either S48I48 or knob-S48I48 conjugated with rhodamine, and 75 nM LysoTracker green. After 30 minutes incubation at 37° C., the cells were rinsed with warm fresh medium to remove the free knob-ELP/ELP in the medium. Next cells were incubated with 75 nM LysoTracker green in a 37° C. incubation chamber. The chamber is mounted on a Zeiss LSM 510 Meta confocal microscope system, which is equipped with argon and red and green HeNe lasers and mounted on a vibration-free table.

[0110] To demonstrate the specificity of knob-ELP internalization for the CAR pathway, hepatocytes were pre-bound with goat anti-mouse CAR antibody. After confirming that the goat anti-mouse CAR antibody has a high affinity with the mouse hepatocytes, the anti-mouse CAR antibody (0.2 mg/mL) was diluted with warm medium 10-fold and incubated with the hepatocytes for 30 minutes at 37° C. Knob-S48I48 conjugated with rhodamine was then added to the medium at a concentration of 10 μ M. After 30 minutes incubation with knob-S48I48 and 75 nM LysoTracker green, the hepatocytes were rinsed, then incubated in fresh warm medium with 75 nM LysoTracker green and imaged as described above.

Example 2

Transcytosis of Knob-ELPs to Lacrimal Gland Acinar Lumen

[0111] Intracellular uptake of carboxyfluorescein (CF)conjugated ELPs in lacrimal gland acinar cells (LGACs) is shown in FIG. **13**. Unlike CF-S48I48, CF-Knob-S48I48 exhibits strong internalization which was shown in green in reconstituted LGACs. FIG. **13** shows that endocytosed CF-Knob-S48I48 was transcytosed into reconstituted acinar lumen which was stained by expressed Lifeact-RFP proteins (red). Lumen A (S48I48) and lumen B (Knob-S48I48) are shown in FIG. **14**. Internalized knob-S48I48 was transcytosed into the luminal area of LGACs as shown in lumen B.

[0112] In a separate experiment the basal-to-apical transport of Cy5-Knob-S48I48 in primary cultures of Lacrimal Gland Acinar Cells (LGACs) was observed. As shown in FIG. 17, uptake of Cy5-Knob-S48I48 in LGACs with overexpressed RFP-Rab5a. Rabbit LGACs were transduced on day 2 with Adenovirus encoding RFP-Rab5a (red) in order to stain early endosome structures. After 16-18 hours LGACs were incubated with 30 µM Cy5-Knob-S48I48 (green) at 37° C. for 10 min before imaging by confocal microscopy over 40 min. In FIG. 17, asterisks denote the acinar lumen, and the arrowheads indicate the dynamic fusion of early endosomes containing Cy5-Knob-S48I48 nanoparticles internalized from the basolateral membrane. The transcytosis experiments were conducted in primary rabbit lacrimal gland acinar cells (LGACs). LGACs were isolated and maintained in a lamininbased primary culture system and grown on the 35 mm petri dishes for 2 to 3 days. These culture conditions let LGACs reconstitute polarity, establish lumina, and format secretory vesicles. The dishes were pre-coated with commercial matrigel (BD Sciences, Franklin Lakes, N.J.). The dishes were incubated with 1 mL matrigel at 1:50 dilution with ice cold medium at 37° C. for 30 min and the dishes were emptied prior to adding cells. Female New Zealand White rabbits weighing between 1.8 and 2.2 kg were obtained from Irish Farms (Norco, Calif.). Before the experiment, the LGACs were pre-incubated at the second day with baculovirus encoding RFP-Rab5a overnight, which can indicate basolateral and apical early endosomes of rabbit LGACs. Cy5 labelled knob-S48I48 (Cy5 knob-S48I48) was utilized in the transcytosis experiment. 30 µM Cy5-knob-S48I48 diluted in the same medium as cell cultured at 4° C. and then warmed to 37° C. and added into dishes. The cells were cultured with Cv5 knob-ELPs in a 37° C. incubator with 5% CO₂. After 10 minutes incubation, the LGACs were washed with fresh warm medium three times to remove the free Cy5-knob-S48I48 in the medium. Then the cells were incubated with fresh warm medium in a 37° C. incubation chamber. The chamber is mounted on a Zeiss LSM 510 Meta confocal microscope system, which is equipped with argon and red and green He-Ne lasers and mounted on a vibration-free table.

