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(54) **HANDHELD DEVICE AND METHOD FOR TOMOGRAPHIC OPTOACOUSTIC IMAGING OF AN OBJECT**

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(57) **ABSTRACT**

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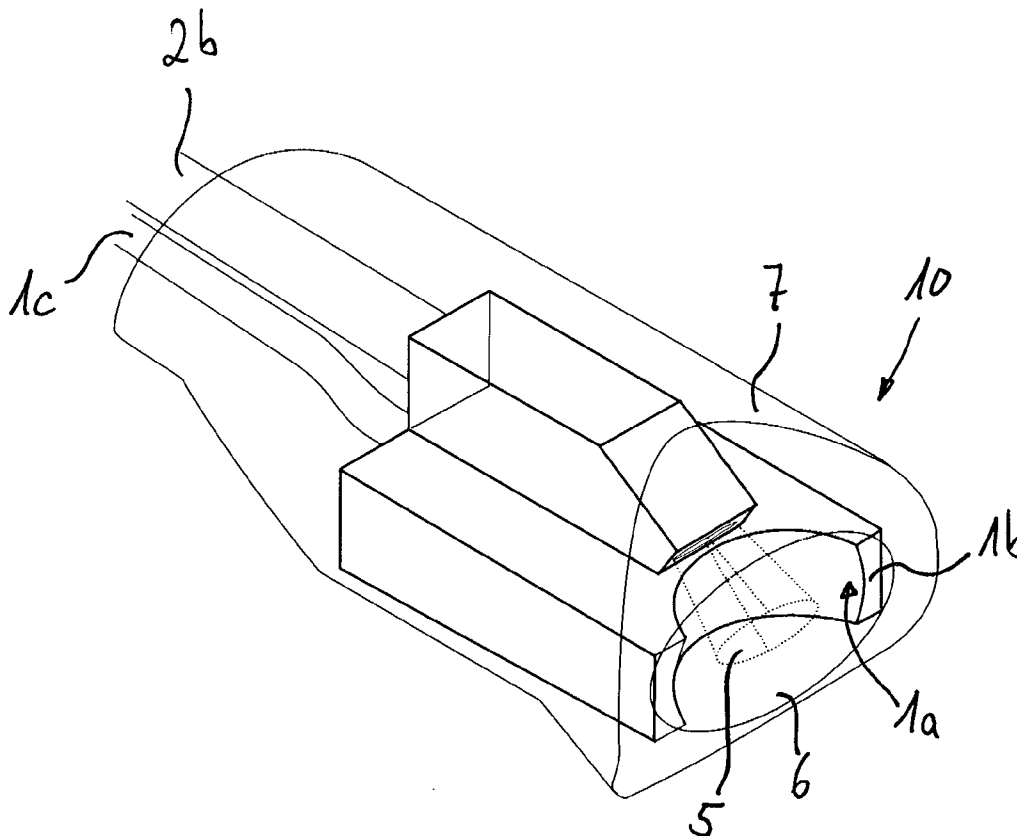
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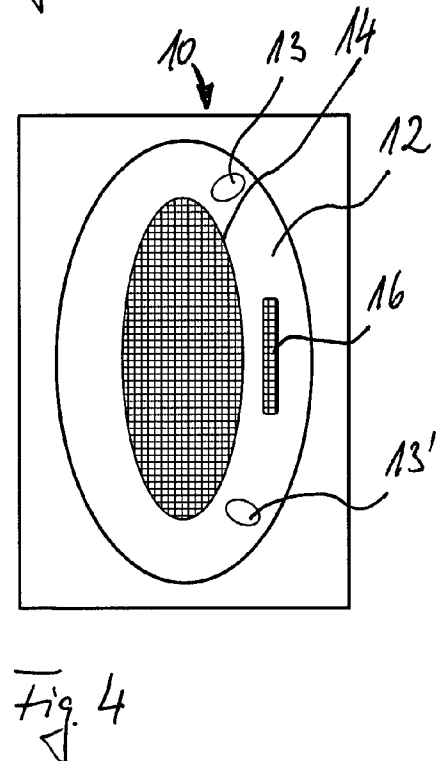
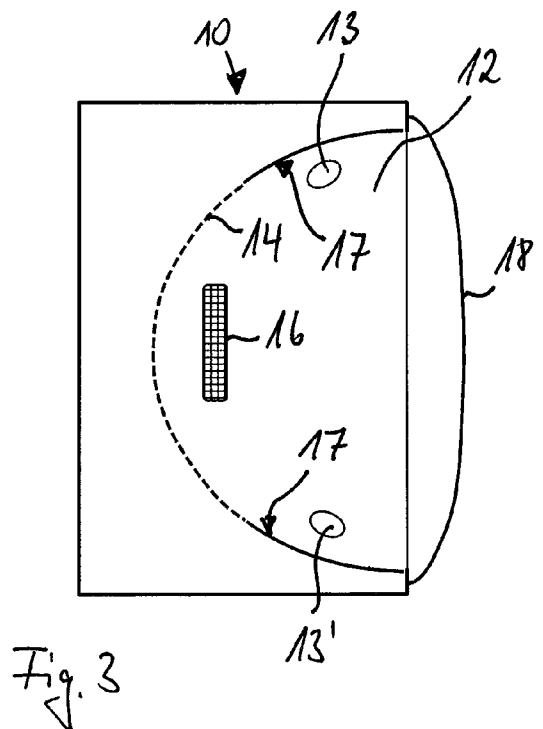
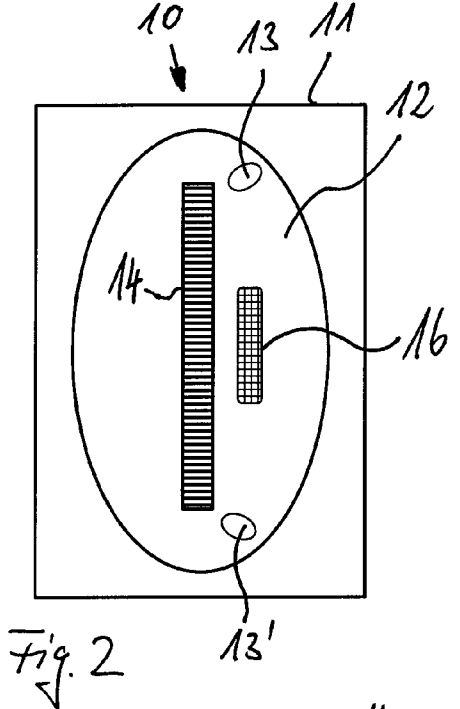
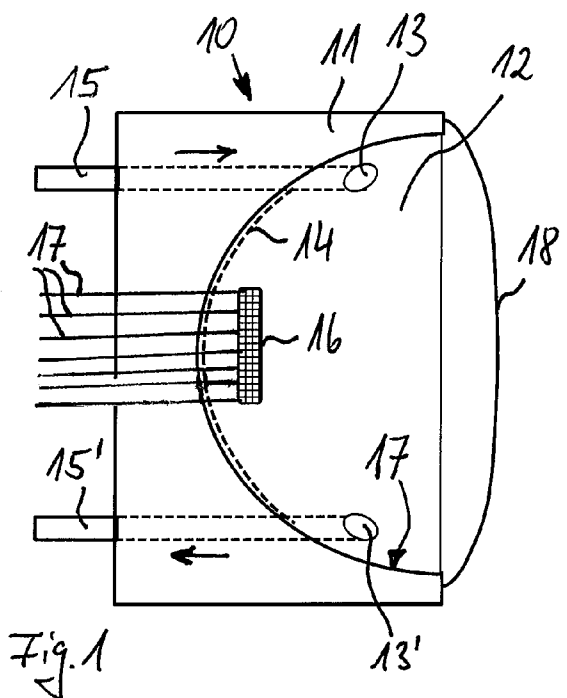
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The present disclosure relates to a handheld device and an according method for optoacoustic imaging of an object, comprising an irradiation unit for irradiating the object with electromagnetic radiation, for example, light, and a detector unit for detecting acoustic, for example, ultrasonic, waves generated in the object upon irradiation with electromagnetic radiation, wherein the detector unit comprises an array of detector elements.

In order to facilitate an acquisition of high-quality tomographic optoacoustic images from different depths within the object at a simple overall design, the handheld device may be provided with a recess, in which the irradiation unit and the array of detector elements are provided, wherein the detector elements are arranged in the recess such that the surface normals of at least a part of the detector elements are directed to a region of interest on or within the object.





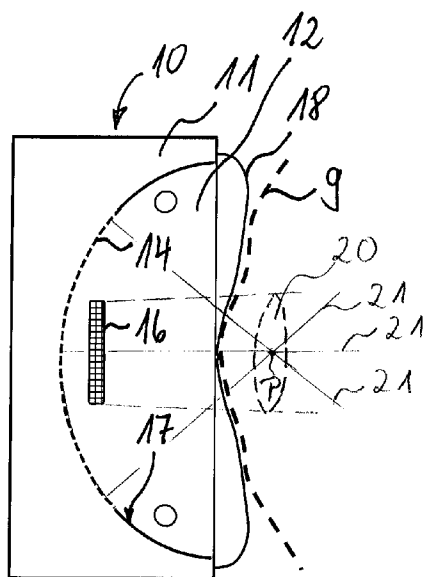


Fig. 5

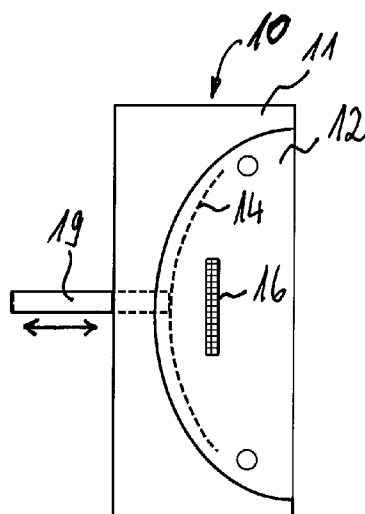


Fig. 6

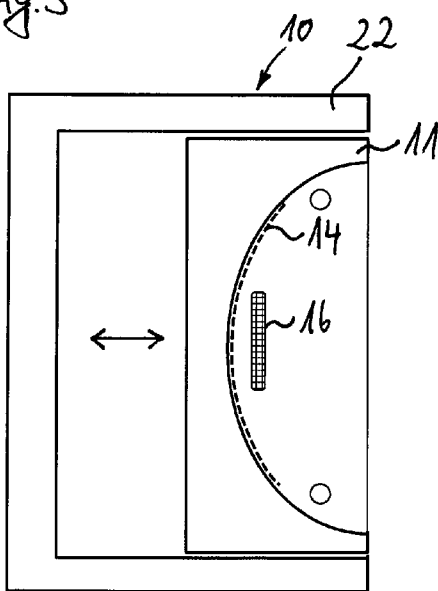


Fig. 7

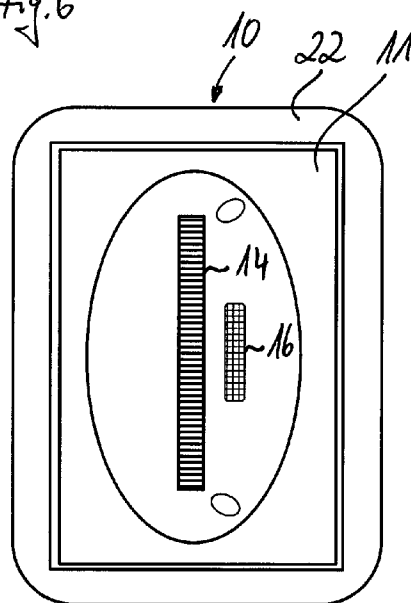
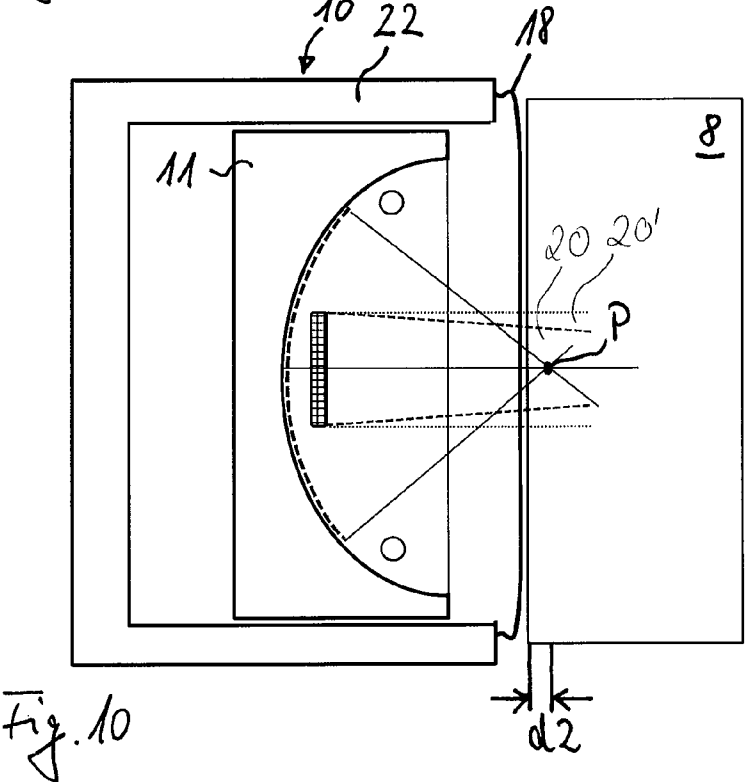
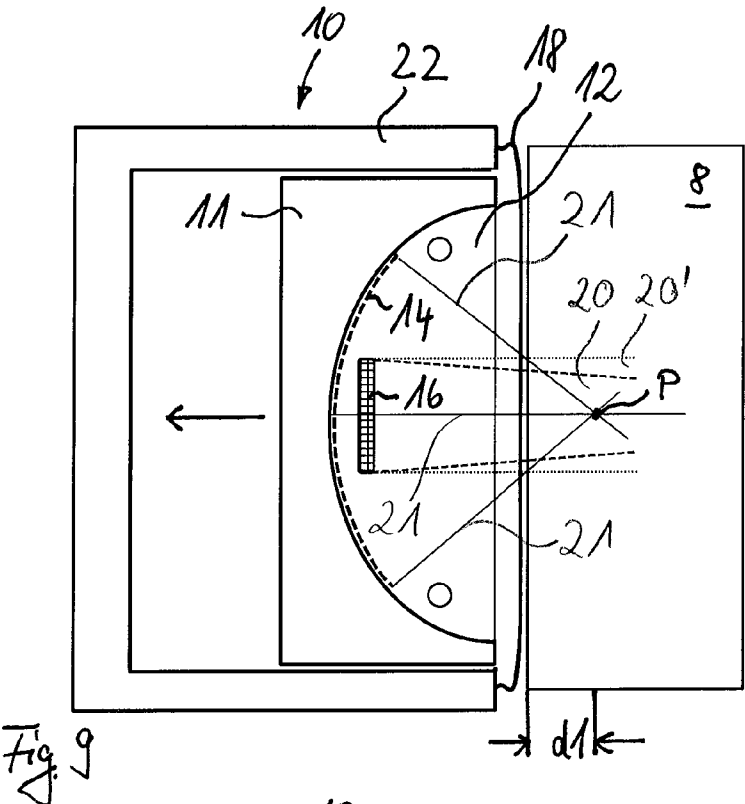