[0113] It was also found that overexpression of Myosin Vb tail suppresses accumulation of knob-S48I48 nanopraticles at the acinar lumen. A mCherry myosin Vb tail, an inhibitor of LGAC transcytosis from basolateral to apical membranes, was found to significantly reduce the transcytosis of knob-S48I48 (FIG. 19). Quantification of these results is shown in FIG. 20A-B. For this experiment, LGACs were pre-infected with adenovirus mCherry-Myosin Vb tail. To obtain the indication of lumen area of LGACs, the cells were also preinfected with Adenovirus EGFP-actin and helper virus at a 37° C. incubator with 5% CO2 overnight. To avoid the clash of fluorescence colours, the knob-S48I48 used in transcytosis inhibition was conjugated with Cy5. The LGACs were grown on 35 mm glass-bottomed dishes for two days. Adenovirus EGFP-actin and helper virus with or without adenovirus mCherry Myosin Vb tail were added into dishes and cultured overnight. After waiting for expression of fluorescence, confocal microscopy was used to make sure adenovirus mCherry-myosin Vb tail and adenovirus EGFP-actin grow in LGACs. On the third day, knob-S48148 conjugated with Cy5 was then mixed with the cold medium at a concentration of 30 μ M, warmed to 37° C. and then added into dishes. After 60 minutes incubation in a 37° C. incubator with 5% CO₂, LGACs were thoroughly rinsed with fresh warm medium then immediately imaged under a Zeiss LSM 510 Meta confocal microscope system, which is equipped with argon and red and green He—Ne lasers and mounted on a vibration-free table. All images were captured under the confocal microscope and processed using ImageJ (NIH, USA).

[0114] FIG. 15 shows a schematic representation showing knob-S48I48 nanoparticles targeted to CAR in LGACs. As depicted in FIG. 15A, Knob-S48I48 reversibly assembles into micelles or disassembles into peptide monomers in response to temperature. Knob-S48I48 contains a full-length Ad5 knob domain at its N-terminus followed by a thrombin cleavage site and the protein polymer S48I48. FIG. 15B depicts multivalent knob-S48I48 nanoparticles associate with the CAR, abundantly expressed on the cellular surface of hepatocytes and LGACs, and followed by internalization via CAR-mediated endocytosis. Endocytosed Knob-S48I48 nanoparticles are transported to early endosomes in LGACs, which is followed by basal-to-apical transport to the acinar lumen, a process called transcytosis. In reconstituted rabbit LGACs, internalized knob-S48I48 nanoparticles are shuttled between basal early endosomes, apical early endosomes, and sorting endosomes.

In Vivo Retention of Knob-S48I48 in the LG of BALB/c Mice.

[0115] Twelve-week-old male BALB/c mice were administered, by intra-lacrimal gland injection, 5 µL of 50 µM rhodamine-labelled S48I48 or rhodamine-labelled knob-S48I48 (red) combined with 50 µg CF-dextran (10 kD, green). After 1 h, mice were euthanized and the glands were retrieved, embedded into the O.C.T. compound (Tissue-Tek), and frozen on dry ice. The frozen tissue blocks were cut into 10 µm thick sections and imaged using confocal fluorescence microscopy. The white arrows indicate endocytosed S48I48 or knob-S48I48 nanoparticles. The bar represents 10 µm. Mouse LGs injected with rhodamine-labelled knob-S48I48 display stronger apical-membrane/luminal accumulation, surface association, and internalization than did untargeted S48I48. This data is shown in FIG. 16. For this experiment, the mice were euthanatized by intraperitoneal injection with 55 mg ketamine and 14 mg xylazine per kilogram of body weight, followed by cervical dislocation. 5 µL of 50 µM rhodamine labelled knob-S48I48 or S48I48 was injected into the lacrimal glands of mice. After 60 minutes, the tear was collected from one eye of mouse by adding Carbachol into the related lacrimal gland. For another gland, it was removed after the tear collection was done at the first eye. After removal, LGs were snap frozen and stored on the dry ice. The frozen glands were cut into 10 µm thick sections and mounted on glass slides. Then the sections were examined with a confocal laser scanning microscope (LSM) at excitation wavelengths of 488 and 534 nm.