Fig. 8



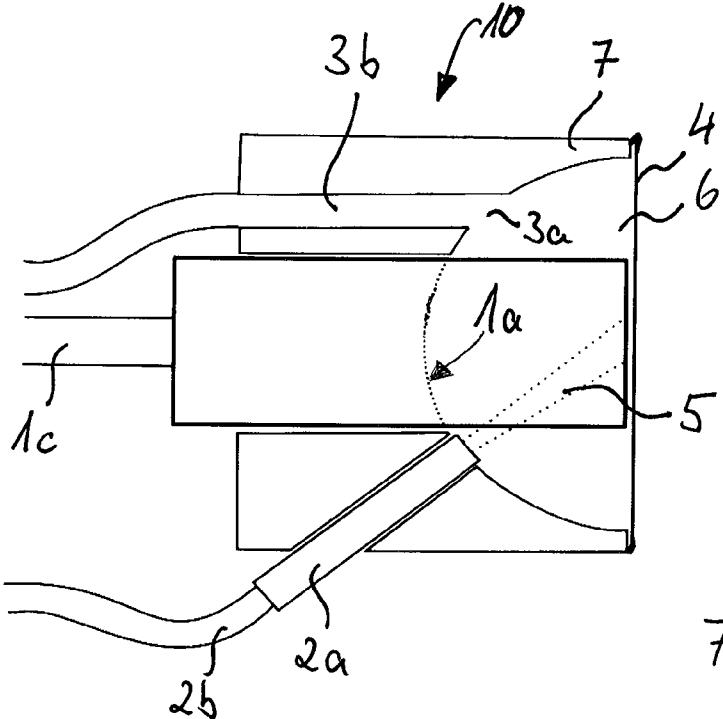


Fig. 11

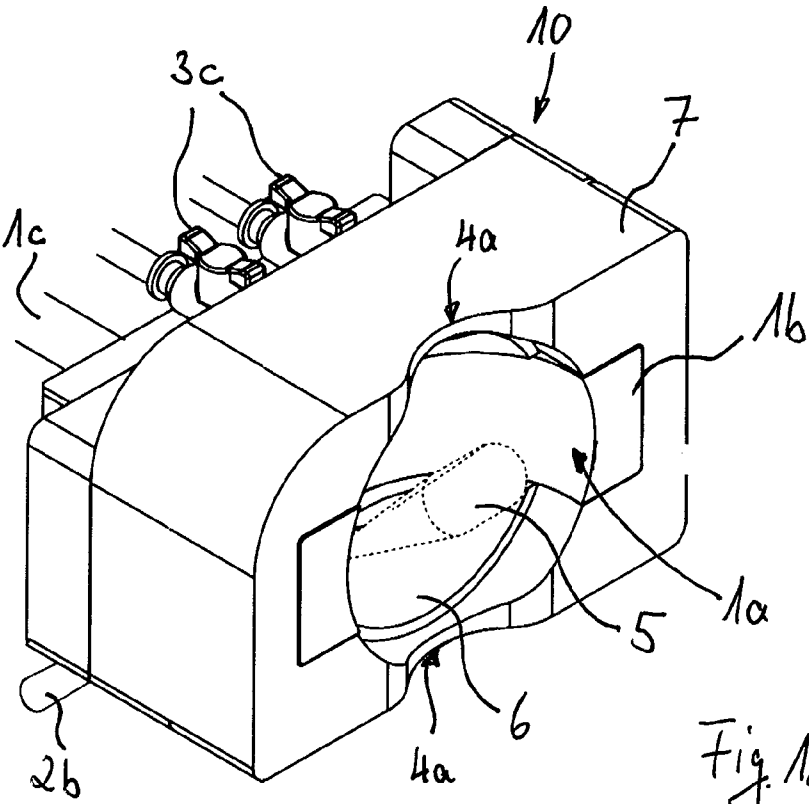
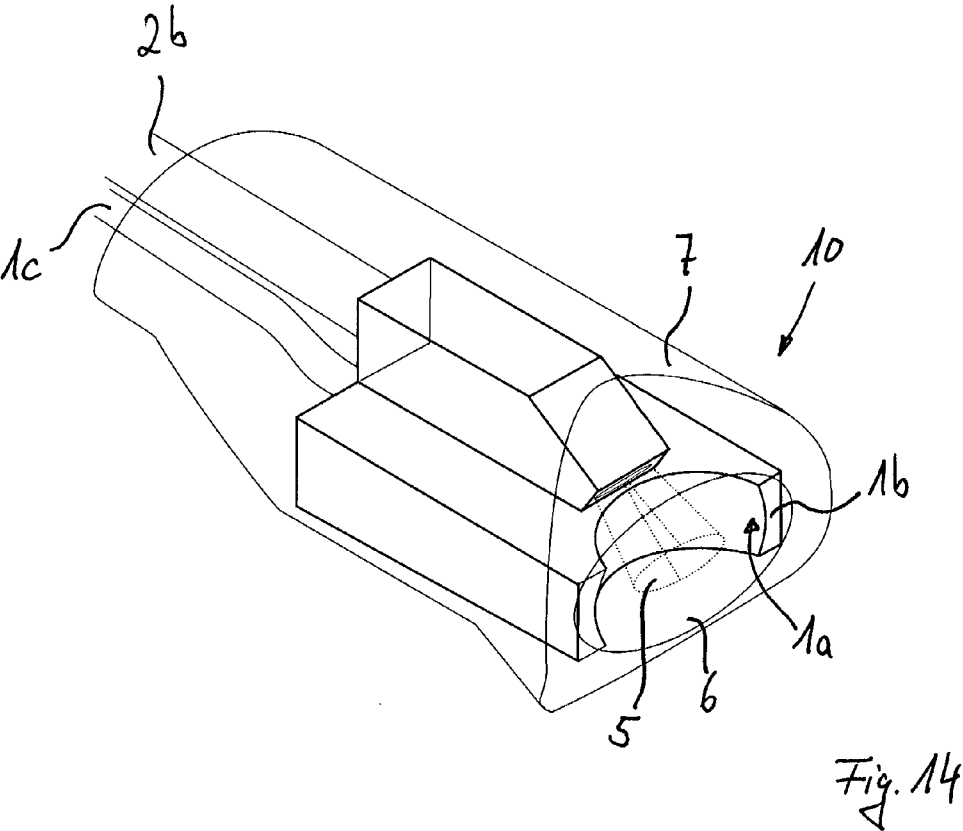
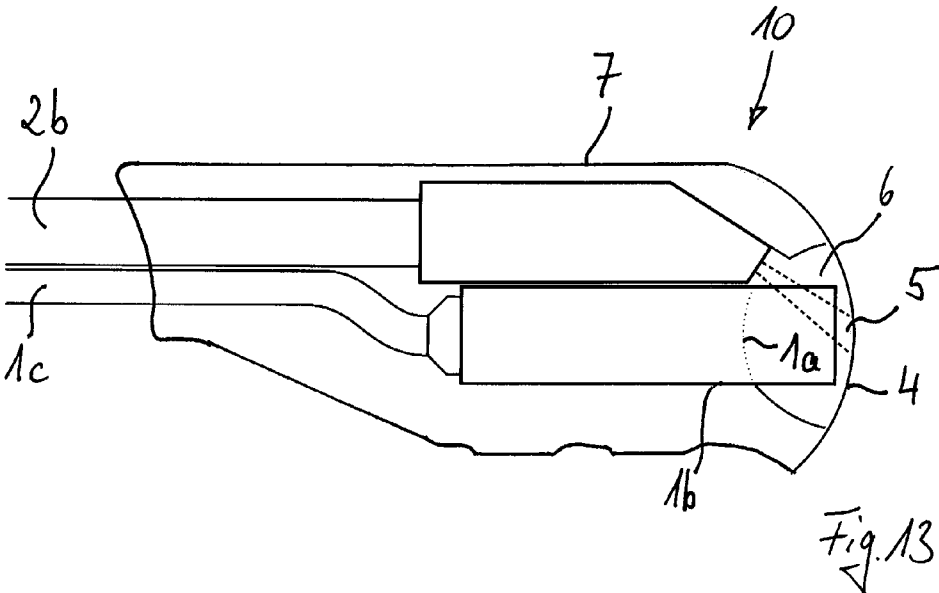