Knob-ELP Purification

[0116] A series of ELPs were genetically engineered, expressed in *E. coli*, and purified using the ELP temperature-

dependent phase transition property (Table 1). The purified material was characterized for molecular weight and purity using SDS-PAGE and matrix assisted laser desorption ion mass spectrometry (FIG. 2, Table 1). Three fusion peptides with knob were prepared, knob-S96, knob-S48I48, and knob-196. The ELPs S96 and 196 have a high and low transition temperature respectively; however, they do not form nanoparticles (data not shown). In contrast, the ELP S48I48 was shown to form nanoparticles at physiological temperatures (Table 1). Each of these fusion peptides appears as a major band around 60 kD (FIG. 2), which corresponds to the predicted and observed molecular weights as determined using mass spectrometry (Table 1). Some contaminating E. coli proteins appear to co-purify with both knob-I96 and knob-S96 but not knob-S48I48. Although not essential for this study, the non-chromatographic purification of proteins fused to ELPs represents a powerful advantage of this approach.

Characterization of Knob-ELP

[0117] To determine if the knob-ELP fusion peptides exist in a trimeric form, as they do for native adenovirus as required for appropriate CAR binding, non-denaturing gel electrophoresis was performed (FIG. 3). Knob-S48I48 surprisingly showed three strong bands around 60 kD, 120 kD and 180 kD, which indicated monomer, dimer and trimer forms of knob-ELP. For comparison, a recombinant knob purified using nickel affinity chromatography (without ELP) was also confirmed to form predominantly trimers. The recombinant knob lane indicates several minor bands, with molecular weights slightly lower than knob. These minor bands may come from partial proteolysis of knob. This data suggests that the ELP architecture may influence the native quaternary structure of fused proteins domains, whereby block copolymers that assemble nanoparticles (S48I48) also promote formation of native trimers. So the recombinant knob-ELP has properties similar to those of the native knob.

[0118] To characterize the ELP behavior of the knob fusion peptides, the transition temperatures were identified by optical density (FIG. 4) and the assembly of nanoparticles was confirmed using dynamic light scattering. Knob-596, a monoblock ELP, only exhibits one increase in optical density over a temperature gradient at a temperature well above physiological conditions. Knob-196 also shows a single increase in optical density; however, due to the hydrophobicity of the isoleucine X residue, this fusion peptide phaseseparates near room temperature. In contrast, the diblock ELP Knob-S48I48 displayed two phase transition temperatures, one around 19.5° C. and another around 60° C. Qualitatively, this behavior is similar to S48I48, which has two transition temperatures at 26.5 and 75° C. For knob-S48I48, at temperatures below 19.5° C., the polypeptides are free in solution; however, between 19.5 and about 40° C. the peptides are presumed to form nanoparticles. Above 60° C., the S48 block phase separates, and nanoparticles are not stable. By comparing the critical aggregation temperatures of knob-S48I48 and S48I48, it can be easily observed that the knob domain slightly depresses the nanoparticle assembly temperature (Table 1).