Fig. 12



**HANDHELD DEVICE AND METHOD FOR
TOMOGRAPHIC OPTOACOUSTIC IMAGING
OF AN OBJECT**

RELATED APPLICATIONS

[0001] This application claims priority to U.S. Provisional Application No. 61/735,578 filed on Dec. 11, 2012 and to European Patent Application 12 008 270.6, filed on Dec. 11, 2012, both of which are hereby incorporated by reference in their entireties.

TECHNICAL FIELD

[0002] The present disclosure relates to a handheld device and method for optoacoustic imaging of an object.

BRIEF DESCRIPTION OF THE DRAWINGS

[0003] The embodiments disclosed herein will become more fully apparent from the following description and appended claims, taken in conjunction with the accompanying drawings. The drawings depict only typical embodiments, which embodiments will be described with additional specificity and detail in connection with the drawings in which:

[0004] FIG. 1 shows a cross-sectional side view of a first embodiment of the handheld device according to the present disclosure.

[0005] FIG. 2 shows a front view of the first embodiment of the handheld device.

[0006] FIG. 3 shows a cross-sectional side view of a second embodiment of the handheld device according to the present disclosure.

[0007] FIG. 4 shows a front view of a third embodiment of the handheld device according to the present disclosure.

[0008] FIG. 5 shows a cross-sectional side view of a fourth embodiment of the handheld device according to the present disclosure.

[0009] FIG. 6 shows a cross-sectional side view of a fifth embodiment of the handheld device according to the present disclosure.

[0010] FIG. 7 shows a cross-sectional side view of a sixth embodiment of the handheld device according to the present disclosure.

[0011] FIG. 8 shows a front view of the sixth embodiment of the handheld device according to the present disclosure.

[0012] FIG. 9 shows a cross-sectional side view of the sixth embodiment of the handheld device according to the present disclosure in a first operational status.

[0013] FIG. 10 shows a cross-sectional side view of the sixth embodiment of the handheld device according to the present disclosure in a second operational status.

[0014] FIG. 11 shows a cross-sectional side view of an example of a first prototype of the handheld device according to the present disclosure.

[0015] FIG. 12 shows a perspective view of the example of a first prototype of the handheld device according to the present disclosure.

[0016] FIG. 13 shows a cross-sectional side view of an example of a second prototype of the handheld device according to the present disclosure.

[0017] FIG. 14 shows a perspective view of the example of a second prototype of the handheld device according to the present disclosure.

DETAILED DESCRIPTION

[0018] Optoacoustic imaging is based on the photoacoustic effect, according to which ultrasonic waves are generated due to an absorption of electromagnetic radiation by an object, e.g. a biological tissue, and a subsequent thermoelastic expansion of the object.

[0019] Optoacoustic imaging of biological tissues provides a unique combination of high spatial resolution and rich contrast based on spectrally-dependent absorption of light. Techniques like multispectral optoacoustic tomography (MSOT) are therefore able to simultaneously render images of anatomical, functional and molecular contrast by exciting tissues at several optical wavelengths, thereby enabling highly promising applications in molecular imaging and diagnostics, drug development and treatment monitoring.

[0020] United States Patent Application Publication No. 2008/0071172 A1 discloses an apparatus combining pulse-echo ultrasound imaging with optoacoustic imaging comprising a conventional linear ultrasound probe and an attachment thereto, wherein said attachment comprises an illumination assembly used to excite optoacoustic signals in the object and, optionally, an additional set of ultrasound detection elements arranged for detection of optoacoustically-induced signals. While the general goal of said apparatus is a combination of pulse-echo ultrasound and optoacoustic imaging, it cannot be ensured that high-quality optoacoustic images, in particular with a high signal-to-noise ratio, quantification and spatial resolution, are obtained from regions of interest on or within the object.

[0021] In some embodiments the present disclosure relates to providing a handheld device and a corresponding method allowing for an improved and reliable optoacoustic imaging of an object, for example, allowing for an acquisition of high-quality optoacoustic images, exhibiting, for example, high signal-to-noise ratio, from regions of interest on or within the object in a simple and reliable manner.

[0022] An embodiment of the handheld device for optoacoustic imaging of an object according to the present disclosure comprises an irradiation unit for irradiating the object with electromagnetic radiation, for example, light, and a detector unit for detecting acoustic waves, for example ultrasonic waves, which are generated in the object upon irradiation with electromagnetic radiation, wherein the detector unit comprises an array of detector elements. The handheld device further comprises a recess in which the irradiation unit and the array of detector elements are provided, wherein the detector elements are arranged in the recess, such that the surface normal of at least a part of the detector elements is directed to a region of interest on or within the object.

[0023] In an embodiment of a method for optoacoustic imaging of an object according to the present disclosure the object is irradiated with electromagnetic radiation, for example, light, by means of an irradiation unit and acoustic waves, for example, ultrasonic waves, are generated in the object upon irradiation with electromagnetic radiation and detected by means of an array of detector elements, wherein the irradiation unit and the array of detector elements are provided in a recess, wherein the detector elements are arranged in the recess such that the surface normal of at least a part of the detector elements is directed to a region of interest on or within the object.

[0024] The term “handheld device” within the meaning of the present disclosure relates to any optoacoustic imaging device which is adapted for being seized and held by clasp-

with fingers and/or a hand in order to position the handheld device onto an object under investigation and/or to move the handheld device by hand relative to the object under investigation, for example, by positioning it onto or moving it along an exterior surface of the object, e.g. the skin of a patient. The term “handheld device” also relates to optoacoustic imaging devices in which only a component thereof, such as a handheld probe comprising the irradiation unit and/or the detector unit, is configured for being seized and held by claspings with fingers and/or a hand for same purposes. In some embodiments, the size of a handheld device or a respective handheld probe within the meaning of the present disclosure is less than 15 cm in width and/or depth and/or height. The term “handheld device” further relates to any optoacoustic imaging device which is designed for acquiring tomographic optoacoustic images at arbitrary orientations of the handheld device or handheld probe, respectively. For example, when acquiring images from the object, the orientation of the handheld device or probe can vary from a vertical up to a vertical down orientation including all orientations in between, for example, a horizontal orientation.

[0025] The present disclosure is based on the approach to provide a handheld optoacoustic imaging device with a recess in which both an irradiation unit and a detector unit are arranged, wherein the detector unit may comprise a curved array of ultrasound transducers, i.e. detector elements, and wherein at least one of the following elements or parameters of the handheld device are designed or chosen such that high-quality optoacoustic images from the region of interest on or within the object can be acquired in a simple and reliable manner: the shape of the recess, the positioning of the recess relative to the object, the arrangement of the irradiation unit within the recess, the shape of the array of detector elements, the arrangement of the array of detector elements within the recess and/or the direction of a surface normal of at least a part of the detector elements. In some instances, the direction of the surface normal of the detector elements, which corresponds to the direction along which the detector elements have the highest sensitivity for ultrasound waves, is directed to the region of interest on or within the object. In some embodiments, the surface normal of the detector elements intersect in an intersection point or in an intersection region which is located in the region of interest from which images are to be acquired. Moreover, the irradiation unit is arranged in the recess and designed such that a region on or within the object which is irradiated with the electromagnetic radiation coincides or overlaps with the region of interest and/or the intersection point or intersection region of the normal of the detector elements. By this means, it can be ensured that images with an improved signal-to-noise-ratio can be acquired from different depths within the object.

[0026] The present disclosure thus relates to acquiring high-quality optoacoustic images of an object by means of a handheld device of an overall simple yet efficient design.

[0027] The present disclosure further relates to a handheld device for sectional optoacoustic imaging of soft tissues for clinical imaging applications. The device uses the principles of multispectral optoacoustic tomography, i.e. illumination of the imaged object with light, in some instances, at multiple wavelengths, with a subsequent detection of the generated high frequency ultrasonic (photoacoustic) responses. In some embodiments, an imaging device employing the photoacoustic effect comprises a laser and a detection system. The laser radiation is delivered into the imaged region while the

absorbed light is converted into heat and creates thermoelastic expansion, i.e. a propagating acoustic (ultrasonic) wave. Detection of such acoustic signals allows for spatial localization of absorbers. If detection is performed by multiple detectors arranged around the imaged object, a tomographic reconstruction of the scanned object becomes possible. Such an imaging modality thus delivers images of tissue anatomy based on light absorption coefficients. In contrast to pure ultrasound scanners, whose contrast capability derives from acoustic properties of the matter, optoacoustic modalities provide information about the optical absorption of a tissue depending on the color of the light excitation. A sequential exposure of the tissue to a wavelength-variable source allows for spectral decomposition of the reconstructed images. This mode of operation extends the palette of applications to spatially-resolved imaging of functional tissue parameters, such as blood oxygenation, as well as quantification of intrinsic biomarkers and extrinsically-administered contrast agents.

[0028] The light penetrating the tissue is affected by scattering and absorption. These effects may strongly affect photoacoustic signal generation and, thus, a suitable system for the delivery of the excitation light may be a part of an optoacoustic imaging system. At the same time, the imaging apparatus may be configured to provide acoustic coupling for efficient and sensitive ultrasound detection.

[0029] The present disclosure relates to a novel design of a handheld tomographic optoacoustic probe as well as a corresponding method for tomographic optoacoustic imaging. Certain embodiments are designed in a way that the region of illumination overlaps with the ultrasound-detection field of view resulting in better contrast of the image. In addition, in some embodiments, a liquid chamber is provided for optical and acoustic coupling, while suppressing out-of-imaging-plane waves that are the main cause of image artifacts.

[0030] In some embodiments, the handheld device comprises a container in which the recess together with the irradiation unit and the detector unit are provided and a carrier on which or in which the container is moveably mounted such that, for example, while images are acquired from the object, the container can be moved towards the object and/or away from the object, wherein the location of the region of interest, for example, the intersection point or intersection region of the normal of the detector elements, and/or the irradiated region of the object can be changed. By this means, high-quality optoacoustic tomographic images can be acquired from different regions at different depths on or within the object without the requirement of moving the handheld device itself relative to the object. The latter facilitates the handling of the handheld device while the image capturing process considerably.

[0031] In a further embodiment, the recess is provided, and may be sealed, with a cover element such that the recess together with the cover element constitute a cavity and wherein the cavity accommodates a coupling medium, for example, water. In this embodiment, the recess forms a first part and the cover element forms a second part of a closed cavity, which is filled with the coupling medium, having an acoustic impedance such that reflections of acoustic waves emanating from the object, passing through the cover element and incident upon the detector elements are minimized or eliminated. It is also contemplated that the coupling medium may have a refractive index such that reflections of electromagnetic radiation emerging from the irradiation unit into the recess, passing through the cover element and entering into

the object are minimized or eliminated. In some instances, the acoustic impedance and/or the refractive index of the coupling medium is identical or close to the acoustic impedance and/or the refractive index of the object. In such embodiments, the recess in which the irradiation unit and the detector unit are integrated also constitutes a container for accommodating the coupling medium. This embodiment represents a very compact design of the handheld device which is, therefore, of particular advantage in handheld applications in which high-quality optoacoustic images are obtained.

[0032] In some embodiments, the region of interest of the object, such as the intersection point or intersection region of the normal of the detector elements, is located around the cover element or beyond the cover element. Alternatively or additionally, the irradiated region of the object is located around the cover element or beyond the cover element. By means of this embodiment, high-quality tomographic images from the surface of the object or within the object can be obtained in a simple and reliable way.

[0033] In some instances, the cover element is arranged and/or designed such that at least a section of the cover element comes into contact with the object while images are acquired from the object. That is, when optoacoustic images are acquired, the handheld device is placed onto the object under investigation such that the cover element comes into contact with the surface of the object under investigation.

[0034] In some embodiments, the cover element is a mechanically flexible element, such as a membrane or a film. Due to its flexibility, the shape of the cover element can be easily adapted to the surface of the object under investigation. By this means, a close contact between the distal end of the handheld device and the object can be achieved which ensures a good optical and acoustical coupling between the irradiation unit and detector unit on the one hand and the object on the other hand. This further ensures the acquisition of high-quality images.

[0035] In some embodiments, at least a section of the cover element has a convex shape, such as a cushion-like shape. In some embodiments when the cover element is mechanically flexible and the cavity is filled with the coupling medium, the cover element exhibits a cushion-like behavior by means of which it easily adapts to various surface topologies of objects under investigation in a particularly reliable way. The above-mentioned advantages apply according.

[0036] According to a further embodiment of the present disclosure, at least one conveyance unit is provided for conveying the coupling medium into and/or out of the recess. The conveyance unit may comprise tubes or pipes which are connected over a pump to a reservoir, which is filled with the coupling medium. In some instances, by continuously circulating the coupling medium, i.e. removing medium from the recess and conveying medium from the reservoir into the recess, gas bubbles evolving in the coupling medium in the recess are efficiently removed therefrom. As a result, adverse effects of gas bubbles on the detection of the acoustic waves, such as acoustic scattering, attenuation and reflections, can be efficiently avoided so that a high image quality can be ensured in a simple and efficient way.

[0037] In a further embodiment, the array of detector elements is a curved array of detector elements or a two-dimensional array of detector elements. In the case of a curved array, the detector elements are arranged along an arc or bow, such as in a circular arc, wherein the surface normal of the detector elements of the array intersect in the center of the curvature of

the arc or circle, respectively. By this means, the detector elements efficiently collect acoustic waves from a region upon or within the object, which is located around the center of the curvature. If, for example, the detector elements are arranged along a curved two-dimensional surface which is spherically shaped, such as a concave surface and/or a calotte, the detector elements collect acoustic waves from a region of the object located around the center of a sphere.

[0038] In some embodiments, the recess comprises and/or is constituted by at least one curved, for example, a concave, surface. Additionally or alternatively, the curved array of detector elements is provided at the curved surface of the recess and/or constitutes a section of the curved surface of the recess. Additionally or alternatively, the irradiation unit is provided at the curved surface of the recess. By one or more of these measures, a very compact design of the handheld device is achieved without negatively affecting the quality of optoacoustic images acquired with the device.