[0119] While optical density is useful to determine the temperature of assembly, dynamic light scattering is necessary to verify the size and formation of stable nanoparticles. Upon heating, both S48I48 and knob-S48I48 self-assemble into nanoparticles and this assembly was shown to be reversible upon cooling (FIG. **5**(A)). When the temperature increased

from 10 to 37° C., both knob-S48I48 and S48I48 transitioned from unimers to nanoparticles, of a radius previously shown to be nanoparticles (see, for e.g., M. R. Dreher, et. al. J Am Chem Soc 130(2) (2008) 687-694). This assembly is reversible, and the nanoparticles were disassembled into unimers when temperature decreased from 37 to 10° C. It was shown by DLS that S48I48 and knob-S48I48 self-assemble into nanoparticles with a diameter consistent with micelles as reported (see, for e.g., M. R. Dreher, et. al. J Am Chem Soc 130(2) (2008) 687-694). At physiological temperature (37° C.), the hydrodynamic radii of S48I48 and knob-S48I48 nanoparticles were 23.7 and 21.7 nm respectively. As observed using dynamic light scattering, the critical nanoparticle temperature (CNT) for knob-ELP is 19.5° C. while ELP without knob is 26.5° C. This downward shift in CNT is consistent with that observed by optical density (FIG. 4). While the addition of knob to the ELP lowers the nanoparticle assembly temperature, it did not change the hydrodynamic radius. The control BSA exhibits a stable size around 4 nm, the same as the unimers of knob-S48I48 and S48I48, because BSA does not have any phase transition behavior. The ANOVA results (FIG. 5(B)) indicate that BSA, S48I48 and knob-S48I48 have similar sizes at 15° C., while the particles size of S48I48 and knob-S48I48 had a significantly larger radii at 37° C. compared with BSA (p<0.01).

[0120] S48I48 protein polymer nanoparticles with and without the Knob domain were viewed by cryo-transmission electron microscopy (TEM) imaging. Cryo-TEM specimens were prepared using FEI Vitrobot (Hillsboro, Oreg.). ELP solutions were kept in an ice bath (4° C.) before processing. A typical procedure involves first loading ~6 uL of the sample on a TEM grid coated with a lacey carbon film (LC325-Cu, Electron Microscopy Sciences). Then, the specimen was carefully blotted under 95% humidity following blotting parameters that were preset depending on the viscosity and concentration of the studied sample. The blotted grid was immediately transferred into liquid ethane, and stored in liquid nitrogen environment. Micrographs were acquired using FEI Tecnai 12 TWIN transmission electron microscope equipped with 16 bit 2Kx2K FEI eagle bottom mount camera (Hillsboro, Oreg.). All images were captured under 100 kV accelerating voltage and processed using ImageJ (NIH, USA). As shown in FIG. 18B, the particles were found to have an average particle size from about 30-40 nm.

Cleavage of Knob-ELP

[0121] To determine if these ELPs can be utilized as a strategy to purify free knob, a thrombin recognition site was incorporated into the construct between knob and the ELP (Table 1). The knob-S48148 construct was incubated with a thrombin cleavage solution, which partially cleaved the fusion peptide, as validated by a band near 20 kD (FIG. 6). Since the thrombin recognition site can be cleaved, there exists the possibility of harvesting recombinant knob from knob-ELP fusion peptides. More importantly, the molecular weight bands resulting from cleavage of knob from ELP further confirm the successful expression of the knob-ELP constructs.

Cellular Uptake

[0122] To determine if knob-mediated internalization is conferred to knob-ELP fusion peptides, live cell uptake experiments were conducted to study the internalization of knob-S48I48 into a hepatocyte cell line. This study was carried out in transformed mouse hepatocytes because of the high expression of CAR, which has been hypothesized to mediate the novel fiber and knob-dependent endocytotic uptake that has been observed. Prior to uptake studies, it was necessary to confirm that the hepatocyte cell line does express CAR (FIG. 7). A western blot comparing CAR expression in three representative and commonly utilized cell types indicated that hepatocyte lysates showed very strong immunoreactivity around 46 kD in mouse hepatocyte cell lysate only, which is the correct molecular weight for CAR. CHO cell lysates showed a slight band and there was no expression detectable in Hela cell lysates.