[0039] According to a further embodiment, at least a section of the curved surface of the recess is designed, for example, shaped, such that a reflection of acoustic waves incident on the curved surface of the recess towards the array of detector elements is reduced or avoided. By this means it is ensured that only direct acoustic waves directly emanating from the object are detected by the detector elements, whereas a detection of indirect acoustic waves which are reflected at the surface of the recess is efficiently reduced or eliminated.

[0040] In further embodiments of the present disclosure, the shape, for example, the curvature, and/or the size and/or the angular coverage of the array of detector elements depend on the size of the object and/or the region of interest of the object. In this manner it is ensured that for any kind of objects, e.g. large areas of the human body or small tissue specimen, acoustic waves are detected by the array of detector elements in the broadest possible solid angle range around the imaged region of the object. By means of the shape of the array of detector elements the orientation of individual detector elements toward the imaged region can be optimized and/or the distance of the detector elements from said region can be minimized in order to increase the detected optoacoustic responses, i.e. the acoustic waves, of the detector elements and minimize effects of acoustic refractions and surface mismatches.

[0041] It will be readily understood by one of skill in the art having the benefit of this disclosure that the components of the embodiments as generally described and illustrated in the Figures herein could be arranged and designed in a wide variety of different configurations. Thus, the following more detailed description of various embodiments, as represented in the Figures, is not intended to limit the scope of the disclosure, but is merely representative of various embodiments. While the various aspects of the embodiments are presented in drawings, the drawings are not necessarily drawn to scale unless specifically indicated.

[0042] FIG. 1 shows a cross-sectional side view of a first embodiment of the handheld device 10 according to the present disclosure. The handheld device 10 comprises a container 11 in which a recess 12 having a surface 17 is provided. The container 11 is made of a metal in some embodiments. The recess 12 in the container 11 has the shape of a part of a sphere, such as of a calotte, or a part of an ellipsoid.

[0043] In the recess 12 an array of ultrasound detector elements 14 is provided. In the given example, the detector

elements of the array 14 are arranged on or along the surface 17 of the recess 12. As shown in the figure, the array is provided in a region of the bottom of the recess 12. In some instances, the array 14 of detector elements is a linear array.

[0044] The recess 12 has an aperture in which an end face of a fiber bundle 16 is provided. The end face of the fiber bundle 16 comprises a plurality of end faces of individual fibers 17 of the fiber bundle, whereof only a few fibers 17 are indicated in FIG. 1. The fibers 17 are connected with a light source (not shown), such as a laser.

[0045] In the recess 12 two openings 13 and 13' are provided through which a liquid, such as an acoustic and/or optical coupling medium, can be filled into the recess 12 and/or sucked off the recess 12. The liquid is conveyed to and from the openings 13 and 13', respectively, by means of conveyance means 15 and 15', like tubes or channels. In some embodiments, the coupling medium is conveyed from a reservoir (not shown) via a first conveyance means 15 (see arrow rightwards) and a first opening 13 into the recess 12, while coupling medium accommodated in the recess 12 is simultaneously sucked off the recess 12 via a second opening 13' and a second conveyance means 15' (see arrow leftwards) and, in some instances, conveyed back to the reservoir. In this manner, a continuous circulation of coupling medium is achieved by means of which bubbles generated in the coupling medium accommodated in the recess 12 can be efficiently removed.

[0046] At the open end of the recess 12 the container 11 is provided with a flexible membrane 18 such that the recess 12 is sealed in a gas-tight and/or liquid-tight manner and a closed cavity accommodating the coupling medium is obtained. Due to the coupling medium filling of the cavity and the flexibility of the membrane 18 the latter exhibits a slightly curved, for example, convex, shape as indicated in FIG. 1.

[0047] FIG. 2 shows a front view of the first embodiment of the handheld device 10 according to the present disclosure. For sake of clarity, the membrane 18 (see FIG. 1) is not shown in FIG. 2.

[0048] As shown by the oval shape of the recess 12 in this view together with the circular shape in the side view of FIG. 1, the recess 12 of the first embodiment has the form of a part of an ellipse or an ellipse-like body. As also shown in FIG. 2, the array 14 of detector elements is a linear array of, e.g. 128 or 256, individual detector elements arrayed along a line.

[0049] The end face of the fiber bundle 16 is arranged in the recess 12 with a certain lateral offset from the array 14 of detector elements. Same applies for the openings 13 and 13' through which coupling medium is guided to and from the recess 12, respectively.

[0050] FIG. 3 shows a cross-sectional side view of a second embodiment of the handheld device 10 according to the present disclosure. Unlike the first embodiment shown in FIGS. 1 and 2, the detector elements of the array 14 are not arranged on the surface 17 of the recess 12, but the array 14 of detector elements forms a part of the surface 17 of the recess 12. This is achieved in some embodiments, by providing the surface 17 of the recess 12 with a further recess in which the array 14 is integrated. In some instances, the surface of the plurality of detector elements of the array 14 aligns with the surface 17 of the recess 12, as indicated in FIG. 3. In this embodiment, the array 14 constitutes a part of the surface 17 of the recess 12.

[0051] With respect to the end face of the fiber bundle 16, the openings 13 and 13', the conveyance means (not shown),

as well as the membrane 18 and the coupling medium filling of the cavity, the elucidations given with respect to FIGS. 1 and 2 apply accordingly.

[0052] FIG. 4 shows a front view of a third embodiment of the handheld device 10 according to the present disclosure. In this embodiment, the array 14 of detector elements is a curved two-dimensional array of detector elements, wherein a plurality of detector elements are arranged along a curved surface the contour thereof may have the form of, e.g., an ellipse.

[0053] Like in the first and second embodiment shown in FIGS. 1 to 3, the detector elements of the two-dimensional array in the third embodiment shown in FIG. 4 can be arranged on or along the surface 17 of the recess 12 or can be integrated into or constitute a part of the surface 17 of the recess 12. Apart from that, the elucidations given with respect to FIGS. 1 to 3 apply accordingly.

[0054] FIG. 5 shows a cross-sectional side view of a fourth embodiment of the handheld device 10 according to the present disclosure.

[0055] Also in this embodiment, the array 14 of detector elements is arranged in a region of the bottom of and integrated in the surface 17 of the recess 12 in the container 11, wherein the detector elements of the array 14 are in alignment with the run of the surface 17. The depth of the recess 12 in this embodiment is less than the depth of the recesses of the embodiments shown in FIGS. 1 and 3. Apart from that, the elucidations given in relation to FIGS. 1 to 4 apply accordingly.

[0056] The distal end of the handheld device 10 is in contact with a curved surface 9 of an object under investigation. Because of the mechanical flexibility of the membrane 18, which seals the coupling medium-filled recess 12 of the container 11, the membrane 18 easily adapts itself to the shape of the surface 9 of the object. In this way, it is ensured that the handheld device 10 can be positioned on the object under investigation very stably.

[0057] In some embodiments, the sensitivity of the detector elements of the array 14 for ultrasonic waves is focused to a focus point or a focus region which defines the region of interest from which images of the object are acquired. In the given embodiment, the surface normals 21 of each of the detector elements of the array 14 intersect at an intersection point P. For sake of clarity, only three surface normals 21 are shown in the present figure. It is not necessary that all the surface normals 21 have to intersect at an intersection point P in order to define a region of interest within the object. The surface normals 21 of the detector elements of the array may simply be directed to the region of interest in embodiments within the scope of this disclosure.

[0058] In the shown embodiment, the light emitted from the end face of the fiber bundle 16 has the form of a flat cone 20 the boundaries of which are indicated by dashed lines. In some embodiments, the intersection point P of the surface normals 21 of the detector elements of the array 14 comes within the light cone 20 emerging from the light bundle 16 and incident onto the surface 9 of the object.