[0123] Having demonstrated that the hepatocyte cell line expresses CAR, a rhodamine-labeled knob-S48I48 was employed to explore uptake via the CAR pathway. A rhodamine-labeled S48I48 was used as a control for cellsurface binding of ELPs. With 30 minutes incubation at 37° C., there was a significant cellular uptake of knob-S48I48 (FIG. 8). For reference, LysoTracker green was used to stain low pH lysosomes inside the cells. A control sample without ELP shows no signal (absence of red labeling). In contrast, both knob-S48I48 and S48I48 can be clearly seen at the surface of the hepatocytes. Compared with S48I48, knob-S48I48 exhibited much stronger punctate red fluorescence inside hepatocyte cells, and S48148 exhibited slightly more intense fluorescence on the cell surface. Both the intracellular fluorescence of knob-S48I48 and S48I48 that was seen was co-localized with low pH compartments; however, only knob-S48I48 showed an abundant punctate intracellular fluorescence labeling pattern (FIG. 8).

[0124] Having demonstrated an effect of the fused knob domain on the cellular internalization of the fluorescent label, a competitive binding study was used to determine the specificity of uptake for the CAR pathway (FIG. 9). Pre-incubation with anti-mouse CAR antibody reduced the intracellular punctate fluorescence associated with intracellular knob-S48I48 nanoparticles relative to the signal detected in hepatocytes without antibody pre-binding. This result suggests the anti-mouse CAR antibody blocks or alters the internalization of knob-S48I48 into hepatocytes. Incubation with a non-specific antibody similarly did not affect knob-S48I48 uptake (data not shown). In conjunction with the previous experiment, this data supports a model of uptake of knob-ELP nanoparticles via a unique CAR-mediated endocytotic pathway.

[0125] To develop a novel targeted drug carrier, the knob domain of fiber protein from adenovirus 5 was fused with a diblock ELP capable of assembling nanoparticles. Plasmids encoding knob-ELP and ELP were constructed and purified from E. coli. Non-denaturing PAGE demonstrated that knob-ELP fusion peptides form trimeric and dimeric quaternary structures, which is a property of the native knob. Dynamic light scattering indicated that both knob-S48I48 and S48I48 can self-assemble into compact nanoparticles, with hydrodynamic diameters around 40 nm. The critical nanoparticle temperature of S48I48 and knob-S48I48 were 26.5 and 19.5° C. respectively. Cellular uptake experiments indicated that both S48I48 and knob-S48I48 bind a hepatocyte cell line; however, the knob-S48I48 showed more intracellular vesicular uptake, specifically into lysosomal compartments. A competitive binding experiment with anti mouse CAR antibody blocks the internalization of knob-S48I48, suggesting that uptake is mediated by knob-CAR binding and endocytosis. Unlike adenovirus, this simplified fusion peptide lacks many of the capsid proteins responsible for immunogenicity; furthermore, the knob-domain lacks the adenoviral RGD motif that targets integrins. As such, these polypeptide nanoparticles are a potentially useful new class of drug carriers that target a unique uptake mechanism, which is differentially expressed throughout the body.

[0126] It should be understood that although the present invention has been specifically disclosed by preferred embodiments and optional features, modification, improvement and variation of the inventions embodied therein herein disclosed may be resorted to by those skilled in the art, and that such modifications, improvements and variations are considered to be within the scope of this invention such as for example, embodiments described in Appendix A attached hereto. The materials, methods, and examples provided here are representative of preferred embodiments, are exemplary, and are not intended as limitations on the scope of the invention.

[0127] The invention has been described broadly and generically herein. Each of the narrower species and subgeneric groupings falling within the generic disclosure also form part of the invention. This includes the generic description of the invention with a proviso or negative limitation removing any subject matter from the genus, regardless of whether or not the excised material is specifically recited herein.

[0128] In addition, where features or aspects of the invention are described in terms of Markush groups, those skilled in the art will recognize that the invention is also thereby described in terms of any individual member or subgroup of members of the Markush group.

[0129] All publications, patent applications, patents, and other references mentioned herein are expressly incorporated by reference in their entirety, to the same extent as if each were incorporated by reference individually. In case of conflict, the present specification, including definitions, will control.