[0059] As already mentioned above, by means of the flexible membrane 18 the handheld device 10 can be positioned on the object under investigation very stably. Moreover, the membrane 18 allows for easily moving the handheld device 10 relative to the object, i.e. along the surface 9 of the object and/or towards or away from the surface 9 of the object. Therefore, by means of moving the handheld device 10 along the surface 9 of the object and/or towards or away from the

surface **9** of the object, the region of interest on or within the object, which is defined by the direction of the surface normals **21** of the detector elements and/or the cone **20** of the light emitted from the light bundle **16**, can be defined easily and reliably.

[0060] Additionally or alternatively, the region of interest on or within the object, from which images of the object shall be acquired, can be defined by varying the distance of the array **14** of detector elements and/or the distance from the end face of the fiber bundle **16** from the surface **9** of the object under investigation.

[0061] FIG. **6** shows a cross-sectional side view of a fifth embodiment of the handheld device **10** according to the present disclosure by means of which the region of interest on or within the object can be varied by changing the distance of the array **14** of detector elements from the object. For this purpose, the array **14** is moveably mounted in the recess **12**. In some instances, a moving mechanism **19** is provided by means of which the array **14** can be moved back and forth, i.e. away from or towards the object (see double-arrow). In the representation of FIG. **6**, the moving mechanism **19** is schematically represented by a single rod which is moveably mounted in a guide provided in the container **11**. Of course, further and even more complex moving mechanisms **19** can be provided for realizing a back-and-forth movement of the array **14**.

[0062] Additionally or alternatively, also the end face of the fiber bundle **16** can be moveably mounted in the recess **12** such that the cone **20** of the light emerging from the end face of the fiber bundle **16** can be moved towards and/or away from the object.

[0063] Regarding the remaining components and features of the handheld device **10**, for example, with respect to the membrane **18**, the conveyance means, the intersection point **P** and the light cone **20**, the elucidations given above with respect to the embodiments given in FIGS. **1** to **5** apply accordingly.

[0064] FIG. **7** shows a cross-sectional side view of a sixth embodiment of the handheld device **10** according to the present disclosure by means of which the region of interest on or within the object can be varied by changing the distance of the array **14** of detector elements and the end face of the fiber bundle **16** from the object. For this purpose, a carrier **22** is provided in which the container **11** is moveably, for example, slidably, mounted such that it can be moved by a respective moving mechanism (not shown) back and forth (see double-arrow). FIG. **8** shows a corresponding front view of the sixth embodiment of the present disclosure. As obvious for the figure, the carrier **22** surrounds the container **11** such that the handheld device **10** can be easily grasped by the hand of a person without limiting the back-and-forth movement of the container **11**. Regarding the remaining components and features of the handheld device **10**, for example, with respect to the membrane **18**, the conveyance means, the intersection point **P** and the light cone **20**, the elucidations given above with respect to the embodiments given in FIGS. **1** to **6** apply accordingly.

[0065] FIG. **9** shows a cross-sectional side view of the sixth embodiment of the handheld device **10** according to the present disclosure in a first operational status in which the movably mounted container **11** is in a first position with respect to the carrier **22** and the object **8**. According to the embodiment shown in FIG. **5**, the surface normals **21** of the detector elements of the linear of two-dimensional array **14**

intersect at an intersection point **P** located beyond membrane **18** at a first depth **d1** within the object **8**. The intersection point **P** is located in a center of curvature of the array **14** of the detector elements. If, e.g., the array **14** is spherically shaped then the intersection point **P** is located in the center of a sphere.

[0066] Moreover, the intersection point **P** lies within the illuminated area of the object **8**, i.e. within the cone **20** of the light beam emerging from the end face of the fiber bundle **16**. In the example shown, the cone **20** is a slightly converging light beam. Alternatively, any other kind of light beams is possible, e.g. a pencil-like parallel light beam **20'** or a slightly diverging cone like the one shown in FIG. **5**.

[0067] By moving the container **11** away (see arrow) from the object **8**, the intersection point **P** as well as the cone **20** or **20'**, respectively, are moved within the object **8** to a second depth **d2** within the object **8**, wherein the second depth **d2** is smaller than the first depth **d1**. This is illustrated by means of FIG. **10** which shows a cross-sectional side view of the sixth embodiment of the handheld device **10** according to the present disclosure in a second operational status. Regarding the remaining components and features of this embodiment of the handheld device **10**, the elucidations given above with respect to the embodiments given in FIGS. **1** to **9** apply accordingly.

[0068] In the embodiment shown in FIGS. **9** and **10**, the membrane **18** is provided at the carrier **22** and forms together with the recess **12** a cavity which is filled with coupling medium. Alternatively, like in the embodiments shown in FIGS. **1**, **3** and **5**, the membrane **18** can be affixed to the container **11** so that it moves together with the container **11** towards and/or away from the object **8**.

[0069] FIG. **11** shows a cross-sectional side view of an example of a first prototype of the handheld device **10** according to the present disclosure. FIG. **12** shows a perspective view of the example of a first prototype of the handheld device **10** according to the present disclosure.

[0070] The device **10** comprises a high frequency cylindrically focused tomographic ultrasound transducer array **1a** to **1c**, fiber bundles **2a** and **2b**, a liquid-filling mechanism **3a** to **3c**, a coupling membrane **4**, an encasement **7** and a recess **6** provided in the encasement **7**.

[0071] The transducer array comprises a piezo-composite sensing surface **1a**, a casing **1b** for the transducer array and electric cables **1c** connected with the individual transducers of the transducer array. The sensing surface **1a** of the transducer array is provided in the recess **6** of the encasement **7**. Each of the fiber bundles comprises a metal ferrule **2a** and a fiber cable **2b** containing multiple multi-mode fibers. The liquid-filling mechanism comprises channel outputs **3a** of the chamber, wherein a first output is provided for delivering the liquid to the chamber and a second output is provided for removing the remaining gas, two channels **3b** going through the chamber enclosure, and two pipe connectors and valves **3c**.

[0072] Electromagnetic radiation, for example, light, emerges from the distal end of each of the fiber cables **2b** in the form of a slightly flattened cone **5** which is running coaxially with the metal ferrule **2a**. The cone **5** represents the light beam illuminating a tissue surface (not shown).

[0073] The device **10** is especially designed for a convenient access to different parts of the human body, most of them having a convex shape, e.g. especially limbs, torso or a neck.

[0074] The ultrasound array *1a* to *1c* comprising a plurality of cylindrically-focused detectors is assembled together with four optical waveguides *2a* and *2b* using the encasement *7* which is made of metal or plastics in some embodiments. The front face of the encasement *7*, i.e. the distal end of the handheld device *10*, is provided with a recess *6* in order to form a chamber which is filled with a liquid, for example, an acoustical and/or optical coupling medium, and which is sealed by the membrane *4* (not shown in FIG. *12* for reasons of clarity). The recess *6* together with the sealing membrane *4* forms a closed cavity which is filled with the coupling medium.

[0075] The membrane *4* may be transparent for at least a part of the electromagnetic radiation, such as light, emerging from the fiber cables *2b*. In some instances, the membrane *4* is acoustically-matched to the acoustical properties of the tissue.

[0076] The front aperture, i.e. open end of the recess *6* sealed with the membrane *4*, of the handheld device *10* is designed to have contact with the tissue. The flexible, or alternatively rigid, membrane *4* is designed such that it can assume a concave shape, which is optimal for radial ultrasound wave propagation for a given arrangement of detectors. Different forms of the membrane *4* can be used within the assembly by exchanging the front frame of the encasement *7*.

[0077] In the embodiment shown, the encasement *7* has an indentation *4a* which is sealed with the flexible membrane *4* such that a section of the membrane *4* in the region of the indentation *4a* exhibits an indentation. Due to the mechanical flexibility of the membrane *4*, the form of the indentation of the membrane *4* follows the object surface's curvature. By this means, the object can be safely and reliably positioned in the indentation of the membrane and can be illuminated with the irradiation light cone *5*.

[0078] The light delivery system comprises a fiber bundle consisting of *640* multimode fibers enclosed in four metal ferrules *2a*. The fibers deliver illumination onto the tissue surface attached to the membrane. Diameters of core and two claddings of fiber used were 189, 1 and 200 microns, respectively.

[0079] The assembly of light guides *2a* and *2b*, the array of ultrasonic transducers *1a* and the membrane *4* are fixed with the encasement in which a chamber for the index-matching liquid is formed. The mentioned liquid may have acoustic properties similar to the tissue under investigation. Moreover it is preferred that it does not absorb the excitation radiation.

[0080] In some embodiments, the recess *6* provided in the encasement *7* has a hemispherical shape. In some instances, its surface is polished in order to achieve good light reflection. In this way, electromagnetic radiation reflected from the tissue surface or the membrane *4* will be guided into the imaged region of interest so that higher illumination efficiency, better signal-to-noise ratio and therefore a better image quality will be achieved.

[0081] FIG. *13* shows a cross-sectional side view of an example of a second prototype of the handheld device *10* according to the present disclosure. FIG. *14* shows a perspective view of the example of a second prototype of the handheld device *10* according to the present disclosure.

[0082] The, curved or two-dimensional, transducer array *1a* and the optical fiber bundle *2b* are stacked and encased within a two-piece metal casing *7*. The array *1a* consists of 128 transducer elements arrayed along an arc, such as a circular arc, and cylindrically focused to the center of the arc along

which they are arranged, i.e. the surface normal (not shown) of each of the transducer elements intersect at the center of the arc or within a region around the center of the arc or curvature.

[0083] The fiber bundle *2b* consists of 256 individual multimode fibers having a 283 μm diameter core and 300 μm diameter cladding. Fiber tips were bent by 33 degrees with respect to the normal to the face plane of the ferrule (not shown) and the transducer elements in order to direct the light beam *5* onto the imaged region of interest on or within the object.

[0084] The coupling membrane *4* between the liquid-filled recess *6* and the imaged object is made of a semi-rigid plastic in some embodiments. Its surface may be glued with pressure-sensitive adhesive onto the convex face of the casing *7*.

[0085] The handheld device *10* shown in FIG. *14* may also comprise a liquid recirculator for removing liquid from the recess *6* and re-introducing liquid into the recess *6*. According to the embodiments shown in FIGS. *1* to *12*, respective openings in the recess *6* as well as appropriate conveyance means for conveying liquid, for example, coupling medium, into and out of the recess *6* would have to be provided.

[0086] Moreover, the embodiments described with reference to FIGS. *1* to *14* may be further equipped with a liquid temperature control unit for controlling the temperature of the liquid accommodated in the recess *6* or *12*, respectively, a degasser for removing gas from the liquid and/or a photodetector for measuring the energy of every single radiation pulse. The mentioned fiber bundle *2b* or *16*, respectively, may be followed by focusing or collimating lenses or prisms.

[0087] Although not explicitly stated, the casing *1b* together with the transducer array *1a* of the embodiments shown in FIGS. *11* to *14* can be movably mounted in the encasement *7* such that the array *1a* can be moved toward and/or away from the object under investigation, whereby the distance between the transducer elements and the object and therefore the region of interest on or within the object can be varied. For this purpose, a moving mechanism is provided for moving the transducer array *1a* and/or the illumination unit *2b*, i.e. the end of the fiber bundle *2b*, back and forth similar to the moving mechanism *19* shown in FIG. *6*, *9* or *10*, respectively. The elucidations given above with respect to FIGS. *5*, *6*, *9* and *10*, for example, those regarding the intersection point *P* of the surface normals *21* and the light cone *20*, apply accordingly.

[0088] Without further elaboration, it is believed that one skilled in the art can use the preceding description to utilize the present disclosure to its fullest extent. The examples and embodiments disclosed herein are to be construed as merely illustrative and exemplary and not a limitation of the scope of the present disclosure in any way. It will be apparent to those having skill in the art, and having the benefit of this disclosure, that changes may be made to the details of the above-described embodiments without departing from the underlying principles of the disclosure herein.

1. A handheld device for optoacoustic imaging of an object, the handheld device comprising:

- an irradiation unit configured to irradiate the object with electromagnetic radiation, and
- a detector unit configured to detect acoustic waves generated in the object upon irradiation with electromagnetic radiation,

wherein the detector unit comprises an array of detector elements and a recess in which the irradiation unit and the array of detector elements are disposed, and

- wherein the detector elements are arranged in the recess such that the surface normals of at least a part of the detector elements are directed to a region of interest of the object.
- 2. The handheld device according to claim 1, wherein the electromagnetic radiation comprises light.
- 3. The handheld device according to claim 1, wherein the acoustic waves comprise ultrasonic waves.
- 4. The handheld device according to claim 1, further comprising:
 - a container in which the recess, the irradiation unit, and the detector unit are located, the container moveably mounted to a carrier such that while images are acquired from the object, the container can be moved with respect to the object and wherein the location of the region of interest and/or the irradiated region of the object can be changed.
- 5. The handheld device according to claim 1, wherein the recess is sealed with a cover element such that the recess and the cover element comprise a cavity, and wherein the cavity accommodates a coupling medium.
- 6. The handheld device according to claim 5, wherein the coupling medium comprises water.
- 7. The handheld device according to claim 5, wherein the region of interest of the object is located either around the cover element or beyond the cover element.
- 8. The handheld device according to claim 5, wherein the cover element comprises a mechanically flexible element.
- 9. The handheld device according to claim 8, wherein the cover element comprises a membrane or a film.
- 10. The handheld device according to claim 5, wherein at least a section of the cover element has a convex shape.
- 11. The handheld device according to claim 5, wherein the cover element is configured such that at least a section of the cover element comes into contact with the object while images are acquired from the object.
- 12. The handheld device according to claim 5, wherein at least one conveyance unit is provided for conveying the coupling medium into and/or out of the recess.

- 13. The handheld device according to claim 1, wherein the array of detector elements is a curved array of detector elements.
- 14. The handheld device according to claim 1, wherein the recess comprises at least one curved surface.
- 15. The handheld device according to claim 14, wherein the curved array of detector elements is disposed along at least a portion of the curved surface of the recess.
- 16. The handheld device according to claim 14, wherein the irradiation unit is disposed at the curved surface of the recess.
- 17. The handheld device according to claim 14, wherein at least a section of the curved surface of the recess is configured such that reflection of acoustic waves incident on the curved surface of the recess towards the array of detector elements is reduced or avoided.
- 18. The handheld device according to claim 1, wherein at least one of:
 - A—the curvature;
 - B—the size; and
 - C—the angular coverage of the array of detector elements depends on at least one of:
 - A—the size of the object and
 - B—the region of interest of the object.
- 19. A method for optoacoustic imaging of an object comprising:
 - irradiating the object with electromagnetic radiation by an irradiation unit and
 - detecting acoustic waves, which are generated in the object upon irradiation with electromagnetic radiation, by an array of detector elements,
 - wherein the irradiation unit and the array of detector elements are disposed in a recess and the detector elements are arranged in the recess such that the surface normals of at least a part of the detector elements are directed to a region of interest of the object.
- 20. The method of claim 19, wherein the electromagnetic radiation comprises light.
- 21. The method of claim 19, wherein the acoustic waves comprise ultrasonic waves.

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