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		20												

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1. A drug delivery agent comprising an elastin-like peptide (ELP) component and a ligand component, wherein:

(a) the ligand component specifically binds to a CAR and/ or pIgR receptor; and/or

(b) the ligand component is mIgA and/or knob ligand, or a biological equivalent thereof of the mIgA or knob ligand.

2. The drug delivery agent of claim **1**, further comprising a detectable label.

3. The drug delivery agent of claim **1**, further comprising a therapeutic agent.

4. The drug delivery agent of claim 3, wherein the therapeutic agent is an anti-cancer drug.

5. The drug delivery agent of claim **1**, wherein the ELP component comprises a diblock.

6. The drug delivery agent of claim **5**, wherein the ELP component comprises a polypeptide with the sequence $(VPGSG)_{48}(VPGIG)_{48}$ (SEQ ID NO: 12).

7. The drug delivery agent of claim 1, wherein the ELP component comprises a polypeptide with the sequence $(VPGSG)_{96}$ (SEQ ID. NO: 13).

8. The drug delivery agent of claim **1**, wherein the ELP component comprises a polypeptide with the sequence (VP-GIG)₉₆ (SEQ ID. NO: 14).

9. The drug delivery agent of claim **1**, wherein the ligand component is a mIgA ligand.

10. The drug delivery agent of claim **9**, wherein the mIgA ligand comprises a polypeptide having the sequence of SEQ ID. NO: 5 or a biological equivalent thereof.

11. The drug delivery agent of claim 1, wherein the ligand component is a knob ligand.

12. The drug delivery agent of claim **11**, wherein the knob ligand comprises a polypeptide having the sequence of SEQ ID. NO: 4 or a biological equivalent thereof.

13. A polynucleotide encoding the drug delivery agent of claim **1**.

14. A host cell comprising the polynucleotide of claim 13.

15. A composition comprising a carrier and a drug delivery agent of claim **1**.

16. A method for preparing a drug delivery agent, comprising expressing the polynucleotide of claim 13.

17. A method for preparing a drug delivery agent, comprising expressing the polynucleotide of in the host cell of claim 14. **18**. The method of claim **16**, further comprising separating or purifying the drug delivery agent.

19. A method for delivering a drug comprising an elastinlike peptide (ELP) to a cell, comprising contacting the cell with a drug delivery agent of claim **1**, wherein:

- (a) the ligand component specifically binds to a CAR and/ or pIgR receptor; and/or
- (b) the ligand component is mIgA and/or knob ligand, or a biological equivalent thereof of the mIgA or knob ligand.

20. A method for delivering a drug to the luminal area of LGACs by transcytosis, comprising contacting the LGAC with a drug delivery agent of claim **1**, wherein:

- (a) the ligand component specifically binds to a CAR and/ or pIgR receptor; and/or
- (b) the ligand component is mIgA and/or knob ligand, or a biological equivalent thereof of the mIgA or knob ligand.

21. The method of claim **20**, wherein the drug is in contact with the ocular surface of the eye.

22. The method of claim **20**, wherein the drug is released from interstitial to luminal surfaces on a mucosal epithelial cell.

23. The method of claim **19**, wherein the contacting is in vitro or in vivo.

24. The method of claim **19**, wherein the cell is one or more of a mucosal cell, an epithelial cell or a hepatocyte and/or contained within a lacrimal gland or tissue.

25. A method for treating a disease of the lacrimal gland, comprising administering to a patient in need of such treatment a drug delivery agent of claim 1 wherein:

- (a) the ligand component specifically binds to a CAR and/ or pIgR receptor; and/or
- (b) the ligand component is mIgA and/or knob ligand, or a biological equivalent thereof of the mIgA or knob ligand, thereby treating the patient.

26. The method of claim **25**, wherein the disease is cancer or Sjorgren's Syndrome.

27. The method of claim 25, wherein the administration is by inhalation or via injection.

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